## Solid Mechanics

## (Based on notes by Prof. Alain Goriely)

Mathematical Institute, University of Oxford
Michaelmas Term 2021

Prof. Dominic Vella

$20^{\text {th }}$ December, 2021

## Contents

1 Introduction: one-dimensional elasticity ..... 8
1.1 A one-dimensional theory ..... 8
1.2 Kinematics ..... 8
1.3 Dynamics ..... 9
1.3.1 Conservation of mass ..... 9
1.3.2 Balance of linear momentum ..... 9
1.3.3 Constitutive laws ..... 11
2 Kinematics ..... 12
2.1 Scalars, vectors, and tensors ..... 12
2.2 Spatial derivatives of tensors ..... 15
2.3 Derivatives in curvilinear coordinates ..... 17
2.4 Derivatives of scalar functions of tensors ..... 18
2.5 The deformation gradient ..... 19
2.6 Volume, surface, and line elements ..... 21
2.7 Polar decomposition theorem ..... 23
2.8 Velocity, acceleration, and velocity gradient ..... 24
2.9 Examples of deformation ..... 25
2.9.1 Homogeneous deformation ..... 25
2.9.2 Inflation of a spherical shell ..... 26
3 Conservation Laws, Stress, and Dynamics ..... 28
3.1 Balance of mass ..... 28
3.1.1 Transport formulas ..... 29
3.2 Balance of linear momentum ..... 29
3.3 Balance of angular momentum ..... 30
3.4 Many stress tensors ..... 31
3.5 Balance of energy for elastic materials ..... 32
4 Constitutive equations ..... 34
4.13 types of assumptions ..... 34
4.1.1 Particular examples ..... 34
4.2 Elastic materials ..... 35
4.3 Constitutive equations for hyperelastic materials ..... 35
4.4 Internal material constraint ..... 36
5 Summary of equations ..... 38
5.1 Boundary conditions ..... 38
6 Isotropic materials ..... 39
6.1 Objectivity and material symmetry ..... 39
6.2 Symmetry of isotropic materials ..... 39
6.3 Adscititious inequalities ..... 41
6.3.1 Example: pure shear of an elastic cube ..... 42
6.4 Choice of strain-energy functions ..... 43
7 Examples of boundary value problems ..... 46
7.1 A simple homogeneous deformation ..... 46
7.2 The half-plane in compression ..... 47
7.3 Inflation of a spherical shell. ..... 48
7.4 The inflation-extension of a tube ..... 52
7.4.1 $\quad$ A toy model for an artery ..... 54
8 Linear Elasticity ..... 58
8.1 Infinitesimal strain tensor ..... 58
8.2 Constant relationships ..... 58
8.3 Isotropic linear elasticity ..... 60
8.3.1 Summary of equations ..... 60
8.4 Examples ..... 61
8.5 Incompressible linear elasticity ..... 62
8.5.1 General principles ..... 63
8.6 Plane/Strain/Stress Solutions ..... 64
8.6.1 Plane solutions ..... 64
8.6.2 Idea ..... 64
8.6.3 Equations ..... 64
8.6.4 Compatibility conditions ..... 65
8.7 Elasto-dynamics ..... 65
8.7.1 Planar waves ..... 66

HEALTH WARNING: The following lecture notes are meant as a rough guide to the lectures. They are not meant to replace the lectures. You should expect that some material in these notes will not be covered in class and that extra material will be covered during the lectures (especially longer proofs, examples, and applications). Nevertheless, I will try to follow the notation and the overall structure of the notes as much as possible.

WHAT IS EXAMINABLE? The one and only official examinable content of the course is described on the web page https://courses.maths.ox.ac.uk/.

## Useful formulae

A few key formulae and definitions that we will be using throughout this course.
Tensor calculus Here $\phi, \mathbf{v}, \mathbf{T}$ are, respectively, scalar, vector and $2^{\text {nd }}$-order tensor fields defined on a moving body. Upper case variables refer to the reference configuration, lower case variables to the current configuration.

$$
\begin{array}{ll}
\mathbf{F}=\operatorname{Grad} \mathbf{x}=\frac{\partial x_{i}}{\partial X_{j}} \mathbf{e}_{i} \otimes \mathbf{E}_{j} & \text { Deformation Gradient } \\
J=\operatorname{det} \mathbf{F} & \text { Determinant of } \mathbf{F} \\
\operatorname{grad} \mathbf{v}=\frac{\partial \mathbf{v}}{\partial x_{i}} \otimes \mathbf{e}_{i} & \text { Definition of the gradient of a vector } \\
\operatorname{grad} \mathbf{T}=\frac{\partial \mathrm{T}}{\partial x_{i}} \otimes \mathbf{e}_{i} & \text { Definition of the gradient of a tensor } \\
\operatorname{div} \mathbf{T}=\frac{\partial T_{i j}}{\partial x_{i}} \mathbf{e}_{j} & \text { Definition of the divergence of a tensor } \\
\operatorname{Grad} \phi=\mathbf{F}^{\mathbf{T}} \operatorname{grad} \phi & \text { Gradient of a scalar } \\
\operatorname{Grad} \mathbf{v}=(\operatorname{grad} \mathbf{v}) \mathbf{F} & \text { Gradient of a vector } \\
\operatorname{Div} \mathbf{v}=J \operatorname{div}\left(J^{-1} \mathbf{F v}\right) & \text { Divergence of a vector } \\
\operatorname{Div} \mathbf{T}=J \operatorname{div}\left(J^{-1} \mathbf{F T}\right) & \text { Divergence of a tensor } \\
\operatorname{div}\left(J^{-1} \mathbf{F}\right)=0 & \text { An important identity } \\
\frac{\partial}{\partial \lambda}(\operatorname{det} \mathbf{T})=(\operatorname{det} \mathbf{T}) \operatorname{tr}\left(\mathbf{T}^{-1} \frac{\partial \mathbf{T}}{\partial \lambda}\right) & \text { A useful identity. } \lambda \text { is a scalar } \tag{T11}
\end{array}
$$

## Kinematics

| $\mathbf{F}=\operatorname{Grad} \mathbf{x}(\mathbf{X}, t)$ | The deformation gradient | $(K 1)$ |
| :--- | :--- | ---: |
| $J=\operatorname{det} \mathbf{F}$ | Determinant of $\mathbf{F}$ | $(K 2)$ |
| $\mathrm{d} \mathbf{x}=\mathbf{F} \mathrm{d} \mathbf{X}$ | Transformation of line element | $(K 3)$ |
| $\mathrm{d} \mathbf{a}=J \mathbf{F}^{-\mathrm{T}} \mathrm{d} \mathbf{A}$ | Transformation of area element | $(K 4)$ |
| $\mathrm{d} v=J \mathrm{~d} V$ | Transformation of volume element | $(K 5)$ |
| $\mathbf{C}=\mathbf{F}^{\mathrm{T}} \mathbf{F}$ | Right Cauchy-Green tensor | $(K 6)$ |
| $\mathbf{B}=\mathbf{F} \mathbf{F}^{\mathrm{T}}$ | Left Cauchy-Green tensor | $(K 7)$ |
| $\mathbf{E}=\frac{1}{2}\left(\mathbf{F}^{\mathrm{T}} \mathbf{F}-\mathbf{1}\right)$ | Euler strain tensor | $(K 8)$ |
| $\mathbf{L}=\operatorname{grad} \mathbf{v}$ | Velocity gradient | $(K 9)$ |
| $\dot{\mathbf{F}}=\mathbf{L} \mathbf{F}$ | Evolution of the deformation gradient $(\mathbf{v}:$ velocity) | $(K 10)$ |
| $\dot{J}=J \operatorname{div} \mathbf{v}$ | Evolution of the volume element | $(K 11)$ |
| $\mathbf{D}=\frac{1}{2}\left(\mathbf{L}+\mathbf{L}^{\mathrm{T}}\right)$ | Eulerian strain rate tensor | $(K 12)$ |
| $\mathbf{W}=\frac{1}{2}\left(\mathbf{L}-\mathbf{L}^{\mathrm{T}}\right)$ | Rate of rotation tensor | $(K 13)$ |

Mechanics Here $\rho$ is the mass density, $\mathbf{T}$ the Cauchy stress tensor, $\mathbf{v}$ the velocity, $W=J \Psi$, where $\Psi$ is the internal energy density.

$$
\begin{array}{lll}
\dot{\rho}+\rho \operatorname{divv}=0 & \text { Conservation of mass (Eulerian form) } \\
\operatorname{div} \mathbf{T}+\rho \mathbf{b}=\rho \dot{\mathbf{v}} & \text { Conservation of linear momentum (Eulerian form) }  \tag{M2}\\
\operatorname{div} \mathbf{T}^{\mathrm{T}}=\mathbf{T}=0 & \text { Conservation of angular momentum (Eulerian form) } \\
\dot{W}=J \operatorname{tr}(\mathbf{T D}) & \text { Conservation of energy (Eulerian form) } \\
\mathbf{T n}=\mathbf{t} & \text { Surface traction associated with } \mathbf{T}(\mathbf{n}: \text { normal outward unit) } & (M 4) \\
\hline(M 4) \\
\hline
\end{array}
$$

Material frame indifference Consider two different frames, connected by a rigid body motion $\mathbf{x}^{*}=\mathbf{Q} \mathbf{x}+\mathbf{c}$. Let $\phi, \mathbf{v}, \mathbf{T}$ be, respectively, scalar, vector and $2^{n d}$-order tensor fields, and $\mathbf{F}$ the deformation gradient. Then

\[

\]

## List of assumptions

- Continuum assumption. We consider a body with reference configuration $\mathcal{B}_{0} \subset \mathbb{R}^{3}$. At time $t$, the body occupies the current configuration $\mathcal{B}_{t} \subset \mathbb{R}^{3}$. A material point, initially at $\mathbf{X} \in \mathcal{B}_{0}$ is mapped to a point $\mathbf{x} \in \mathcal{B}_{t}$ by the one-parameter mapping $\mathbf{x}=$ $\chi(\mathbf{X}, t)$ so that $\chi: \mathcal{B}_{0} \rightarrow \mathcal{B}_{t}$. The continuum assumption states that $\chi$ is a bijection mapping for all time $t$. This implies that we can write $\mathbf{x}=\chi^{-1}(\mathbf{X})$. We further assume that this mapping is twice continuously differentiable in $\mathbf{X}$ and $t$. This assumption can be relaxed in problems involving phase boundaries (with possible jumps in the first derivative). In many instances and applications, we will assume that $\chi$ is actually smooth.
- Conservation of mass. We assume the existence of a scalar density function $\rho=\rho(\mathbf{x})$ defined on the body $\mathcal{B}_{t}$ and whose integral over any material subset $\Omega_{t} \subset \mathcal{B}_{t}$ of the body remains constant in time. So that $\frac{\mathrm{d}}{\mathrm{d} t} \int_{\Omega_{t}} \rho(\mathbf{x}) \mathrm{d} v=0$
- Balance of linear momentum. We assume that the rate of change of linear momentum of an arbitrary material subset $\Omega_{t} \subset \mathcal{B}_{t}$ is equal to sum of all the forces acting on $\Omega_{t}$.
- Balance of angular momentum. We assume that the rate of change of angular momentum of an arbitrary material subset $\Omega_{t} \subset \mathcal{B}_{t}$ with respect to a given point is equal to sum of all the torques acting on $\Omega_{t}$ with respect to the same point.
- Polar media. For polar media, we assume that the body is not subject to body or contact torques.
- Cauchy's postulate. Cauchy's postulate simply states that the traction vector on a given surface element depends smoothly on the the normal to that element.


## Foreword

The traditional approach to continuum mechanics is to consider the regime of small deformations, where a material is slightly perturbed from an unstressed configuration. In that regime, the governing equations and constitutive relationships are linear. An example of this approach is found in the theory of linear elasticity that has been successfully developed over the last two centuries to address many fundamental problems of physics and engineering 93 .

Starting in the 1940 's, it was found that the theory of linear elasticity was inadequate to model the response of elastomers such as rubbers in large deformations [128, 147. Similarly, many tissues and organs also operate in large deformations. For instance, large arteries in mammals are typically stretched between $20 \%$ to $60 \%$ from their unloaded configurations [68, 83] and their response to loads is drastically different from the response of elastomers.


Figure 1: The importance of nonlinearities and large deformations is demonstrated in a pressure experiment, as originally investigated by Mallock in 1890 [102] (A). The experiment consists of increasing the pressure inside a tube or a sphere while recording the radius of the bulge. B. In the case of rubber, the experiment of Osborne and Sutherland [122] shows a sudden limit-point instability at a critical pressure. Past that pressure, the radius suddenly increases. C. In a similar experiment performed on a dog bladder, the behavior of the system is qualitatively different and the instability disappears. In this case, it will be increasingly harder to increase the size of the bulge by increasing the pressure.

A striking example of the difference between rubbers and soft tissues is observed in experiments first performed in the nineteenth century [102, 122]. In these experiments, a cylindrical elastic membrane made out of rubber or soft tissue is pressurized (see Figure 11). At a critical pressure, the radius of the rubber cylinder will suddenly jump to a new equilibrium, whereas for soft tissues, the radius will evolve continuously to an asymptotic radius. Therefore, a continuum theory for the mechanical response of materials in large deformations requires the general theory of nonlinear elasticity, which, in contrast to the theory of linear elasticity, assumes neither small deformations, a particular choice of constitutive law, nor a particular symmetry of the material.

In these notes, we review the general theory of nonlinear solid mechanics, starting with the description of kinematics and moving to the Cauchy equations governing the response of a continuum. The first part is a general approach to continuum mechanics. The second part is the specialisation to elasticity. In the theory of elasticity, these equations are complemented by constitutive laws relating stresses to strains. The theory is presented at an introductory level and further details can be found in the textbooks of Ogden [118], Gurtin, Fried, and Anand [60, 61, Truesdell and Noll [146, or Antman (7).

## 1 Introduction: one-dimensional elasticity

■ Overview We explore elasticity in one dimension to give a general idea of the different steps necessary to develop a general theory of elasticity.

### 1.1 A one-dimensional theory

Here, we consider a one-dimensional continuum that can only deform along its length. Therefore, there is no bending, twisting, or shearing, just stretching. The emphasis here is on understanding the different steps that enter in the development of a full theory of continuum in the simplest possible context. The steps are

1) Kinematics: A description of the possible deformations. The definition of strains, given by geometry. In our context, it is just the stretch along the line.
2) Mechanics: The definitions of stresses and forces acting on the medium. Then a statement of balance laws based on the balance of linear and angular momenta, this is applicable to all continuum media but for our problem, linear momentum is sufficient.
3) Constitutive laws: A statement of the relationship between stresses and strains. This is where we describe the response of the material under loads.

The results of these three steps is a closed set of equations whose solutions (with appropriate boundary conditions and initial data) is a description of the stresses and deformations in a particular body under a particular set of forces.

### 1.2 Kinematics

Consider a 1D continuum of length L. Any material point is labelled by $X \in[0, L]$. The motion or deformation is the mapping $x=x(X, t)$, which is assumed smooth and invertible to ensure that there is no material separation, discontinuity, or overlap. The kinematics is

fully described by a the stretch and the velocity at one point.

$$
\begin{equation*}
\lambda=\frac{\partial x}{\partial X}, \quad \text { stretch; } \quad \dot{x}=V(X, t)=\frac{\partial x}{\partial t}, \quad \text { velocity. } \tag{1}
\end{equation*}
$$

Since the mapping is invertible, we have $\lambda>0$ for all motion. The identity mapping $x=X$ corresponds to the stress-free (Langrangian) configuration.

Motion: The velocity of a material point is $V(X, t)=\dot{x}=\partial x / \partial t$. Since $X=X(x, t)$ is invertible, we can write,

$$
\begin{equation*}
v(x, t)=\dot{x}(X(x, t), t), \tag{2}
\end{equation*}
$$

where $v$ is the velocity at the spatial point $x$.
The acceleration of a point is,

$$
\begin{equation*}
\ddot{x}(X, t)=\frac{\mathrm{D}^{2} x}{\mathrm{D} t^{2}}, \quad \text { or } \quad a=\frac{\mathrm{D} v}{\mathrm{D} t}=\frac{\partial v}{\partial t}+v \frac{\partial v}{\partial x}, \tag{3}
\end{equation*}
$$

where

$$
\begin{equation*}
\frac{\mathrm{D}}{\mathrm{D} t}=\frac{\partial}{\partial t}+v \frac{\partial}{\partial x}, \tag{4}
\end{equation*}
$$

is the material time derivative. (Note that we shall use the notation common in fluid mechanics that $\frac{\mathrm{D}}{\mathrm{Dt}}$ corresponds to a material time derivative for consistency with courses in Part B; elsewhere, including in old exam questions, it may be written $\frac{d}{d t}$.)

### 1.3 Dynamics

We use two fundamental principles to obtain equations for the motion of a continuum: the conservation of mass and the balance of linear momentum (in a general theory we will also need the balance of angular momentum but it does not play a role in 1D).

### 1.3.1 Conservation of mass

We define $\rho$ to be the linear density in the current configuration (mass per unit length as measured in the current configuration) and $\rho_{0}$ the linear density in the reference configuration. Assuming no mass is created, we have

$$
\begin{equation*}
\int_{X_{1}}^{X_{2}} \rho_{0} \mathrm{~d} X=\int_{x_{1}}^{x_{2}} \rho \mathrm{~d} x \tag{5}
\end{equation*}
$$

with $x_{1}=x\left(X_{1}, t\right), x_{2}=x\left(X_{2}, t\right)$. Since $\mathrm{d} x=\lambda \mathrm{d} X$, we have

$$
\begin{equation*}
\int_{X_{1}}^{X_{2}} \rho_{0} \mathrm{~d} X=\int_{X_{1}}^{X_{2}} \rho \lambda \mathrm{~d} X \tag{6}
\end{equation*}
$$

which implies that $\lambda \rho=\rho_{0}$, the Lagrangian conservation of mass. This is the first conservation law.

### 1.3.2 Balance of linear momentum

The general principle for the balance of linear momentum is

$$
\frac{\mathrm{d}}{\mathrm{~d} t}(\text { linear momentum })=\text { force acting on the system. }
$$

Let us decompose this into the following pieces:


## 1) The linear momentum:

$$
\begin{equation*}
\int_{X_{1}}^{X_{2}} \rho_{0} \dot{x} \mathrm{~d} X \tag{7}
\end{equation*}
$$

2) forces: themselves further decompose into forces due to external (body) forces or internal (contact) forces:

- Body forces,

$$
\begin{equation*}
\int_{X_{1}}^{X_{2}} \rho_{0} f \mathrm{~d} X \tag{8}
\end{equation*}
$$

where $f$ is the density of body force (force per unit mass).

- Contact forces: force the material exerts on itself.


This material exerts a force $n\left(X_{2}\right)$ on $\left[0, X_{2}\right]$ counted positive (tensile) if the force is in the direction of the axis, compressive otherwise. Therefore, from the principle of action=reaction, the contact force acting on the segment $\left[X_{1}, X_{2}\right]$ is $n\left(X_{2}\right)-n\left(X_{1}\right)$.

Therefore, the balance of linear momentum for a one-dimensional continuum implies

$$
\begin{equation*}
\frac{\mathrm{d}}{\mathrm{~d} t} \int_{X_{1}}^{X_{2}} \rho_{0} \dot{x} \mathrm{~d} X=\int_{X_{1}}^{X_{2}} \rho_{0} f \mathrm{~d} X+n\left(X_{2}\right)-n\left(X_{1}\right) \tag{9}
\end{equation*}
$$

We can obtain an expression with a single integral by moving the derivative inside the integral and using the fundamental theorem of calculus,

$$
\begin{equation*}
\int_{X_{1}}^{X_{2}} \frac{\partial n}{\partial X} \mathrm{~d} X=n\left(X_{2}\right)-n\left(X_{1}\right) . \tag{10}
\end{equation*}
$$

That is

$$
\begin{equation*}
\int_{X_{1}}^{X_{2}}\left(\rho_{0} \ddot{x}-\rho_{0}+f \frac{\partial n}{\partial X}\right) \mathrm{d} X=0 . \tag{11}
\end{equation*}
$$

This relation is valid $\forall X_{1}, X_{2}$, so that, we can localise the integral (assuming continuity of the integrand) to obtain

$$
\begin{equation*}
\rho_{0} a=\rho_{0} f+\frac{\partial n}{\partial X} . \tag{12}
\end{equation*}
$$

This is an equation for the force $n(X)$ in the material (Cauchy first equation). This equation is in the reference configuration (all quantities depend on the material variable $X$ and time $t)$. We can obtain an equation in the current configuration by using $\mathrm{d} X=\lambda^{-1} \mathrm{~d} x$

$$
\begin{equation*}
\rho a=\rho f+\frac{\partial n}{\partial x} . \tag{13}
\end{equation*}
$$

But what is $\partial n / \partial x$ ? We need a constitutive law to close the system.

### 1.3.3 Constitutive laws

To close the problem, we need to relate the stresses to the strains, that is a relationship between $\sigma$ and $\lambda$ such as Hooke's law

$$
\begin{equation*}
n=K(\lambda-1) \tag{14}
\end{equation*}
$$

This Hookean law is only typically valid for small deformations. For large deformations, we will assume in general that the material is hyperelastic, that is the constitutive law derives from a potential $\Psi$ capturing the elastic energy associated with deformation so that

$$
\begin{equation*}
n=f(\lambda)=\frac{\partial \Psi}{\partial \lambda} \tag{15}
\end{equation*}
$$

with the requirement that $f(1)=0$ and that the derivative of $f$ at $\lambda=1$ exists. For such systems, the Hooke constant $K=f^{\prime}(1)$ is then simply the linearised behaviour for small deformations around the stress-free state. The theory of three-dimensional elasticity developed in next section when applied to the uniaxial extension of an incompressible rectangular neo-Hookean bar suggests the following nonlinear law

$$
\begin{equation*}
n=\frac{K}{3}\left(\lambda^{2}-\lambda^{-1}\right), \tag{16}
\end{equation*}
$$

Close to $\lambda=1$, we recover Hooke's law (as shown in Fig 2). More generally, materials


Figure 2: Comparison between the linear (dash) and nonlinear (solid) Hookean response for $K=3$.
that show strain-stiffening (increase in stiffness for large deformations) or strain-softening (decrease in stiffness) can be modelled by various functions of the stretch.

## 2 Kinematics

- Overview We develop a completely general theory for the deformation of three-dimensional bodies with no assumptions on displacements. To do so, we introduce two configurations and relate them through the motion in time and the deformation gradient. The deformation gradient is naturally defines as a two-point tensors and its analysis require some tensor calculus.

Our first task consists in defining properly the deformation of a body in a three-dimensional space. To do so, we first define our body as occupying a region of a three-dimensional space. After a deformation, the body also occupies a region in space and the motion of each point of the body, from its initial to its current positions, can be defined by a mapping. The relative motion of nearby points can be extracted from this mapping and its derivatives in space and time. It allows us to define key quantities such as strains and stretch. Therefore, we first introduce basic notion of kinematics in three dimensions.

A body $B$ is a set of material points whose elements can be put into a 1-1 correspondence (bijection) with points in a region $\mathcal{B} \subset \mathbb{E}^{3}$. As the body moves or deforms, this set can change with time $t \in \mathbb{R}$. In nonlinear elasticity, one considers multiple configurations for the description of a body and denotes by $\mathcal{B}_{t}$ (or $\mathcal{B}$, when there is no possibility of confusion) the configuration of $B$ at time $t$.

For static systems, we use $\mathcal{B}_{0}$ as the initial configuration, typically an unloaded configuration, and $\mathcal{B}$ for the current configuration where loads are applied. The initial configuration, $\mathcal{B}_{0}$, is parameterized by material points relative to the position vector $\mathbf{X}_{0}$ with origin $\mathbf{O}$ and the current configuration, $\mathcal{B}$, by the position vector $\mathbf{x}$ with origin $\mathbf{o}$.

The basic assumption for the deformation of a continuum is that the body retains its integrity and that material points do not overlap during a deformation. Therefore, both $\mathcal{B}_{0}$ and $\mathcal{B}$ are bijections of $B$, and there exists an invertible mapping, pictured in Figure 3, called deformation or motion $\boldsymbol{\chi}: \mathcal{B}_{0} \rightarrow \mathcal{B}_{t}$ such that

$$
\begin{equation*}
\mathbf{x}=\chi(\mathbf{X}, t), \quad \forall \mathbf{X} \in \mathcal{B}_{0} \quad \text { and } \quad \mathbf{X}=\chi^{-1}(\mathbf{x}, t), \quad \forall \mathbf{x} \in \mathcal{B}_{t} . \tag{17}
\end{equation*}
$$

In the absence of phase boundaries, singularities, or jumps, we assume that this mapping is twice continuously differentiable in space and smooth in time.

It is convenient to use two orthonormal rectangular Cartesian bases: the initial basis $\left\{\mathbf{E}_{1}, \mathbf{E}_{2}, \mathbf{E}_{3}\right\}$ and the current basis $\left\{\mathbf{e}_{1}, \mathbf{e}_{2}, \mathbf{e}_{3}\right\}$ to represent vectors in the initial and current configurations:

$$
\begin{equation*}
\mathbf{X}=X_{i} \mathbf{E}_{i}, \quad \mathbf{x}=x_{i} \mathbf{e}_{i}, \tag{18}
\end{equation*}
$$

where summation over repeated indices is always assumed unless explicitly specified.
The convention in continuum mechanics is to refer to coordinates in the current configuration, or quantities expressed with these coordinates, as Eulerian or spatial. Coordinates in the initial configuration, or quantities expressed with these coordinates, are referred to as Lagrangian, referential, or material.

### 2.1 Scalars, vectors, and tensors

To describe the deformations of a body $B$, we introduce, at each material point, physical quantities known as fields; this makes continuum mechanics a theory of fields. These quantities can be scalar fields, such as density, temperature; vector fields, such as velocity, acceleration, force; or tensor fields, such as deformation gradients or stress and strain tensors. These different fields can all be understood as tensor fields of different orders. By definition, a scalar


Figure 3: Basic kinematics of nonlinear elasticity. Two configurations are defined. The deformation is a 1-1 map between points of the reference configuration $\mathcal{B}_{0}$ and points of the current configuration $\mathcal{B}$.
field is a tensor field of order 0 and a vector field is a first-order tensor field. Higher-order tensor fields require the definition of the tensor product.

The scalar product between two vectors $\mathbf{a}=a_{i} \mathbf{e}_{i}$ and $\mathbf{b}=b_{i} \mathbf{e}_{i}$, in the same vector space, follows the usual definition:

$$
\begin{equation*}
\mathbf{u} \cdot \mathbf{v}=u_{i} v_{i}, \tag{19}
\end{equation*}
$$

and is used to defined the Euclidean norm

$$
\begin{equation*}
|\mathbf{v}|=\sqrt{\mathbf{v} \cdot \mathbf{v}} \tag{20}
\end{equation*}
$$

We can also use the scalar product to define the tensor product. Consider two vectors $\mathbf{u}=u_{i} \mathbf{e}_{i}$ and $\mathbf{v}=v_{i} \mathbf{E}_{i}$, not necessarily defined in the same vector space. Then, the tensor product, $\mathbf{u} \otimes \mathbf{v}$, of these two vectors is a second-order tensor such that, for an arbitrary vector $\mathbf{a}=a_{i} \mathbf{E}_{i}$,

$$
\begin{equation*}
(\mathbf{u} \otimes \mathbf{v}) \mathbf{a}=(\mathbf{v} \cdot \mathbf{a}) \mathbf{u} \tag{21}
\end{equation*}
$$

(In more familiar vector notation, we can also write $\mathbf{u} \otimes \mathbf{v}=\mathbf{u v}^{\mathrm{T}}$.) This definition implies that the vector $\mathbf{v}$ and a must belong to the same vector space, but in general, $\mathbf{u}$ can belong to a different space. We see from this definition that a second-order tensor maps vectors from one vector space to vectors in another vector space.

Explicitly, the tensor product is

$$
\begin{equation*}
\mathbf{u} \otimes \mathbf{v}=u_{i} \mathbf{e}_{i} \otimes v_{j} \mathbf{E}_{j}=u_{i} v_{j} \mathbf{e}_{i} \otimes \mathbf{E}_{j} . \tag{22}
\end{equation*}
$$

When there is no possibility of confusion, we can write the components of the second-order tensor $\mathbf{u} \otimes \mathbf{v}$ in the Cartesian bases $\left\{\mathbf{e}_{1}, \mathbf{e}_{2}, \mathbf{e}_{3}\right\}$ and $\left\{\mathbf{E}_{1}, \mathbf{E}_{2}, \mathbf{E}_{3}\right\}$ as $(\mathbf{u} \otimes \mathbf{v})_{i j}=u_{i} v_{j}, i, j=$ $1,2,3$.

Equipped with the tensor product, we can define a general second-order tensor in the Cartesian bases $\left\{\mathbf{e}_{1}, \mathbf{e}_{2}, \mathbf{e}_{3}\right\}$ and $\left\{\mathbf{E}_{1}, \mathbf{E}_{2}, \mathbf{E}_{3}\right\}$ as

$$
\begin{equation*}
\mathbf{T}=T_{i j} \mathbf{e}_{i} \otimes \mathbf{E}_{j} \quad \Longleftrightarrow \quad T_{i j}=\mathbf{e}_{i} \cdot \mathbf{T} \mathbf{E}_{j} \tag{23}
\end{equation*}
$$

which implies that for a vector $\mathbf{a}=a_{j} \mathbf{E}_{j}$,

$$
\begin{equation*}
(\mathbf{T a})_{i}=T_{i j} a_{j} . \tag{24}
\end{equation*}
$$

We define the matrix of components of a tensor in Cartesian coordinates by [ $\mathbf{T}]$ such that $[\mathbf{T}]_{i j}=T_{i j}$. We can then extend most definitions and identities of traditional linear algebra to tensors.

A particularly important class of second-order tensor are the tensors whose component matrices are square matrices. For these second-order tensors, the determinant and trace of a second-order tensor are defined, respectively, as

$$
\begin{equation*}
\operatorname{det} \mathbf{T}=\operatorname{det}([\mathbf{T}]), \quad \operatorname{tr} \mathbf{T}=\operatorname{tr}([\mathbf{T}])=T_{i i} . \tag{25}
\end{equation*}
$$

In particular, in three dimensions, we have

$$
\begin{equation*}
\operatorname{det} \mathbf{T}=\operatorname{det}([\mathbf{T}])=\epsilon_{i j k} T_{1 i} T_{2 j} T_{3 k}, \tag{26}
\end{equation*}
$$

where $\epsilon_{i j k}$ denotes the usual Levi-Civita permutation symbols or permutation symbols, that is $\epsilon_{i j k}=1$ is $(i, j, k)$ for an even permutation of $(1,2,3),-1$ if it is an odd permutation, and 0 if any index is repeated.

Similarly, the matrix of the transpose of a tensor is the transpose of the matrix, that is

$$
\begin{equation*}
\left[\mathbf{T}^{\boldsymbol{\top}}\right]=[\mathbf{T}]^{\boldsymbol{\top}} \tag{27}
\end{equation*}
$$

and a tensor is symmetric, $\mathbf{T}^{\boldsymbol{\top}}=\mathbf{T}$, if and only if $T_{i j}=T_{j i}$.
The product of two tensors $\mathbf{S}$ and $\mathbf{T}$ is only defined when the image of a vector by $\mathbf{T}$ is in the domain of $\mathbf{S}$. Then, for an arbitrary vector $\mathbf{a}$, we have

$$
\begin{equation*}
(\mathbf{S T}) \mathbf{a}=\mathbf{S}(\mathbf{T a}) . \tag{28}
\end{equation*}
$$

In such cases, the matrix of the product is the product of the two matrices:

$$
\begin{equation*}
[\mathbf{S T}]=[\mathbf{S}][\mathbf{T}] . \tag{29}
\end{equation*}
$$

A tensor $\mathbf{S}$ is an orthogonal tensor if

$$
\begin{equation*}
\mathbf{S S}^{\top}=\mathbf{S}^{\top} \mathbf{S}=\mathbf{1}, \tag{30}
\end{equation*}
$$

where $\mathbf{1}$ is the identity tensor defined as $(\mathbf{1}) \mathbf{a}=\mathbf{a} \forall \mathbf{a}$. As expected, it follows that the components of an orthogonal tensor is an orthogonal matrix. The group of all orthogonal tensors in three dimensions is denoted $O(3)$. A proper orthogonal tensor is an orthogonal tensor with the additional property $\operatorname{det} \mathbf{S}=1$. The group of all proper orthogonal tensors in three dimensions is denoted $S O(3)$. Orthogonal and proper orthogonal tensors are particularly useful to characterize rotations and proper rotations in a three-dimensional space.

We can also contract two tensors together to obtain a scalar by introducing the double contraction

$$
\begin{equation*}
\mathbf{S}: \mathbf{T}=\operatorname{tr}(\mathbf{S T})=S_{i j} T_{j i} . \tag{31}
\end{equation*}
$$

If the determinant of a tensor $\mathbf{T}$ does not vanish, the matrix of inverse of $\mathbf{T}$ is the inverse of the matrix:

$$
\begin{equation*}
\left[\mathbf{T}^{-1}\right]=[\mathbf{T}]^{-1} \tag{32}
\end{equation*}
$$

Explicitly, for a tensor $\mathbf{T}=T_{i j} \mathbf{e}_{i} \otimes \mathbf{E}_{j}$, we have

$$
\begin{equation*}
\mathbf{T}^{-1}=\left([\mathbf{T}]^{-1}\right)_{i j} \mathbf{E}_{i} \otimes \mathbf{e}_{j} \tag{33}
\end{equation*}
$$

so that

$$
\begin{align*}
& \mathbf{T T}^{-1}=\mathbf{1}=\delta_{i j} \mathbf{e}_{i} \otimes \mathbf{e}_{j},  \tag{34}\\
& \mathbf{T}^{-1} \mathbf{T}=\mathbf{1}=\delta_{i j} \mathbf{E}_{i} \otimes \mathbf{E}_{j}, \tag{35}
\end{align*}
$$

where $\delta_{i j}$ is the usual Kronecker delta's symbol ( $\delta_{i i}=1$ and $\delta_{i j}=0$ for $i \neq j$ ).
The tensor product can also be used to define higher-order tensors. For instance, a thirdorder tensor, $\mathbf{Q}$, and a fourth-order tensor $\mathcal{Q}$, in the basis $\left\{\mathbf{e}_{1}, \mathbf{e}_{2}, \mathbf{e}_{3}\right\}$ are defined as

$$
\begin{align*}
& \mathbf{Q}=Q_{i j k} \mathbf{e}_{i} \otimes \mathbf{e}_{j} \otimes \mathbf{e}_{k},  \tag{36}\\
& \mathcal{Q}=Q_{i j k l} \mathbf{e}_{i} \otimes \mathbf{e}_{j} \otimes \mathbf{e}_{k} \otimes \mathbf{e}_{l} . \tag{37}
\end{align*}
$$

However, in this case, the equivalence with linear algebra is lost and identities for higher-order tensors must be obtained by following the rules defining the tensor products and playing the game of indices. Note that higher-order tensors can also be defined with respect to multiple vector spaces.

### 2.2 Spatial derivatives of tensors

Next, we define spatial derivatives of scalar, vector, and tensor fields. We have two sets of spatial variables, the Lagrangian variables $\mathbf{X}$ and the Eulerian variables $\mathbf{x}$. We can therefore define different types of spatial derivatives depending on the description of a given quantity.

We first consider the case where $\phi, u, \mathbf{T}$ are scalar, vector and tensor fields respectively over $\mathbf{x}$, that is

$$
\begin{equation*}
\phi=\phi(\mathbf{x}, t), \quad \mathbf{u}=u_{i}(\mathbf{x}, t) \mathbf{e}_{i}, \quad \mathbf{T}=T_{i j}(\mathbf{x}, t) \mathbf{e}_{i} \otimes \mathbf{e}_{j} . \tag{38}
\end{equation*}
$$

We define the Eulerian gradient of scalar and vector functions as

$$
\begin{align*}
\operatorname{grad} \phi & =\frac{\partial \phi}{\partial \mathbf{x}}=\frac{\partial \phi}{\partial x_{i}} \mathbf{e}_{i}  \tag{39}\\
\operatorname{grad} \mathbf{u} & =\frac{\partial \mathbf{u}}{\partial \mathbf{x}}=\frac{\partial \mathbf{u}}{\partial x_{j}} \otimes \mathbf{e}_{j}=\frac{\partial\left(u_{i} \mathbf{e}_{i}\right)}{\partial x_{j}} \otimes \mathbf{e}_{j}=\frac{\partial u_{i}}{\partial x_{j}} \mathbf{e}_{i} \otimes \mathbf{e}_{j} . \tag{40}
\end{align*}
$$

The gradient is an operation that increases the order of the tensor and is defined, in general, as the operation

$$
\begin{equation*}
\operatorname{grad}(\cdot)=\frac{\partial(\cdot)}{\partial x_{j}} \otimes \mathbf{e}_{j} . \tag{41}
\end{equation*}
$$

It follows from this definition that

$$
\begin{equation*}
\operatorname{grad}(\phi \mathbf{u})=\mathbf{u} \otimes \operatorname{grad} \phi+\phi \operatorname{grad} \mathbf{u} \tag{42}
\end{equation*}
$$

Similarly, we define the gradient of a second-order tensor as

$$
\begin{equation*}
\operatorname{grad} \mathbf{T}=\frac{\partial}{\partial x_{k}}\left(T_{i j} \mathbf{e}_{i} \otimes \mathbf{e}_{j}\right) \otimes \mathbf{e}_{k}=\frac{\partial T_{i j}}{\partial x_{k}} \mathbf{e}_{i} \otimes \mathbf{e}_{j} \otimes \mathbf{e}_{k} \tag{43}
\end{equation*}
$$

The divergence decreases the order of a tensor by contracting indices. For a vector, we have simply

$$
\begin{equation*}
\operatorname{div} \mathbf{u}=\frac{\partial u_{i}}{\partial x_{i}} \tag{44}
\end{equation*}
$$

For a second-order tensor, the contraction can take place on the first or second index depending on the convention. Here, we choose to define the divergence as a contraction on the first index, that is

$$
\begin{equation*}
\operatorname{div} \mathbf{T}=\frac{\partial T_{i j}}{\partial x_{k}} \mathbf{e}_{j}\left(\mathbf{e}_{i} \cdot \mathbf{e}_{k}\right)=\frac{\partial T_{i j}}{\partial x_{i}} \mathbf{e}_{j} \tag{45}
\end{equation*}
$$

With this particular definition of the divergence operator, the divergence theorem, applied on a domain $\Omega \subset \mathbb{R}^{3}$, reads

$$
\begin{equation*}
\int_{\partial \Omega} \operatorname{Tn} \mathrm{d} a=\int_{\Omega} \operatorname{div}\left(\mathbf{T}^{\boldsymbol{\top}}\right) \mathrm{d} v \tag{46}
\end{equation*}
$$

We consider now spatial derivatives with respect to Lagrangian coordinates, that is $\Phi, U$, and $\mathbf{T}$ are now fields over $\mathbf{X}$ :

$$
\begin{equation*}
\Phi=\phi(\mathbf{X}, t), \quad \mathbf{U}=u_{i}(\mathbf{X}, t) \mathbf{E}_{i}, \quad \mathbf{T}=T_{i j}(\mathbf{X}, t) \mathbf{e}_{i} \otimes \mathbf{E}_{j} \tag{47}
\end{equation*}
$$

The Lagrangian gradient is then the operation

$$
\begin{equation*}
\operatorname{Grad}(\cdot)=\frac{\partial(\cdot)}{\partial X_{j}} \otimes \mathbf{E}_{j} \tag{48}
\end{equation*}
$$

Note that we use the lower case "grad" and "div" to describe spatial derivatives with respect to Eulerian coordinates and the upper case "Grad" and "Div" for spatial derivatives with respect to Lagrangian coordinates. Explicitly, we have

$$
\begin{align*}
\operatorname{Grad} \Phi & =\frac{\partial \Phi}{\partial \mathbf{X}}=\frac{\partial \Phi}{\partial X_{i}} \mathbf{E}_{i}  \tag{49}\\
\operatorname{Grad} \mathbf{U} & =\frac{\partial \mathbf{U}}{\partial \mathbf{X}}=\frac{\partial \mathbf{U}}{\partial X_{j}} \otimes \mathbf{E}_{j}=\frac{\partial\left(U_{i} \mathbf{E}_{i}\right)}{\partial X_{j}} \otimes \mathbf{E}_{j}=\frac{\partial U_{i}}{\partial X_{j}} \mathbf{E}_{i} \otimes \mathbf{E}_{j}  \tag{50}\\
\operatorname{Grad} \mathbf{T} & =\frac{\partial}{\partial X_{k}}\left(T_{i j} \mathbf{e}_{i} \otimes \mathbf{E}_{j}\right) \otimes \mathbf{E}_{k}=\frac{\partial T_{i j}}{\partial X_{k}} \mathbf{e}_{i} \otimes \mathbf{E}_{j} \otimes \mathbf{E}_{k} \tag{51}
\end{align*}
$$

The divergence is then

$$
\begin{align*}
\operatorname{Div} \mathbf{U} & =\frac{\partial U_{i}}{\partial X_{i}}  \tag{52}\\
\operatorname{Div} \mathbf{T} & =\frac{\partial T_{i j}}{\partial X_{k}} \mathbf{e}_{j}\left(\mathbf{E}_{i} \cdot \mathbf{E}_{k}\right)=\frac{\partial T_{i j}}{\partial X_{i}} \mathbf{E}_{j} \tag{53}
\end{align*}
$$

Note that these definitions can be appropriately modified for the case where $\mathbf{T}=T_{i j} \mathbf{E}_{i} \otimes \mathbf{E}_{j}$ by changing $\mathbf{e}_{j} \rightarrow \mathbf{E}_{j}$ in the definition of Grad and Div.

### 2.3 Derivatives in curvilinear coordinates

It is often convenient to describe a body and a deformation with respect to curvilinear coordinates. For instance, it is natural to use cylindrical coordinates to describe simple deformations of a cylinder. We use the curvilinear coordinates $\left\{q_{1}, q_{2}, q_{3}\right\}$ in the current configuration and $\left\{Q_{1}, Q_{2}, Q_{3}\right\}$ in the reference configuration. These coordinates are related to the Cartesian coordinates in each configuration through the position vectors $\mathbf{x}=\mathbf{x}\left(q_{1}, q_{2}, q_{3}\right)$ and $\mathbf{X}=\mathbf{X}\left(Q_{1}, Q_{2}, Q_{3}\right)$. Here, we use greek subscripts to denote quantities defined in nonCartesian coordinates. For instance, we associate to each coordinate set, a set of basis vectors

$$
\begin{equation*}
\mathbf{e}_{\alpha}=h_{\alpha}^{-1} \frac{\partial \mathbf{x}}{\partial q_{\alpha}}, \quad \mathbf{E}_{\alpha}=H_{\alpha}^{-1} \frac{\partial \mathbf{X}}{\partial Q_{\alpha}}, \quad \alpha=1,2,3, \tag{54}
\end{equation*}
$$

where $h_{\alpha}$ and $H_{\alpha}$ are scale factors, used to normalize the basis vectors:

$$
\begin{equation*}
h_{\alpha}=\left|\frac{\partial \mathbf{x}}{\partial q_{\alpha}}\right|, \quad H_{\alpha}=\left|\frac{\partial \mathbf{X}}{\partial Q_{\alpha}}\right|, \quad \alpha=1,2,3, \tag{55}
\end{equation*}
$$

For brevity, we restrict our attention to a set of orthogonal coordinates, so that

$$
\begin{equation*}
\mathbf{e}_{\alpha} \cdot \mathbf{e}_{\beta}=\delta_{\alpha \beta}, \quad \mathbf{E}_{\alpha} \cdot \mathbf{E}_{\beta}=\delta_{\alpha \beta}, \quad \alpha, \beta=1,2,3 \tag{56}
\end{equation*}
$$

We define the gradient, $\operatorname{grad} \mathbf{T}=\nabla \otimes \mathbf{T}$, of a tensor $\mathbf{T}$ at a point $\mathbf{x} \in \mathcal{B}$ as the tensor that maps a vector $\mathbf{v}$ in the tangent space of $\mathcal{B}$ at $\mathbf{x}$ onto the infinitesimal variation of $\mathbf{T}$ along a path going through $\mathbf{x}$ with tangent $\mathbf{v}$. For any given $\mathbf{v}$, we define a path $\Gamma$, parameterized by its arc length $s$, going through $\mathbf{x}$ and tangent to $\mathbf{v}$. The operation of the gradient on a vector $\mathbf{v}$ is

$$
\begin{align*}
(\nabla \otimes \mathbf{T}) \mathbf{v} & =\frac{\mathrm{d} \mathbf{T}(\Gamma(s))}{\mathrm{d} s}=\lim _{\mathrm{d} s \rightarrow 0} \frac{\mathbf{T}(\Gamma(s+\mathrm{d} s))-\mathbf{T}(\Gamma(s))}{\mathrm{d} s} \\
& =\frac{\partial \mathbf{T}(\mathbf{x})}{\partial x^{\alpha}} \frac{\mathrm{d} x^{\alpha}}{\mathrm{d} s}=\frac{\partial \mathbf{T}(\mathbf{x})}{\partial x^{\alpha}} \delta_{\alpha \beta} \frac{\mathrm{d} q_{\beta}}{\mathrm{d} s} \\
& =\frac{\partial \mathbf{T}}{\partial q_{\alpha}}\left(h_{\alpha}^{-1} \mathbf{e}_{\alpha} \cdot h_{\beta} \mathbf{e}_{\beta}\right) \frac{\mathrm{d} q_{\beta}}{\mathrm{d} s} \\
& =\left(\frac{\partial \mathbf{T}}{\partial q_{\alpha}} \otimes h_{\alpha}^{-1} \mathbf{e}_{\alpha}\right)(\mathbf{v}) \tag{57}
\end{align*}
$$

where we have used the fact that the tangent to $\Gamma$ at $\mathbf{x}$ is $h_{\beta} \mathbf{e}_{\beta}\left(\mathrm{d} q_{\beta} / \mathrm{d} s\right)$. Since this operation applies to arbitrary vectors $\mathbf{v}$, the gradient of a tensor in orthogonal curvilinear coordinates is

$$
\begin{equation*}
\operatorname{grad} \mathbf{T}=h_{\alpha}^{-1} \frac{\partial \mathbf{T}}{\partial q_{\alpha}} \otimes \mathbf{e}_{\alpha}, \quad \operatorname{Grad} \mathbf{T}=H_{\alpha}^{-1} \frac{\partial \mathbf{T}}{\partial Q_{\alpha}} \otimes \mathbf{E}_{\alpha} \tag{58}
\end{equation*}
$$

Similarly, we define the divergence of a tensor field $\mathbf{T}$ as $\operatorname{div} \mathbf{T}=\nabla \cdot \mathbf{T}$, that is

$$
\begin{equation*}
\operatorname{div} \mathbf{T}=h_{\alpha}^{-1} \mathbf{e}_{\alpha} \cdot \frac{\partial \mathbf{T}}{\partial q_{\alpha}}, \quad \operatorname{Div} \mathbf{T}=H_{\alpha}^{-1} \mathbf{E}_{\alpha} \cdot \frac{\partial \mathbf{T}}{\partial Q_{\alpha}} \tag{59}
\end{equation*}
$$

Note that we take the scalar product on the left which corresponds to the contraction on the first index of $\mathbf{T}$. Choosing Cartesian coordinates $\left\{q_{1}, q_{2}, q_{3}\right\}=\left\{x_{1}, x_{2}, x_{3}\right\}$ leads to $h_{\alpha}=1 \forall \alpha$, and the definitions (58) and (59) reduce to those of the previous section.

As an example, consider the choice of polar coordinates $\left\{q_{1}, q_{2}\right\}=\{r, \theta\}$ in the Euclidean plane. The position vector is $\mathbf{x}=r \cos \theta \mathbf{e}_{1}+r \sin \theta \mathbf{e}_{2}$, so that

$$
\begin{array}{ll}
\mathbf{e}_{r}=\frac{\partial \mathbf{x}}{\partial r}, & h_{r}=1,  \tag{60}\\
\mathbf{e}_{\theta}=\frac{1}{r} \frac{\partial \mathbf{x}}{\partial \theta}, & h_{\theta}=r .
\end{array}
$$

Hence, according to (58), the gradient of a scalar $\phi$ is

$$
\begin{equation*}
\operatorname{grad} \phi=\left(\partial_{r} \phi\right) \mathbf{e}_{r}+\frac{1}{r}\left(\partial_{\theta} \phi\right) \mathbf{e}_{\theta}, \tag{61}
\end{equation*}
$$

and we recover the usual formula of vector calculus. Similarly, if we write a second-order tensor $\mathbf{T}$ in polar representation:

$$
\begin{equation*}
\mathbf{T}=T_{r r} \mathbf{e}_{r} \otimes \mathbf{e}_{r}+T_{r \theta} \mathbf{e}_{r} \otimes \mathbf{e}_{\theta}+T_{\theta r} \mathbf{e}_{\theta} \otimes \mathbf{e}_{r}+T_{\theta \theta} \mathbf{e}_{\theta} \otimes \mathbf{e}_{\theta} \tag{62}
\end{equation*}
$$

then its divergence is the first order tensor

$$
\begin{align*}
\operatorname{div} \mathbf{T}= & \left(\frac{1}{r} \frac{\partial}{\partial r}\left(r T_{r r}\right)+\frac{1}{r} \frac{\partial T_{\theta r}}{\partial \theta}-\frac{T_{\theta \theta}}{r}\right) \mathbf{e}_{r} \\
& \left.+\left(\frac{1}{r} \frac{\partial}{\partial r}\left(r T_{r \theta}\right)+\frac{1}{r} \frac{\partial T_{\theta \theta}}{\partial \theta}+\frac{T_{\theta r}}{r}\right)\right) \mathbf{e}_{\theta} . \tag{63}
\end{align*}
$$

And, the gradient of $\mathbf{T}$ is the third order tensor

$$
\begin{aligned}
\operatorname{grad} \mathbf{T}= & \frac{\partial \mathbf{T}}{\partial r} \otimes \mathbf{e}_{r}+\frac{1}{r} \frac{\partial \mathbf{T}}{\partial \theta} \otimes \mathbf{e}_{\theta} \\
= & \left(\partial_{r} T_{r r}\right) \mathbf{e}_{r} \otimes \mathbf{e}_{r} \otimes \mathbf{e}_{r}+\left(\partial_{r} T_{r \theta}\right) \mathbf{e}_{r} \otimes \mathbf{e}_{\theta} \otimes \mathbf{e}_{r} \\
& +\left(\partial_{r} T_{\theta r}\right) \mathbf{e}_{\theta} \otimes \mathbf{e}_{r} \otimes \mathbf{e}_{r}+\left(\partial_{r} T_{\theta \theta}\right) \mathbf{e}_{\theta} \otimes \mathbf{e}_{\theta} \otimes \mathbf{e}_{r} \\
& +\left(\frac{1}{r}\left(\partial_{\theta} T_{r r}\right)-T_{r \theta}-T_{\theta r}\right) \mathbf{e}_{r} \otimes \mathbf{e}_{r} \otimes \mathbf{e}_{\theta} \\
& +\left(\frac{1}{r}\left(\partial_{\theta} T_{\theta r}\right)+T_{r r}-T_{\theta \theta}\right) \mathbf{e}_{\theta} \otimes \mathbf{e}_{r} \otimes \mathbf{e}_{\theta} \\
& +\left(\frac{1}{r}\left(\partial_{\theta} T_{r \theta}\right)+T_{r r}-T_{\theta \theta}\right) \mathbf{e}_{r} \otimes \mathbf{e}_{\theta} \otimes \mathbf{e}_{\theta} \\
& +\left(\frac{1}{r}\left(\partial_{\theta} T_{\theta \theta}\right)+T_{r \theta}+T_{\theta r}\right) \mathbf{e}_{\theta} \otimes \mathbf{e}_{\theta} \otimes \mathbf{e}_{\theta} .
\end{aligned}
$$

### 2.4 Derivatives of scalar functions of tensors

We will also consider scalar functions of tensors and their derivatives with respect to a tensor. Let $\mathbf{A}, \mathbf{B}, \mathbf{C}$ be second-order tensors with Cartesian components in the basis $\left\{\mathbf{e}_{1}, \mathbf{e}_{2}, \mathbf{e}_{3}\right\}$ given by $A_{i j}, B_{i j}, C_{i j}$. Let $F=F(\mathbf{A})$ be a scalar function of $\mathbf{A}$. The derivative of the scalar function $F$ with respect to the tensor $\mathbf{A}$ is a tensor with Cartesian components

$$
\begin{equation*}
\left(\frac{\partial F(\mathbf{A})}{\partial \mathbf{A}}\right)_{i j}=\frac{\partial F(\mathbf{A})}{\partial A_{j i}} . \tag{64}
\end{equation*}
$$

That is

$$
\begin{equation*}
\frac{\partial F(\mathbf{A})}{\partial \mathbf{A}}=\frac{\partial F}{\partial A_{j i}} \mathbf{e}_{i} \otimes \mathbf{e}_{j} . \tag{65}
\end{equation*}
$$

Now, let $\mathbf{A}=\mathbf{B C}$ and consider the derivative of $F$ with respect to $\mathbf{B}$. In components, we have

$$
\begin{align*}
\left(\frac{\partial F(\mathbf{A})}{\partial \mathbf{B}}\right)_{i j} & =\frac{\partial F\left(B_{k l} C_{l m}\right)}{\partial B_{j i}} \\
& =\frac{\partial A_{k m}}{\partial B_{j i}} \frac{\partial F(\mathbf{A})}{\partial A_{k m}}=\frac{\partial B_{k l} C_{l m}}{\partial B_{j i}} \frac{\partial F(\mathbf{A})}{\partial A_{k m}} \\
& =\delta_{j k} \delta_{i l} C_{l m} \frac{\partial F(\mathbf{A})}{\partial A_{k m}}=C_{i m} \frac{\partial F(\mathbf{A})}{\partial A_{j m}} \\
& =C_{i m}\left(\frac{\partial F(\mathbf{A})}{\partial \mathbf{A}}\right)_{m j} \tag{66}
\end{align*}
$$

So that, in general, we can write

$$
\begin{equation*}
\frac{\partial F(\mathbf{A})}{\partial \mathbf{B}}=\mathbf{C} \frac{\partial F(\mathbf{A})}{\partial \mathbf{A}} \tag{67}
\end{equation*}
$$

Other useful identities are Jacobi's relations for the first and second derivative of a nonvanishing determinant,

$$
\begin{align*}
& \frac{\partial}{\partial \mathbf{A}}(\operatorname{det}(\mathbf{A}))=\operatorname{det}(\mathbf{A}) \mathbf{A}^{-1}  \tag{68}\\
& \operatorname{tr}\left[\left(\frac{\partial}{\partial \mathbf{A}} \frac{\partial}{\partial \mathbf{A}} \operatorname{det} \mathbf{A}\right) \mathbf{B}\right]=\operatorname{det}(\mathbf{A})\left[\operatorname{tr}\left(\mathbf{A}^{-1} \mathbf{B}\right) \mathbf{A}^{-1}-\mathbf{A}^{-1} \mathbf{B} \mathbf{A}^{-1}\right] \tag{69}
\end{align*}
$$

where the contraction $\operatorname{tr}(\mathcal{L A})$ of a second-order tensor $\mathbf{A}$ with a fourth-order tensor $\mathcal{L}$ is defined by $(\operatorname{tr}(\mathcal{L} \mathbf{A}))_{i j}=\mathcal{L}_{i j k l} A_{l k}$. In the last equality, the derivative of the inverse of a tensor by itself defines a fourth-order tensor such that

$$
\begin{equation*}
\operatorname{tr}\left[\left(\frac{\partial}{\partial \mathbf{A}} \mathbf{A}^{-1}\right) \mathbf{B}\right]=-\mathbf{A}^{-1} \mathbf{B} \mathbf{A}^{-1} \tag{70}
\end{equation*}
$$

If $\mathbf{A}=\mathbf{A}(t)$, the derivative of a scalar function of $\mathbf{A}$ with respect to a parameter $t$ can be obtained by the chain rule. That is,

$$
\begin{equation*}
\frac{\mathrm{d}}{\mathrm{~d} t} F(\mathbf{A})=\operatorname{tr}\left(\frac{\partial F(\mathbf{A})}{\partial \mathbf{A}} \frac{\mathrm{d} \mathbf{A}}{\mathrm{~d} t}\right) \tag{71}
\end{equation*}
$$

As an example, the first Jacobi relation (68) can be used to compute the derivative of the determinant of a tensor with respect to a parameter

$$
\begin{equation*}
\frac{\mathrm{d}}{\mathrm{~d} t}(\operatorname{det}(\mathbf{A}))=\operatorname{tr}\left(\frac{\partial}{\partial \mathbf{A}}(\operatorname{det}(\mathbf{A})) \frac{\mathrm{d} \mathbf{A}}{\mathrm{~d} t}\right)=\operatorname{det}(\mathbf{A}) \operatorname{tr}\left(\mathbf{A}^{-1} \frac{\mathrm{~d} \mathbf{A}}{\mathrm{~d} t}\right) . \tag{72}
\end{equation*}
$$

### 2.5 The deformation gradient

The central geometric object of nonlinear elasticity that describes locally relative deformations is the deformation gradient, obtained as the spatial derivative of the mapping $\chi$. Given a vector $\mathbf{x}=x_{i}(\mathbf{X}) \mathbf{e}_{i}$, the deformation gradient tensor is $\mathbf{F}=\operatorname{Grad} \boldsymbol{\chi}$. In Cartesian coordinates, it reads

$$
\begin{equation*}
\mathbf{F}=\frac{\partial}{\partial X_{j}}\left(x_{i} \mathbf{e}_{i}\right) \otimes \mathbf{E}_{j}=\frac{\partial x_{i}}{\partial X_{j}} \mathbf{e}_{i} \otimes \mathbf{E}_{j} \equiv F_{i j} \mathbf{e}_{i} \otimes \mathbf{E}_{j} . \tag{73}
\end{equation*}
$$

Note that the bases in which the gradient is taken are mixed. Geometrically, $\mathbf{F}$ is a linear map that transforms a vector $\mathbf{v}$ in the tangent space $T_{p} \mathcal{B}_{0}$ at a material point $p \in \mathcal{B}_{0}$ to a vector $\mathbf{F v}$ in the tangent space $T_{p} \mathcal{B}$ at the same material point but in the current configuration (see Figure (4).


Figure 4: The deformation gradient maps vectors on the tangent space at a material point in the initial configuration to vectors in the tangent space in the current configuration at the same material point.

We can also express the deformation gradient in curvilinear coordinates. Let $\left\{q_{1}, q_{2}, q_{3}\right\}$ and $\left\{Q_{1}, Q_{2}, Q_{3}\right\}$ be the coordinates in the reference and current configuration, respectively. The deformation $\boldsymbol{\chi}$ in the bases $\left\{\mathbf{e}_{1}, \mathbf{e}_{2}, \mathbf{e}_{3}\right\}$ and $\left\{\mathbf{E}_{1}, \mathbf{E}_{2}, \mathbf{E}_{3}\right\}$ is given by $q_{\alpha}=$ $q_{\alpha}\left(Q_{1}, Q_{2}, Q_{3}\right), \alpha=1,2,3$. Then, following the definition of the gradient (58), we have

$$
\begin{align*}
\operatorname{Grad} \mathbf{x} & =H_{\beta}^{-1} \frac{\partial \mathbf{x}}{\partial Q_{\beta}} \otimes \mathbf{E}_{\beta} \\
& =H_{\beta}^{-1} \frac{\partial \mathbf{x}}{\partial q_{\alpha}} \frac{\partial q_{\alpha}}{\partial Q_{\beta}} \otimes \mathbf{E}_{\beta}  \tag{74}\\
& =\frac{h_{\alpha}}{H_{\beta}} \frac{\partial q_{\alpha}}{\partial Q_{\beta}} \mathbf{e}_{\alpha} \otimes \mathbf{E}_{\beta}, \tag{75}
\end{align*}
$$

where we used $\frac{\partial \mathbf{x}}{\partial q_{\beta}}=h_{\beta} \mathbf{e}_{\beta}$ and the scale factors $h_{\alpha}, H_{\beta}$ given by 55 . Then, we conclude that the matrix of coefficients of the deformation gradient $\mathbf{F}=F_{\alpha \beta} \mathbf{e}_{\alpha} \otimes \mathbf{E}_{\beta}$ is

$$
\begin{equation*}
[\mathbf{F}]_{\alpha \beta}=F_{\alpha \beta}=\frac{h_{\alpha}}{H_{\beta}} \frac{\partial q_{\alpha}}{\partial Q_{\beta}} \quad \text { (no summation on indices). } \tag{76}
\end{equation*}
$$

As an example, we consider the deformation of a ring in a plane to another ring shown in Figure 5. In the two sets of polar coordinates $\left\{q_{1}, q_{2}\right\}=\{r, \theta\}$ and $\left\{Q_{1}, Q_{2}\right\}=\{R, \Theta\}$, this deformation is given by

$$
\begin{equation*}
r=f(R), \quad \theta=\Theta . \tag{77}
\end{equation*}
$$



Figure 5: Deformation of a ring into another ring in the plane.
For these coordinates, we have $h_{r}=H_{R}=1$ and $h_{\theta}=r, H_{\Theta}=R$, and the deformation gradient is

$$
[F]=\left[\begin{array}{cc}
\frac{h_{r}}{H_{R}} \frac{\partial r}{\partial R} & \frac{h_{r}}{H_{\Theta}} \frac{\partial r}{\partial \Theta}  \tag{78}\\
\frac{h_{\theta}}{H_{R}} \frac{\partial \theta}{\partial R} & \frac{h_{\theta}}{H_{\Theta}} \frac{\partial \theta}{\partial \Theta}
\end{array}\right]=\left[\begin{array}{cc}
f^{\prime}(R) & 0 \\
0 & \frac{f(R)}{R}
\end{array}\right],
$$

that is,

$$
\begin{equation*}
\mathbf{F}=f^{\prime}(R) \mathbf{e}_{r} \otimes \mathbf{E}_{R}+\frac{r}{R} \mathbf{e}_{\theta} \otimes \mathbf{E}_{\Theta} . \tag{79}
\end{equation*}
$$

### 2.6 Volume, surface, and line elements

The deformation of a body may change the relative size of material elements. First, consider a set of material points in the reference configuration $\Omega_{0} \subseteq \mathcal{B}_{0}$. This set evolves in time and is deformed to a new volume $\Omega \subseteq \mathcal{B}$ in the current configuration. The new volume is related to the reference volume by

$$
\begin{equation*}
\int_{\Omega} \mathrm{d} v=\int_{\Omega_{0}} J \mathrm{~d} V \tag{80}
\end{equation*}
$$

where

$$
\begin{equation*}
J(\mathbf{X}, t)=\operatorname{det} \mathbf{F}(\mathbf{X}, t) \tag{81}
\end{equation*}
$$

is the Jacobian of the transformation that represents the local change of volume, that is the image of an infinitesimal volume element $\mathrm{d} v$ at a material point $p$ is

$$
\begin{equation*}
\mathrm{d} v=J \mathrm{~d} V, \tag{82}
\end{equation*}
$$

as shown in Figure 6 .
Since volume elements are positive and cannot vanish in a deformation, we require that $J>0$ in all deformations, which ensures the invertibility of the deformation gradient. That is, there exists a second-order tensor $\mathbf{F}^{-1}$ mapping vectors from $\mathcal{B}$ to $\mathcal{B}$, such that $\mathbf{F}^{-1} \mathbf{F}=\mathbf{1}$. Explicitly, this tensor is

$$
\begin{equation*}
\mathbf{F}^{-1}=\operatorname{grad} \mathbf{X}(\mathbf{x}, t) \tag{83}
\end{equation*}
$$

A transformation that conserves locally every volume element, that is $J=1$, is said to be isochoric.


Figure 6: Transformation of volume: In a deformation, an infinitesimal volume element $\mathrm{d} V$ at a material point evolves by a factor $J$ to a new volume $\mathrm{d} v=J \mathrm{~d} V$.

Similarly, we can define an area element by considering a material area element normal to a given vector $\mathbf{N}$. Then, it is standard to show [118] that the surface integral transforms as

$$
\begin{equation*}
\int_{\partial \Omega} \mathbf{n} \mathrm{d} a=\int_{\partial \Omega_{0}} J \mathbf{F}^{-\mathrm{T}} \mathbf{N} \mathrm{~d} A, \tag{84}
\end{equation*}
$$

where $\mathbf{n}(\mathbf{x}, t)$ and $\mathbf{N}(\mathbf{X}, t)$ are outward unit normals, $\mathrm{d} A$ and $\mathrm{d} a$ are the area elements at a given point as shown in Figure 7. That is, an infinitesimal element of area defined in


Figure 7: Transformation of area: In a deformation, an infinitesimal area is transformed according to Nanson's rule.
the reference configuration by a normal $\mathbf{N}$ and surface area $\mathrm{d} A$ is transformed into another element of area in the current configuration defined by a vector $\mathbf{n}$ with area $\mathrm{d} a$ and related to the reference one by Nanson's formula:

$$
\begin{equation*}
\mathbf{n} \mathrm{d} a=J \mathbf{F}^{-\mathrm{T}} \mathbf{N} \mathrm{~d} A . \tag{85}
\end{equation*}
$$

Finally, consider a local infinitesimal vector $\mathrm{d} \mathbf{X}$ tangent to a material line in $\mathcal{B}_{0}$ at a material point $p$, then its image is $\mathrm{d} \mathbf{x}=\mathbf{F d} \mathbf{X}$ as shown in Figure 8. If $\mathbf{M}$ is the unit vector along $\mathrm{d} \mathbf{X}$ then

$$
\begin{equation*}
\mathrm{d} \mathbf{X}=\mathbf{M} \mathrm{d} S \quad \text { and } \quad \mathrm{d} \mathbf{x}=\mathbf{m} \mathrm{d} s \tag{86}
\end{equation*}
$$



Figure 8: Transformation of material lines: In a deformation, an infinitesimal line element is mapped by the deformation gradient to a new line element.
where $\mathrm{d} S=|\mathrm{d} \mathbf{X}|$ and $\mathrm{d} s=|\mathrm{d} \mathbf{x}|$. This last identity implies that $\mathbf{m} \mathrm{d} s=\mathbf{F M} \mathrm{d} S$. Now take the norm of each side:

$$
\begin{equation*}
|\mathrm{d} s|^{2}=(\mathbf{F M} \cdot \mathbf{F M})|\mathrm{d} S|^{2}=\left(\mathbf{F}^{\top} \mathbf{F M}\right) \cdot \mathbf{M}|\mathrm{d} S|^{2} . \tag{87}
\end{equation*}
$$

Equivalently, we can write

$$
\begin{equation*}
\frac{\mathrm{D} s}{\mathrm{D} S}=\sqrt{\left(\mathbf{F}^{\top} \mathbf{F M}\right) \cdot \mathbf{M}} \tag{88}
\end{equation*}
$$

where $\mathrm{d} s / \mathrm{d} S$ is the change of length of a material line in the direction M. This last relationship can be used to define the stretch, $\lambda=\lambda(\mathbf{M})$ of a material line in the direction $\mathbf{M}$ as

$$
\begin{equation*}
\lambda(\mathbf{M})=\sqrt{\left(\mathbf{F}^{\top} \mathbf{F M}\right) \cdot \mathbf{M}} \tag{89}
\end{equation*}
$$

Since we are interested in characterizing elastic materials, we need to characterize deformations which change the relative length of line elements. Therefore, stretches provides a natural measure of strain in a material. A material is said to be unstrained in the direction $\mathbf{M}$ if and only if $\lambda(\mathbf{M})=1$.

In (87), we see the appearance of an important tensor in the description of strain for a three-dimensional body, namely the right Cauchy-Green tensor

$$
\begin{equation*}
\mathbf{C}=\mathbf{F}^{\top} \mathbf{F} \tag{90}
\end{equation*}
$$

A material is unstrained at a given point if it is unstrained in all directions. That is $\lambda(\mathbf{M})=$ $1 \forall \mathbf{M}$. In terms of the right Cauchy-Green tensor, this implies $\mathbf{C}=\mathbf{1}$.

Geometrically, the tensor $\mathbf{C}$ can be interpreted as a metric on $\mathcal{B}$ as it provides a way to measure distances and angles on the new body.

### 2.7 Polar decomposition theorem

The action of the deformation gradient $\mathbf{F}$ on a vector $\mathbf{M}$ can be decomposed into a rotation about a direction $\mathbf{m}$, followed by a stretch of size $\lambda(\mathbf{M})$. This decomposition into a stretch and a rotation can be applied directly to the deformation gradient through the polar decomposition theorem stating that: For a second-order tensor $\mathbf{F}$ such that $\operatorname{det} \mathbf{F}>0$, there exist unique positive definite symmetric tensors $\mathbf{U}, \mathbf{V}$ and a unique proper orthogonal tensor $\mathbf{R}$ such that,

$$
\mathbf{F}=\mathbf{R} \mathbf{U}=\mathbf{V R} .
$$

The positive symmetric tensors $\mathbf{U}$ and $\mathbf{V}$ are called the left and right stretch tensors, respectively. Their squares can easily be obtained from $\mathbf{F}$ as follows

$$
\begin{array}{ll}
\mathbf{F}^{\top} \mathbf{F}=\mathbf{U}^{2} \equiv \mathbf{C}, & \text { the right Cauchy-Green tensor, } \\
\mathbf{F F}^{\top}=\mathbf{V}^{2} \equiv \mathbf{B}, & \text { the left Cauchy-Green tensor } .
\end{array}
$$

Since $\mathbf{V}=\mathbf{R U R}^{\boldsymbol{\top}}$, $\mathbf{U}$ and $\mathbf{V}$ have the same eigenvalues $\left\{\lambda_{1}, \lambda_{2}, \lambda_{3}\right\}$. The principal stretches, can be obtained conveniently as the square roots of the eigenvalues of either $\mathbf{C}$ or $\mathbf{B}$. Note that since $\mathbf{U}$ and $\mathbf{V}$ are positive symmetric, the principal stretches are positive and real and the corresponding eigenvectors $\left\{\mathbf{u}_{1}, \mathbf{u}_{2}, \mathbf{u}_{3}\right\}$ and $\left\{\mathbf{v}_{1}, \mathbf{v}_{2}, \mathbf{v}_{3}\right\}$ of $\mathbf{U}$ and $\mathbf{V}$ form two bases. Therefore, the stretch tensors can be written as

$$
\begin{align*}
\mathbf{U} & =\sum_{i=1}^{3} \lambda_{i} \mathbf{u}_{i} \otimes \mathbf{u}_{i},  \tag{91}\\
\mathbf{V} & =\sum_{i=1}^{3} \lambda_{i} \mathbf{v}_{i} \otimes \mathbf{v}_{i} \tag{92}
\end{align*}
$$

Since $J=\operatorname{det} \mathbf{F}=\operatorname{det}(\mathbf{R U})=(\operatorname{det} \mathbf{R})(\operatorname{det} \mathbf{U})=\operatorname{det} \mathbf{U}=\operatorname{det} \mathbf{V}$, we have $J=\lambda_{1} \lambda_{2} \lambda_{3}$ and we can re-write $\mathbf{F}$ as

$$
\begin{equation*}
\mathbf{F}=\sum_{i=1}^{3} \lambda_{i} \mathbf{v}_{i} \otimes \mathbf{u}_{i} . \tag{93}
\end{equation*}
$$

### 2.8 Velocity, acceleration, and velocity gradient

The motion associated with a deformation $\mathbf{x}=\boldsymbol{\chi}(\mathbf{X}, t), \mathbf{X} \in \mathcal{B}_{0}$, is associated with change in time $t$. Since $\mathbf{X}$ is the position of a material point, the velocity and acceleration of this material point are, respectively,

$$
\begin{align*}
& \mathbf{v}(\mathbf{x}, t)=\frac{\partial}{\partial t} \chi(\mathbf{X}, t) \equiv \dot{\chi}(\mathbf{X}, t)  \tag{94}\\
& \mathbf{a}(\mathbf{x}, t)=\frac{\partial^{2}}{\partial t^{2}} \boldsymbol{\chi}(\mathbf{X}, t) \equiv \ddot{\chi}(\mathbf{X}, t) \tag{95}
\end{align*}
$$

In general, we define the material time derivative $\mathrm{D} / \mathrm{D} t$ as a total time derivative with respect to a fixed material coordinate $\mathbf{X}$. For a scalar field $\phi=\phi(\mathbf{x}, t)$, the material derivative is

$$
\begin{equation*}
\left.\frac{\mathrm{D} \phi}{\mathrm{D} t} \equiv \frac{\mathrm{~d} \phi}{\mathrm{~d} t}\right|_{\mathbf{X}} \equiv \dot{\phi} \equiv \frac{\partial \phi}{\partial t}+(\operatorname{grad} \phi) \cdot \mathbf{v} \tag{96}
\end{equation*}
$$

and we define the derivative of a vector field $\mathbf{u}=\mathbf{u}(\mathbf{x}, t)$ similarly as

$$
\begin{equation*}
\frac{\mathrm{D} \mathbf{u}}{\mathrm{D} t}=\frac{\partial \mathbf{u}}{\partial t}+(\operatorname{grad} \mathbf{u}) \mathbf{v} . \tag{97}
\end{equation*}
$$

Another important kinematic quantity is the velocity gradient tensor, defined as

$$
\begin{equation*}
\mathbf{L}=\operatorname{grad} \mathbf{v}, \quad L_{i j}=\frac{\partial v_{i}}{\partial x_{j}}, \quad \mathbf{L}=L_{i j} \mathbf{e}_{i} \otimes \mathbf{e}_{j} \tag{98}
\end{equation*}
$$

Since, in general the chain rule gives $\operatorname{Grad} \mathbf{u}=(\operatorname{grad} \mathbf{u}) \mathbf{F}$, we have

$$
\begin{equation*}
\operatorname{Grad} \mathbf{v}=(\operatorname{grad} \mathbf{v}) \mathbf{F}=\mathbf{L F}, \tag{99}
\end{equation*}
$$

but also,

$$
\begin{equation*}
\operatorname{Grad} \mathbf{v}=\operatorname{Grad} \dot{\mathbf{x}}=\frac{\partial}{\partial t} \operatorname{Grad} \mathbf{x}=\frac{\partial \mathbf{F}}{\partial t}=\dot{\mathbf{F}}, \tag{100}
\end{equation*}
$$

so that the evolution of the deformation gradient can be expressed in terms of the velocity gradient tensor as

$$
\begin{equation*}
\dot{\mathbf{F}}=\mathbf{L F} . \tag{101}
\end{equation*}
$$

Taking the determinant of each side of this last equality and applying Jacobi's formula (72) for the derivative of the determinant of a nonsingular matrix

$$
\begin{equation*}
\frac{\partial}{\partial t} \operatorname{det} \mathbf{F}=(\operatorname{det} \mathbf{F}) \operatorname{tr}\left(\mathbf{F}^{-1} \dot{\mathbf{F}}\right)=(\operatorname{det} \mathbf{F}) \operatorname{tr}(\mathbf{L}) \tag{102}
\end{equation*}
$$

leads to an equation for the evolution of the determinant:

$$
\begin{equation*}
\dot{J}=J \operatorname{tr}(\mathbf{L})=J \operatorname{div} \mathbf{v} \tag{103}
\end{equation*}
$$

In particular, since $J \neq 0$, we note the well-known relationship between conservation of volume during motion and the vanishing of the divergence of the velocity:

$$
\begin{equation*}
\operatorname{div} \mathbf{v}=0 \quad \Longleftrightarrow \quad \dot{J}=0 \tag{104}
\end{equation*}
$$

### 2.9 Examples of deformation

### 2.9.1 Homogeneous deformation

$$
\begin{equation*}
\mathbf{x}=\mathbf{F X}+\mathbf{x}_{0}, \quad \mathbf{F}, \mathbf{x}_{0} \text { constant } \tag{105}
\end{equation*}
$$

- Simple elongation

$$
\begin{equation*}
\mathbf{F}=\mathbf{U}=\lambda_{1} \mathbf{U}^{(1)} \otimes \mathbf{U}^{(1)}+\lambda_{2}\left(\mathbf{U}^{(2)} \otimes \mathbf{U}^{(2)}+\mathbf{U}^{(3)} \otimes \mathbf{U}^{(3)}\right) \tag{106}
\end{equation*}
$$

- Dilation

$$
\begin{equation*}
\mathbf{F}=\lambda \mathbb{1} \tag{107}
\end{equation*}
$$

- Simple shear


$$
\begin{equation*}
x_{1}=X_{1}+\gamma X_{2}, \quad x_{2}=X_{2}, \quad x_{3}=X_{3}, \tag{108}
\end{equation*}
$$

which imply (homework),

$$
\Longrightarrow \quad \mathbf{F}=\left[\begin{array}{lll}
1 & \gamma & 0  \tag{109}\\
0 & 1 & 0 \\
0 & 0 & 1
\end{array}\right], \quad \mathbf{U}^{2}=\left[\begin{array}{ccc}
1 & \gamma & 0 \\
\gamma & 1+\gamma^{2} & 0 \\
0 & 0 & 1
\end{array}\right]
$$

### 2.9.2 Inflation of a spherical shell

We consider the symmetric deformation of a spherical shell with radii $R=A$ and $R=B$ in the initial configuration into a spherical shell of radii $r=a$ and $r=b$ in the current configuration. We consider the possibility where both $A$ and $a$ vanish (a sphere under load); the case where $A=0$ but $a>0$ (the cavitation of a sphere); as well as the case $A>0$ and $a=0$ (the anti-cavitation of a spherical shell). Under the deformation, the shell expands and any point located at $(R, \Theta, \Phi)$ in the reference configuration is moved to the point $(r, \Theta, \Phi)$ where $r=r(R)$ as shown in Figure 9. Explicitly, the deformation, $\mathbf{x}=\boldsymbol{\chi}(\mathbf{X})$, reads

$$
\begin{equation*}
r=r(R), \quad \theta=\Theta, \quad \phi=\Phi \tag{110}
\end{equation*}
$$

so that the position vectors are, respectively,

$$
\begin{equation*}
\mathbf{X}=R \mathbf{E}_{R}, \quad \mathbf{x}=r(R) \mathbf{e}_{r}=\frac{r(R)}{R} \mathbf{X} . \tag{111}
\end{equation*}
$$

Due to the symmetry of the deformation, we can identify the basis vectors so that $\mathbf{E}_{R}=$ $\mathbf{e}_{r}, \mathbf{E}_{\Theta}=\mathbf{e}_{\theta}, \mathbf{E}_{\Phi}=\mathbf{e}_{\phi}$.


Figure 9: Radial deformation of a shell with inner and outer radii $A$ and $B$ to a shell with radii $a$ and $b$.

To compute the deformation gradient, we use the method described in Section 2.5. We have two sets the two sets of spherical coordinates $\left\{q_{\alpha}\right\}=\{r, \theta, \phi\}$ and $\left\{Q_{\alpha}\right\}=\{R, \Theta, \Phi\}$. For these coordinates, the scale factors, defined by (55), are

$$
\begin{align*}
& h_{r}=1, \quad H_{R}=1,  \tag{112}\\
& h_{\theta}=r, \quad H_{\Theta}=R,  \tag{113}\\
& h_{\phi}=r \sin \theta, \quad H_{\Phi}=R \sin \Theta . \tag{114}
\end{align*}
$$

Following Equation (76), the deformation gradient is

$$
\mathbf{F}=r^{\prime} \mathbf{e}_{r} \otimes \mathbf{e}_{r}+\frac{r}{R} \mathbf{e}_{\theta} \otimes \mathbf{e}_{\theta}+\frac{r}{R} \mathbf{e}_{\phi} \otimes \mathbf{e}_{\phi},
$$

which we write

$$
\begin{equation*}
\mathbf{F}=\operatorname{diag}\left(r^{\prime}, r / R, r / R\right) \tag{115}
\end{equation*}
$$

where the primes denote derivatives with respect to $R$.
Note if we only consider isochoric deformation then $\operatorname{det} \mathbf{F}=1$, which implies

$$
\begin{equation*}
r^{\prime}\left(\frac{r}{R}\right)^{2}=1 \quad \Longrightarrow \quad r^{\prime} r^{2}=R^{2} \quad \Longleftrightarrow \quad \frac{1}{3} \frac{\mathrm{D}\left(r^{3}\right)}{\mathrm{D} R}=R^{2} \quad \Longrightarrow \quad r^{3}=R^{3}+C \tag{116}
\end{equation*}
$$

Since $r(a)=A, r(b)=B$,

$$
\begin{equation*}
C=b^{3}-B^{3}=a^{3}-A^{3} \quad \Longrightarrow \quad a^{3}=b^{3}-B^{3}+A^{3} \quad \Longrightarrow \quad r=\sqrt{a^{3}-A^{3}+R^{3}} \tag{117}
\end{equation*}
$$

This is a one-parameter family of solutions.

## 3 Conservation Laws, Stress, and Dynamics

Overview We use basic physical principles to derive local equations for the evolution of mass and stress in space. The requirement for localising the balance of linear momentum naturally leads to the definition of the Cauchy stress tensor.

We have obtained a complete description of the deformation of a body. Starting with a mapping $\chi$, we defined the deformation gradient $\mathbf{F}$. This tensor contains all information on relative deformation of a body, such as local changes of volume, area, and stretch. It was used to define secondary quantities, such as the left and right Cauchy-Green tensor, B and $\mathbf{C}$, that contain information on the strain developed during a deformation. Now that we have a complete kinematic description of the body, we can define physical fields at each point on the body and use fundamental laws of physics to find local relationship between these fields.

The governing equations of continuum mechanics are obtained by considering the local balance of physical quantities: mass, linear momentum, angular momentum, and energy. The traditional approach to derive local laws consists in stating a balance law on an arbitrary subset of the body and, under suitable conditions, obtaining local relationships between physical quantities expressed as differential equations. We illustrate this process first with the balance of mass.

### 3.1 Balance of mass

To describe the properties and response of a material, we attach physical quantities at each point of the body $B$. First, we define a scalar field $\rho=\rho(\mathbf{x}, t)$, the volume density (mass per unit current volume) at each point of the body in the current configuration and assume that the mass of any subset of the body $\Omega \subseteq \mathcal{B}$ is conserved in time, that is

$$
\begin{equation*}
\frac{\mathrm{d}}{\mathrm{~d} t} \int_{\Omega} \rho(\mathbf{x}, t) \mathrm{d} v=0 \tag{118}
\end{equation*}
$$

The problem here is that the position of a material subset $\Omega$ evolves with time, and the time derivative cannot be directly applied to the integrand. Therefore, we first map the integral to the reference configuration

$$
\begin{equation*}
\frac{\mathrm{d}}{\mathrm{~d} t} \int_{\Omega_{0}} \rho(\mathbf{x}(\mathbf{X}, t), t) J \mathrm{~d} V=0 \tag{119}
\end{equation*}
$$

where we have used the transformation of a volume element 82).
Second, since the domain $\Omega_{0}$ is fixed, we can write

$$
\begin{equation*}
\frac{\mathrm{d}}{\mathrm{~d} t} \int_{\Omega_{0}} J \rho(\mathbf{x}, t) \mathrm{d} V=\int_{\Omega_{0}} \frac{\partial}{\partial t}(J \rho) \mathrm{d} V=0 . \tag{120}
\end{equation*}
$$

Third, since we wish to obtain a balance law in the current configuration, we map the integral back, that is

$$
\begin{equation*}
\int_{\Omega_{0}} \frac{\partial}{\partial t}(J \rho) \mathrm{d} V=\int_{\Omega} \frac{\partial}{\partial t}(J \rho) J^{-1} \mathrm{~d} v=\int_{\Omega}(\dot{\rho}+\rho \operatorname{div} \mathbf{v}) \mathrm{d} v=0 \tag{121}
\end{equation*}
$$

where we have used 103).
Fourth, assuming that the integrand is continuous, the vanishing of an integral on an arbitrary domain implies that it vanishes pointwise, which leads to the usual continuity equation for the evolution of density in the current configuration 60]

$$
\begin{equation*}
\dot{\rho}+\rho \operatorname{div} \mathbf{v}=0 \tag{122}
\end{equation*}
$$

The procedures of (i) mapping an integral relationship between configurations and (ii) localizing this relationship to obtain a local differential equation is a two-step process called Maxwell transport and the localization procedure, respectively.

In the first step, integrals in the current configuration are transformed into integrals in the initial configuration that are expressed on a fixed domain. In this configuration, the balance law can be written as a single integral over a domain. Once this expression has been obtained, the integral can be mapped back to the current configuration.

In the second step, a local differential equation is obtained from the integral by assuming that it holds on an arbitrary subset and that the integrand is continuous.

Note that the localization procedure can be also applied directly to the first integral appearing in (121). That is

$$
\begin{equation*}
\frac{\partial}{\partial t}(J \rho)=0 \tag{123}
\end{equation*}
$$

If we define the reference density $\rho_{0}(\mathbf{X}, t)=J(\mathbf{X}, t) \rho(\mathbf{x}(\mathbf{X}, t), t)$, then the mass conservation in the reference configuration is simply

$$
\begin{equation*}
\frac{\partial}{\partial t} \rho_{0}=0 \tag{124}
\end{equation*}
$$

### 3.1.1 Transport formulas

We will be making systematic use of Maxwell transport to obtain balance laws. It is therefore important to obtain general transport relationships for any scalar $\phi$ or vector field $\mathbf{u}$ associated with the moving body in the current configuration. Indeed, following the same steps as in (119)-121), we obtain [120] the useful transport formulae:

$$
\begin{align*}
& \frac{\mathrm{d}}{\mathrm{~d} t} \int_{\Omega} \phi \mathrm{d} v=\int_{\Omega}[\dot{\phi}+(\operatorname{div} \mathbf{v}) \phi] \mathrm{d} v  \tag{125}\\
& \frac{\mathrm{~d}}{\mathrm{~d} t} \int_{\Omega} \mathbf{u} \mathrm{d} v=\int_{\Omega}[\dot{\mathbf{u}}+(\operatorname{div} \mathbf{v}) \mathbf{u}] \mathrm{d} v \tag{126}
\end{align*}
$$

where $\Omega \subseteq \mathcal{B}$ is an arbitrary subset.

### 3.2 Balance of linear momentum

The balance of linear momentum expresses the fundamental relationship between the rate of change of linear momentum of a body as a result of the force applied to the body. When applied to a rigid body, it simply leads to Newton's second law. However, in the case of a deformable body, the body also experiences internal forces that need to be taken into account.

In the current configuration, the total linear momentum on any part of the body $\Omega \subseteq \mathcal{B}$ is simply

$$
\begin{equation*}
\int_{\Omega} \rho(\mathbf{x}, t) \mathbf{v}(\mathbf{x}, t) \mathrm{d} v \tag{127}
\end{equation*}
$$

where $\rho(\mathbf{x}, t)$ is the density and $\mathbf{v}(\mathbf{x}, t)$ the velocity of a point at $(\mathbf{x}, t)$.
The total force acting on a point $\mathbf{x} \in \Omega$ includes a body-force density $\mathbf{b}$, representing the contributions of external forces and a contact-force density $\mathbf{t}_{n}$, representing the force per unit area resulting in contact. Therefore, the total force acting on $\Omega$ is

$$
\begin{equation*}
\int_{\Omega} \rho(\mathbf{x}, t) \mathbf{b}(\mathbf{x}, t) \mathrm{d} v+\int_{\partial \Omega} \mathbf{t}_{n} \mathrm{~d} a . \tag{128}
\end{equation*}
$$

Euler's first law of motion then states that the rate of change of the linear momentum on any part of the body $\Omega \subseteq \mathcal{B}$ is equal to the sum of the forces acting on $\Omega$ [146]. Therefore, in our context, this law reads

$$
\begin{equation*}
\underbrace{\frac{\mathrm{d}}{\mathrm{~d} t} \int_{\Omega} \rho(\mathbf{x}, t) \mathbf{v}(\mathbf{x}, t) \mathrm{d} v}_{\text {rate of change of linear momentum }}=\underbrace{\int_{\Omega} \rho(\mathbf{x}, t) \mathbf{b}(\mathbf{x}, t) \mathrm{d} v+\int_{\partial \Omega} \mathbf{t}_{n} \mathrm{~d} a}_{\text {sum of body and contact forces }} . \tag{129}
\end{equation*}
$$

We apply the transport formula (126) by mapping the rate of linear momentum to the reference configuration

$$
\begin{align*}
\frac{\mathrm{d}}{\mathrm{~d} t} \int_{\Omega} \rho \mathbf{v} \mathrm{d} v & =\frac{\mathrm{d}}{\mathrm{~d} t} \int_{\Omega_{0}} \rho \mathbf{v} J \mathrm{~d} V=\int_{\Omega_{0}} \frac{\mathrm{~d}}{\mathrm{~d} t}(\rho \mathbf{v} J) \mathrm{d} V,  \tag{130}\\
& =\int_{\Omega_{0}}(\rho \dot{\mathbf{v}}+\underbrace{\dot{\rho} \mathbf{v}+\rho \mathbf{v} d i \mathbf{v} \mathbf{v}}_{=0, \text { per continuity }}) J \mathrm{~d} V,  \tag{131}\\
& =\int_{\Omega} \rho \dot{\mathbf{v}} \mathrm{d} v, \tag{132}
\end{align*}
$$

where we have used the identity (103).
To apply the localization procedure, we need to express all the quantities as a single integral. However, the last integral in (129) is a surface integral and so needs to be expressed as a volume integral. The standard way to transform a surface integral to a volume integral is to use the divergence theorem. However, the integrand does not have the required form for a direct application of the divergence theorem. This difficulty prompts us to re-express the contact-force density $\mathbf{t}_{\mathrm{n}}$ in a tensorial form.

We first use Cauchy's stress principle, which states that the contact-force density depends continuously on the unit normal n. Then, Cauchy's tetrahedral argument [118] can be used to show that the contact-force density depends linearly on the unit normal, so that

$$
\begin{equation*}
\mathbf{t}_{n}=\mathbf{T n}, \tag{133}
\end{equation*}
$$

where $\mathbf{T}$ is a second-order tensor independent of $\mathbf{n}$. This last identity has the correct form for the application of the divergence theorem (46):

$$
\begin{equation*}
\int_{\partial \Omega} \mathbf{t}_{\mathbf{n}} \mathrm{d} a=\int_{\partial \Omega} \boldsymbol{\operatorname { T n }} \mathrm{d} a=\int_{\Omega} \operatorname{div}\left(\mathbf{T}^{\boldsymbol{\top}}\right) \mathrm{d} v \tag{134}
\end{equation*}
$$

The tensor $\mathbf{T}$ is the Cauchy stress tensor, a central quantity describing forces per unit area in a material. Using this last equality, Euler's law (129) simplifies to

$$
\begin{equation*}
\int_{\Omega} \rho \dot{\mathbf{v}} \mathrm{d} v=\int_{\Omega} \rho \mathbf{b} \mathrm{d} v+\int_{\Omega} \operatorname{div}\left(\mathbf{T}^{\boldsymbol{\top}}\right) \mathrm{d} v \tag{135}
\end{equation*}
$$

and the localization procedure leads to the first Cauchy equation:

$$
\begin{equation*}
\operatorname{div}\left(\mathbf{T}^{\boldsymbol{T}}\right)+\rho \mathbf{b}=\rho \dot{\mathbf{v}} . \tag{136}
\end{equation*}
$$

### 3.3 Balance of angular momentum

In a continuum both forces and torques have to be balanced. The corresponding balance for torque is Euler's second law of motion stating that the rate of change of angular momentum
of an arbitrary material subset $\Omega \subseteq \mathcal{B}$ with respect to a given point is equal to the sum of all torques acting on $\Omega$ with respect to the same point.

The total angular momentum of $\Omega$ is

$$
\begin{equation*}
\int_{\Omega} \mathbf{x} \times(\rho \mathbf{v}) \mathrm{d} v \tag{137}
\end{equation*}
$$

where, without loss of generality, we choose to express the angular momentum with respect to the origin.

If we assume here that the material under consideration is non-polar, that is the body is not subject to extra body or contact torques and cannot support couple stresses, then the total torque due to body and traction forces acting on $\Omega$, with respect to the origin, is

$$
\begin{equation*}
\int_{\Omega} \rho \mathbf{x} \times \mathbf{b} \mathrm{d} v+\int_{\partial \Omega} \mathbf{x} \times \mathbf{t}_{n} \mathrm{~d} a \tag{138}
\end{equation*}
$$

Then, Euler's second law can be written as

$$
\begin{equation*}
\underbrace{\frac{\mathrm{d}}{\mathrm{~d} t} \int_{\Omega} \rho \mathbf{x} \times \mathbf{v} \mathrm{d} v}_{\text {rate of change of angular momentum }}=\underbrace{\int_{\Omega} \rho \mathbf{x} \times \mathbf{b} \mathrm{d} v+\int_{\partial \Omega} \mathbf{x} \times \mathbf{t}_{n} \mathrm{~d} a .}_{\text {torques due to body and traction forces }} \tag{139}
\end{equation*}
$$

The transport procedure and the continuity equation can be used to simplify this expression to

$$
\begin{equation*}
\int_{\Omega} \rho \mathbf{x} \times(\dot{\mathbf{v}}-\mathbf{b}) \mathrm{d} v=\int_{\partial \Omega} \mathbf{x} \times \mathbf{T n} \mathrm{d} a \tag{140}
\end{equation*}
$$

where we have expressed the contact force in terms of the Cauchy stress tensor, $\mathbf{t}_{n}=\mathbf{T n}$. Cauchy's first equation (136) can be used to transform the left hand side of this expression to obtain

$$
\begin{equation*}
\int_{\Omega} \mathbf{x} \times \operatorname{div}\left(\mathbf{T}^{\boldsymbol{\top}}\right) \mathrm{d} v=\int_{\partial \Omega} \mathbf{x} \times \mathbf{T n} \mathrm{d} a . \tag{141}
\end{equation*}
$$

By application of the divergence theorem and the localization procedure, the last integral implies that the Cauchy stress tensor is symmetric, that is

$$
\begin{equation*}
\mathbf{T}^{\top}=\mathbf{T} \tag{142}
\end{equation*}
$$

We can now simplify (136) to obtain the standard form of Cauchy's equation, also known as the equation of motion for a continuum:

$$
\begin{equation*}
\operatorname{div} \mathbf{T}+\rho \mathbf{b}=\rho \dot{\mathbf{v}}, \tag{143}
\end{equation*}
$$

### 3.4 Many stress tensors

The Cauchy stress tensor is the natural measure for contact forces measured in the current configuration per unit area in the current configuration. The contact forces acting on the boundary $\partial \Omega$ of a region $\Omega$ can be extracted from $\mathbf{T}$ by considering different directions with respect to the boundary. Let $\mathbf{n}$ be the normal vector to $\partial \Omega$ at a point $p$ in the body. Then, recalling that $\mathbf{t}_{n}=T \mathbf{n}$, the normal stress, that is, the force per area normal to $\partial \Omega$, applied at $p$ is

$$
\begin{equation*}
\mathbf{n} \cdot \mathbf{t}_{n}=\mathbf{n} \cdot(\mathbf{T n}) . \tag{144}
\end{equation*}
$$

Considering a vector $\mathbf{m}$ tangent to $\partial \Omega$ at $p$ (that is $\mathbf{m} \cdot \mathbf{n}=0$ ), the product

$$
\begin{equation*}
\mathbf{m} \cdot \mathbf{t}_{n}=\mathbf{m} \cdot(\mathbf{T n}) . \tag{145}
\end{equation*}
$$

is a shear stress acting on $\Omega$ at $p$.
While the Cauchy stress is a natural measure for forces acting on a continuum it is not always a convenient quantity for computation since the area in the current configuration changes during the deformation. Therefore, it is often useful to measure contact forces with respect to areas measured initially in the reference configuration. To do so, we apply Nanson's formula $\mathbf{n} \mathrm{d} a=J \mathbf{F}^{-\top} \mathbf{N} \mathrm{d} A$ to the traction vector to obtain the contact-force on a material area element:

$$
\begin{equation*}
\mathbf{t}_{n} \mathrm{~d} a=\mathbf{T n} \mathrm{d} a=\left(J \mathbf{T F}^{-\mathbf{T}}\right) \mathbf{N} \mathrm{d} A=\mathbf{S}^{\boldsymbol{\top}} \mathbf{N} \mathrm{d} A, \tag{146}
\end{equation*}
$$

where

$$
\begin{equation*}
\mathbf{S}=J \mathbf{F}^{-1} \mathbf{T} \tag{147}
\end{equation*}
$$

is the nominal stress tensor. Its transpose, $\mathbf{S}^{\boldsymbol{\top}}$, is the first Piola-Kirchhoff stress tensor. It is also called the engineering stress tensor, as it is a convenient quantity for experimental measurements.

Note that we also have $\mathbf{F S}=J \mathbf{T}=J \mathbf{T}^{\mathrm{T}}=\mathbf{S}^{\mathrm{T}} \mathbf{F}^{\mathrm{T}}$ (since $\mathbf{T}$ is symmetric) and so

$$
\begin{equation*}
\mathbf{S}^{\top} \mathbf{F}^{\top}=\mathbf{F S} \tag{148}
\end{equation*}
$$

### 3.5 Balance of energy for elastic materials

The equations for the stress and mass density derived so far are valid for a large class of continuum bodies independently of their specific material characteristics, including solids and fluids. To close the system of equations, constitutive relationships between stress, deformation gradient, rate of deformation and density must be imposed to characterize the particular body under consideration. The balance of energy provides restrictions on the form of these constitutive relationships. Here, we turn our attention to elastic materials.

The general principle for the balance of energy states that for any part of a body $\Omega \subseteq \mathcal{B}$, the rate of change of the total mechanical energy $\mathcal{E}$ is balanced by the power of the forces $\mathcal{P}$. If we ignore heat dissipation, the total energy for an elastic material is the sum of the kinetic energy and an internal elastic energy. That is, we have

$$
\begin{equation*}
\mathcal{E}=\underbrace{\frac{1}{2} \int_{\Omega} \rho \mathbf{v} \cdot \mathbf{v} \mathrm{d} v}_{\text {kinetic energy }}+\underbrace{\int_{\Omega} J^{-1} W \mathrm{~d} v}_{\text {internal energy }} \tag{149}
\end{equation*}
$$

where $W$ is the internal elastic energy density per unit reference volume.
The power of the forces acting on $\Omega$ is given by

$$
\begin{equation*}
\mathcal{P}=\int_{\Omega} \rho \mathbf{b} \cdot \mathbf{v} \mathrm{d} v+\int_{\partial \Omega} \mathbf{t}_{n} \cdot \mathbf{v} \mathrm{~d} a \tag{150}
\end{equation*}
$$

The balance of energy is then

$$
\begin{equation*}
\frac{\mathrm{D} \mathcal{E}}{\mathrm{D} t}=\mathcal{P} \tag{151}
\end{equation*}
$$

The transport and localization procedure applied to the energy principle together with the equations of continuity and motion, lead to a local form of energy balance [118] for the stress power

$$
\begin{equation*}
\frac{\mathrm{D} W}{\mathrm{D} t}=\operatorname{tr}(\mathbf{S} \dot{\mathbf{F}}) \tag{152}
\end{equation*}
$$

From a thermodynamic point of view, the combination of $\mathbf{S}$ and $\mathbf{F}$ in the stress power $\operatorname{tr}(\mathbf{S} \dot{\mathbf{F}})$, identifies these two tensors as being work conjugate, that is they form a conjugate pair of stress and deformation tensors. We will use this important identity later on when we further restrict the dependence of the internal energy.

## 4 Constitutive equations

■ Overview We close the system of Cauchy equations for stress, density, and velocity by introducing a relationship between stresses and strains, the constitutive equations. Depending on the choice of constitutive equations, the continuum equations can describe a fluid, a solid, or a gas.

So far, we have obtained through conservation of mass and balance of momenta, the following three equations

$$
\begin{align*}
& \dot{\rho}+\rho \operatorname{div} \mathbf{v}=0, \quad \text { mass }  \tag{153}\\
& \operatorname{div} \mathbf{T}+\rho \mathbf{b}=\rho \dot{\mathbf{v}}, \quad \text { linear momentum }  \tag{154}\\
& \mathbf{T}^{T}=\mathbf{T}, \quad \text { angular momentum } \tag{155}
\end{align*}
$$

There are 10 unknowns: 1 in $\rho, 3$ in the vector $\mathbf{v}$ and 6 in the symmetric tensor $\mathbf{T}$. But there are only 4 equations. We need 6 extra relationships to close this system. These will be given by the constitutive equations.

### 4.13 types of assumptions

1) Possible deformations.
e.g. Only rigid motions are allowed $(\mathbf{F}=\mathbf{R}, 3$ parameters $) . ~ \Longrightarrow$ rigid body mechanics. e.g. Only isochoric motion $\Longrightarrow$ Incompressible material.
2) Constraining the stress tensor
e.g. $\mathbf{T}=\mathcal{T}(\mathbf{F})$
e.g. $\mathbf{T}=-p \mathbb{1}$
3) Relate stress to motion
$e . g$. pressure function of density, $\rho$ (for a gas).

### 4.1.1 Particular examples

1) Ideal fluids
(a) $\operatorname{det} \mathbf{F}=1$ (Isochoric)
(b) $\rho=$ const
(c) $\mathbf{T}=-p \mathbb{1}$

Note: the pressure is not determined by the motion (ball under uniform pressure). (It is the Lagrange multiplier associated with the incompressibility constraint.)
2) Elastic fluids
(a) $\mathbf{T}=-p \mathbb{1}$
(b) $p=p(\rho)$

Here $\ddot{\rho}=p^{\prime}\left(\rho_{0}\right) \nabla^{2} \rho$ and $\sqrt{p^{\prime}}$ is the sound speed.
N.B.: both fluids are inviscid (do not exert shearing forces!)

A particular case of an elastic fluid is an ideal gas: $p=\lambda \rho^{\gamma}$, for $\lambda>0, \gamma>1$.
3) Newtonian fluids. Shear stress through friction.

Take $\mathbf{L}=\operatorname{grad} \mathbf{v}$ which gives relative motion of particles, velocity gradient.
(a) $\operatorname{det} \mathbf{F}=1$, incompressible
(b) $\mathbf{T}=-p \mathbb{1}+\mathcal{C}[\mathbf{L}]$ where $\mathcal{C}$ is a linear function of $\mathbf{L}$.

Note $\mathcal{C}[0]=0 \Longrightarrow \mathbf{T}=-p \mathbb{1}$, A Newtonian fluid at rest is ideal
Note $\mathcal{C}[\mathbf{L}]$ has 40 independent constants (once we have removed arbitrariness of $p \mathbb{1}$. However objectivity (independence from observer) implies

$$
\begin{equation*}
\mathcal{C}[\mathbf{L}]=2 \mu \mathbf{D}, \quad \mathbf{D}=\frac{1}{2}\left(\mathbf{L}+\mathbf{L}^{T}\right), \tag{156}
\end{equation*}
$$

which has a single constant, viscosity $\mu$. This implies

$$
\begin{align*}
\rho \dot{\mathbf{v}} & =\operatorname{div} \mathbf{T}+\rho \mathbf{b}  \tag{157}\\
\operatorname{div} \mathbf{v} & =0  \tag{158}\\
\mathbf{T} & =-p \mathbb{1}+2 \mu \mathbf{D} \tag{159}
\end{align*}
$$

After some algebra,

$$
\begin{align*}
\rho \frac{\partial \mathbf{v}}{\partial t}+\rho \mathbf{v} \cdot \operatorname{grad} \mathbf{v} & =\mu \nabla^{2} \mathbf{v}-\operatorname{grad} p+\rho \mathbf{b}  \tag{160}\\
\operatorname{div} \mathbf{v} & =0 \tag{161}
\end{align*}
$$

which are the Navier-Stokes equations. (N.B. $\nu=\mu / \rho$ is the kinematic viscosity.) Stokes flow: 1) steady, 2) neglect acceleration.

$$
\begin{align*}
\mu \nabla^{2} \mathbf{v} & =\operatorname{grad} p-\rho \mathbf{b}  \tag{162}\\
\operatorname{div} \mathbf{v} & =0 \tag{163}
\end{align*}
$$

N.B. for more general fluids, $\mathbf{T}=-p \mathbb{1}+\mathcal{N}(\mathbf{L})$.

### 4.2 Elastic materials

For elastic materials, we have the simple relationship

$$
\begin{equation*}
\mathbf{T}=\mathcal{Z}(\mathbf{F}) \tag{164}
\end{equation*}
$$

This implies that the stress in $\mathcal{B}$ at $\mathbf{x}$ depends on $\mathbf{F}$ and not on the history of the deformation (path-independent). Also, by the definition of the reference configuration (assuming that it is stress free), we have

$$
\begin{equation*}
\mathcal{Z}(\mathbb{1})=0 . \tag{165}
\end{equation*}
$$

This relationship defines a Cauchy, elastic material.

### 4.3 Constitutive equations for hyperelastic materials

We further assume that the material is hyperelastic. That is, the internal energy density $W$ is a function of $\mathbf{F}$ alone. Explicitly, we posit that

$$
\begin{equation*}
W(\mathbf{X}, t)=W(\mathbf{F}(\mathbf{X}, t), \mathbf{X}), \tag{166}
\end{equation*}
$$

in which case, $W$ is referred to as the strain-energy function of the system. Using (71), the time derivative of $W$ is

$$
\begin{equation*}
\frac{\mathrm{D}}{\mathrm{D} t} W(\mathbf{F})=\operatorname{tr}\left(\frac{\partial W}{\partial \mathbf{F}} \dot{\mathbf{F}}\right) \tag{167}
\end{equation*}
$$

so that the energy balance 152 reads now

$$
\begin{equation*}
\operatorname{tr}\left[\left(\frac{\partial W}{\partial \mathbf{F}}-\mathbf{S}\right) \dot{\mathbf{F}}\right]=0 \tag{168}
\end{equation*}
$$

Since this identity must be true for all motions, we conclude that

$$
\begin{equation*}
\mathbf{S}=\frac{\partial W}{\partial \mathbf{F}} \tag{169}
\end{equation*}
$$

where we used the derivative of a scalar $W$ with respect to the second-order tensor $\mathbf{F}$ defined with respect to Cartesian bases in the reference and current configurations, by

$$
\begin{equation*}
\frac{\partial W}{\partial \mathbf{F}}=\frac{\partial W}{\partial F_{j i}} \mathbf{E}_{i} \otimes \mathbf{e}_{j}, \quad\left(\frac{\partial W}{\partial \mathbf{F}}\right)_{i j}=\frac{\partial W}{\partial F_{j i}} \tag{170}
\end{equation*}
$$

Written in terms of the Cauchy stress this identity provides a constitutive relationship relating the Cauchy stress to the deformation gradient:

$$
\begin{equation*}
\mathbf{T}=J^{-1} \mathbf{F} \frac{\partial W}{\partial \mathbf{F}} \tag{171}
\end{equation*}
$$

### 4.4 Internal material constraint

If we consider a material where the possible deformations are constrained during all motions, extra internal material constraints must be satisfied. We consider the case where these constraints take the form $C(\mathbf{F})=0$ where $C(\mathbf{F})$ is a smooth scalar function of the deformation gradient. For instance, in the case of an incompressible material, we assume that all deformations must preserve volume, which implies $\operatorname{det}(\mathbf{F})=1$. In this case, $C(\mathbf{F})=\operatorname{det}(\mathbf{F})-1$.

A simple way to ensure that a constraint holds is to introduce a Lagrangian multiplier $p=p(\mathbf{X}, t)$ and modify accordingly the energy density $W \rightarrow W-p C$ so that Equation (168) reads now

$$
\begin{equation*}
\operatorname{tr}\left[\left(\frac{\partial}{\partial \mathbf{F}}(W-p C)-\mathbf{S}\right) \dot{\mathbf{F}}\right]=0 \tag{172}
\end{equation*}
$$

which leads to

$$
\begin{equation*}
\mathbf{S}=\frac{\partial W}{\partial \mathbf{F}}-p \frac{\partial C}{\partial \mathbf{F}} \tag{173}
\end{equation*}
$$

In terms of the Cauchy stress, we have

$$
\begin{equation*}
\mathbf{T}=J^{-1} \mathbf{F S}=J^{-1} \mathbf{F} \frac{\partial W}{\partial \mathbf{F}}-p \mathbf{N} \tag{174}
\end{equation*}
$$

where

$$
\begin{equation*}
\mathbf{N}=J^{-1} \mathbf{F} \frac{\partial C}{\partial \mathbf{F}} \tag{175}
\end{equation*}
$$

is the reaction stress enforcing the constraint. In particular, for incompressible materials, we have

$$
\begin{equation*}
\frac{\partial C}{\partial \mathbf{F}}=(\operatorname{det} \mathbf{F}) \mathbf{F}^{-1}=J \mathbf{F}^{-1}, \tag{176}
\end{equation*}
$$

that is, $\mathbf{N}=\mathbf{1}$. The constitutive relationship for an incompressible hyperelastic material is then

$$
\begin{equation*}
\mathbf{T}=\mathbf{F} \frac{\partial W}{\partial \mathbf{F}}-p \mathbf{1} \tag{177}
\end{equation*}
$$

Recalling that a hydrostatic pressure is a stress that is multiple of the identity, we can identify the reaction stress in 177) with a hydrostatic pressure. Physically, we see that a pressure $p$ is required to enforce locally the conservation of volume,

For a given $W=W(\mathbf{F})$, the Cauchy stress for compressible or incompressible materials can be written in the general form

$$
\begin{equation*}
\mathbf{T}=J^{-1} \mathbf{F} \frac{\partial W}{\partial \mathbf{F}}-p \mathbf{1} \tag{178}
\end{equation*}
$$

where $J=1$ for an incompressible material and $p=p(\mathbf{x}, t)$ must be determined. If the material is unconstrained, then $p=0$.

## 5 Summary of equations

■ Overview A brief pause to collect all the equations we have seen so far. Counting to make sure that the numbers of unknowns matches the number of equations is always a good idea

We can now collect the different equations from the previous sections to obtain a closed set of equations

$$
\begin{align*}
\dot{\rho}+\rho \operatorname{div} \mathbf{v}=0, & \text { continuity equation }  \tag{179}\\
\operatorname{div} \mathbf{T}+\rho \mathbf{b}=\rho \dot{\mathbf{v}}, & \text { equation of motion }  \tag{180}\\
\mathbf{T}^{\top}=\mathbf{T}, & \text { symmetry of Cauchy stress tensor }  \tag{181}\\
\mathbf{T}=J^{-1} \mathbf{F} \frac{\partial W}{\partial \mathbf{F}}-p \mathbf{1}, & \text { constitutive law } \tag{182}
\end{align*}
$$

Since the elements of $\mathbf{F}$ are related to the motion $\boldsymbol{\chi}$ by $\mathbf{F}=\operatorname{Grad} \boldsymbol{\chi}$, and $\mathbf{v}=\partial_{t} \boldsymbol{\chi}(\mathbf{X}(\mathbf{x}, t), t)$, there are ten unknowns in this system: the scalar field $\rho$, the vector field $\chi$ and the six components of the symmetric tensor $\mathbf{T}$ for ten equations (excluding the third equation, which we already used to reduce the number of unknowns in $\mathbf{T}$ ).

It is also sometimes convenient to write these equations with respect to the reference variables [118:

$$
\begin{align*}
\dot{\rho}_{0}=0, & \text { continuity equation }  \tag{183}\\
\text { Div } \mathbf{S}+\rho_{0} \mathbf{B}=\rho_{0} \dot{\mathbf{v}} & \text { equation of motion }  \tag{184}\\
\mathbf{S}^{\top} \mathbf{F}^{\top}=\mathbf{F S}, & \text { symmetry of Cauchy stress tensor }  \tag{185}\\
\mathbf{S}=\frac{\partial W}{\partial \mathbf{F}}-p \mathbf{J F} \mathbf{F}^{-1}, & \text { constitutive law } \tag{186}
\end{align*}
$$

where the divergence and gradient are now taken in the initial reference configuration, $\rho_{0}=$ $J(\mathbf{X}, t) \rho(\mathbf{x}(\mathbf{X}, t), t)$ is the reference density at a material point, $\mathbf{B}=\mathbf{b}(\mathbf{x}(\mathbf{X}, \mathbf{t}), \mathbf{t})$ is the body force acting at the same point, and $\dot{\mathbf{v}}=\dot{\mathbf{v}}(\mathbf{x}(\mathbf{X}, t), t)$ is the acceleration of a material point.

### 5.1 Boundary conditions

Equilibrium and static solutions are obtained by setting $\mathbf{v}(\mathbf{X}, t)=0$ for all $\mathbf{X} \in \mathcal{B}_{0}$ and for all time $t$. The equilibrium solutions must satisfy the conditions imposed on the boundary. Depending on the setting, many different types of boundary conditions can be applied and it is well appreciated that the solutions will depend crucially on these conditions. The two main types of boundary conditions are dead loading and rigid loading.

In dead loading, a traction is prescribed and maintained constant throughout the deformation, i.e. the prescribed traction is independent of deformation. A typical example of dead loading is hydrostatic loading where a constant pressure $P>0$ is applied at the boundary in the current configuration. In this case, $\mathbf{t}_{\mathrm{n}}=-P \mathbf{n}$, so that $\mathbf{T}=-P \mathbf{1}$.

In rigid loading, fixed displacements are prescribed at the boundary.
In mixed-loading, a surface traction $\mathbf{t}_{\mathrm{b}}$ and deformation $\mathbf{x}_{\mathrm{b}}$ are prescribed at the boundary:

$$
\begin{array}{ll}
\mathbf{T n}=\mathbf{t}_{\mathrm{b}} & \text { for } \mathbf{X} \in \partial \mathcal{B}_{0}^{t} \\
\mathbf{x}(\mathbf{X})=\mathbf{x}_{\mathrm{b}} & \text { for } \mathbf{X} \in \partial \mathcal{B}_{0}^{d} \tag{188}
\end{array}
$$

where $\partial \mathcal{B}_{0}^{\mathrm{t}}$ and $\partial \mathcal{B}_{0}^{\mathrm{d}}$ are parts of the body boundary such that $\partial \mathcal{B}_{0}^{\mathrm{t}} \cup \partial \mathcal{B}_{0}^{\mathrm{d}}=\partial \mathcal{B}_{0}$ and $\partial \mathcal{B}_{0}^{\mathrm{t}} \cap$ $\partial \mathcal{B}_{0}^{\mathrm{d}}=\emptyset$. Note that $\mathbf{t}_{\mathrm{b}}$ can be a function of the deformation gradient as well as of the position.

## 6 Isotropic materials

■ Overview We can make much progress by further restricting our analysis to special claases of materials with given symmetry. The simplest ones are the isotropic materials.

### 6.1 Objectivity and material symmetry

The functional form of the elastic energy can be restricted by combining a fundamental principle, the principle of objectivity, together with symmetry properties of the material.

The principle of objectivity or material-frame indifference [146] states that material properties are independent of superimposed rigid-body motions. For hyperelastic materials, the principle of objectivity implies

$$
\begin{equation*}
W(\mathbf{Q F})=W(\mathbf{F}), \quad \forall \mathbf{Q} \in S O(3), \tag{189}
\end{equation*}
$$

where $S O(3)$ is the set of all proper orthogonal tensors. The principle of objectivity implies that $W$ only depends on $\mathbf{F}$ through $\mathbf{C}$, so that we can write $W(\mathbf{F})=\bar{W}(\mathbf{C})$. Here, to simplify the notation we will drop the overbar and simply write $W(\mathbf{F})=W(\mathbf{C})$.

Next, we consider the implication of material symmetries. A material is said to be symmetric with respect to a linear transformation if the reference configuration is mapped by this transformation to another configuration that is mechanically indistinguishable from it. The set of all such linear transformations constitutes a symmetry group $\mathbb{Q} \subseteq S O(3)$. The symmetry condition for a hyperelastic material is [118]

$$
\begin{equation*}
W(\mathbf{F Q})=W(\mathbf{F}), \quad \forall \mathbf{Q} \in \mathbb{Q} . \tag{190}
\end{equation*}
$$

### 6.2 Symmetry of isotropic materials

The maximal possible symmetry group is $S O(3)$, which defines an isotropic material. The case of isotropic materials is particularly important both for its simplicity and its wide applicability. Isotropy implies that the strain-energy function depends on $\mathbf{F}$ only through $\mathbf{V}$, where $\mathbf{V}$ is the symmetric second-order tensor appearing in the polar decomposition $\mathbf{F}=\mathbf{V R}$. Indeed, choosing $\mathbf{Q}=\mathbf{R}^{\top}$ in leads to

$$
\begin{equation*}
W(\mathbf{F Q})=W\left(\mathbf{F R}^{\top}\right)=W\left(\mathbf{V R} \mathbf{R}^{\top}\right)=W(\mathbf{V}) \tag{191}
\end{equation*}
$$

Combining isotropy with objectivity, we have

$$
\begin{equation*}
W\left(\mathbf{Q F} \tilde{\mathbf{Q}}^{\boldsymbol{\top}}\right)=W\left(\mathbf{F} \tilde{\mathbf{Q}}^{\boldsymbol{\top}}\right)=W(\mathbf{F})=W(\mathbf{V}), \quad \forall \mathbf{Q}, \tilde{\mathbf{Q}} \in S O(3), \tag{192}
\end{equation*}
$$

and choosing $\tilde{\mathbf{Q}}=\mathbf{Q R}$ in $W\left(\mathbf{Q F} \tilde{\mathbf{Q}}^{\mathbf{\top}}\right)$ leads to the conclusion that the strain-energy function satisfies

$$
\begin{equation*}
W(\mathbf{V})=W\left(\mathbf{Q V Q}^{\boldsymbol{\top}}\right), \quad \forall \mathbf{Q} \in S O(3) \tag{193}
\end{equation*}
$$

The property 193) defines $W$ as an isotropic function of $\mathbf{V}$. By inspection, it can readily be observed that the determinant and trace are simple examples of isotropic functions of a second-order tensor. More generally, an isotropic function of $\mathbf{V}$ can only depend on $\mathbf{V}$ through its three principal invariants

$$
\begin{equation*}
\left\{\operatorname{tr}(\mathbf{V}), \frac{1}{2}\left(\operatorname{tr}(\mathbf{V})^{2}-\operatorname{tr}\left(\mathbf{V}^{2}\right)\right), \operatorname{det}(\mathbf{V})\right\} . \tag{194}
\end{equation*}
$$

However, since $\mathbf{V}$ is a symmetric positive-definite tensor, it is often more convenient to express $W$ through the principal invariants of the left Cauchy-Green tensor $\mathbf{B}=\mathbf{V}^{2}=\mathbf{F F}^{\top}$ :

$$
\begin{align*}
I_{1} & =\operatorname{tr}(\mathbf{B})=\lambda_{1}^{2}+\lambda_{2}^{2}+\lambda_{3}^{2},  \tag{195}\\
I_{2} & =\frac{1}{2}\left(I_{1}^{2}-\operatorname{tr}\left(\mathbf{B}^{2}\right)\right)=\lambda_{2}^{2} \lambda_{3}^{2}+\lambda_{3}^{2} \lambda_{1}^{2}+\lambda_{1}^{2} \lambda_{2}^{2},  \tag{196}\\
I_{3} & =\operatorname{det}(\mathbf{B})=\lambda_{1}^{2} \lambda_{2}^{2} \lambda_{3}^{2} . \tag{197}
\end{align*}
$$

Equivalently, (193) implies that $W$ only depends on $\mathbf{F}$ through its principal stretches $\lambda_{1}, \lambda_{2}$, $\lambda_{3}$ (the square roots of the principal values of $\mathbf{B}$ ). With a slight abuse of notation, we write either $W=W\left(I_{1}, I_{2}, I_{3}\right)$, or $W=W\left(\lambda_{1}, \lambda_{2}, \lambda_{3}\right)$.

For an isotropic compressible material, we have $J=1$, which implies that $\lambda_{3}=1 /\left(\lambda_{1} \lambda_{2}\right)$. Therefore, $W$ can be either expressed in terms of $\left\{\lambda_{1}, \lambda_{2}\right\}$ or $\left\{I_{1}, I_{2}\right\}$.

To compute the explicit form of the Cauchy stress tensor for a compressible material in terms of the invariants and their derivatives we use

$$
\begin{equation*}
\frac{\partial I_{1}}{\partial \mathbf{F}}=2 \mathbf{F}^{\mathrm{T}}, \quad \frac{\partial I_{2}}{\partial \mathbf{F}}=2 I_{1} \mathbf{F}^{\mathrm{T}}-2 \mathbf{F}^{\mathrm{T}} \mathbf{B}, \quad \frac{\partial I_{3}}{\partial \mathbf{F}}=2 I_{3} \mathbf{F}^{-1} \tag{198}
\end{equation*}
$$

to find

$$
\begin{equation*}
\mathbf{T}=w_{0} \mathbf{1}+w_{1} \mathbf{B}+w_{2} \mathbf{B}^{2} \tag{199}
\end{equation*}
$$

where the functions $w_{i}$ depend on the invariants and are given explicitly by

$$
\begin{align*}
w_{0} & =2 J \frac{\partial W}{\partial I_{3}}-p,  \tag{200}\\
w_{1} & =2 J^{-1} \frac{\partial W}{\partial I_{1}}+2 J^{-1} \frac{\partial W}{\partial I_{2}} I_{1},  \tag{201}\\
w_{2} & =-2 J^{-1} \frac{\partial W}{\partial I_{2}} . \tag{202}
\end{align*}
$$

As before we choose $p=0$ for compressible materials and $J=I_{3}=1$ for incompressible materials. If the reference configuration is assumed stress-free, then we must have $\mathbf{T}(\mathbf{F}=$ $\mathbf{1})=\mathbf{0}$, that is the functions $w_{i}=w_{i}\left(I_{1}, I_{2}, I_{3}\right)$ satisfy

$$
\begin{equation*}
w_{0}(3,3,1)+w_{1}(3,3,1)+w_{2}(3,3,1)=0 . \tag{203}
\end{equation*}
$$

A convenient alternative representation, the Rivlin-Ericksen representation, is obtained from (199) by using the Cayley-Hamilton theorem [60] for B. In terms of the invariants, the Cayley-Hamilton theorem in three dimensions reads

$$
\begin{equation*}
\mathbf{B}^{3}-I_{1} \mathbf{B}^{2}+I_{2} \mathbf{B}-I_{3} \mathbf{1}=0 \tag{204}
\end{equation*}
$$

Substituting $\mathbf{B}^{2}=I_{1} \mathbf{B}-I_{2} \mathbf{1}+I_{3} \mathbf{B}^{-1}$ in gives

$$
\begin{equation*}
\mathbf{T}=\beta_{0} \mathbf{1}+\beta_{1} \mathbf{B}+\beta_{-1} \mathbf{B}^{-1} \tag{205}
\end{equation*}
$$

where

$$
\begin{align*}
& \beta_{0}=2 J \frac{\partial W}{\partial I_{3}}+2 J^{-1} I_{2} \frac{\partial W}{\partial I_{2}}-p  \tag{206}\\
& \beta_{1}=2 J^{-1} \frac{\partial W}{\partial I_{1}}  \tag{207}\\
& \beta_{-1}=-2 J \frac{\partial W}{\partial I_{2}} . \tag{208}
\end{align*}
$$

### 6.3 Adscititious inequalities

The principle of objectivity together with isotropy leads to a representation of the strainenergy function in terms of three invariants. This formulation still leads to many choices for a suitable functional form of $W$. If we want to establish general results independent of the particular choice of strain-energy function, we can impose certain desired behaviors [151]. For instance, we may require that, in simple extension an isotropic elastic body extends rather than shrinks. These conditions take the form of inequalities either on the coefficients of the constitutive relations, or on the principal stresses and strains. They are called adscititious inequalities as they come from outside the theory and are derived empirically from everyday experience or experiments [147. We mention here three standard inequalities often used in elasticity and suitable for most elastomers.

- Baker-Ericksen inequalities. The Baker-Ericksen inequalities follow from the requirement that the greater principal stress occurs in the direction of the greater principal stretch [9] which implies

$$
\begin{equation*}
\lambda_{i} \neq \lambda_{j} \quad \Rightarrow \quad\left(t_{i}-t_{j}\right)\left(\lambda_{i}-\lambda_{j}\right)>0, \quad i, j=1,2,3, \tag{209}
\end{equation*}
$$

where $\left\{t_{1}, t_{2}, t_{3}\right\}$ and $\left\{\lambda_{1}, \lambda_{2}, \lambda_{3}\right\}$ are the principal stresses and principal stretches obtained by the spectral decomposition

$$
\begin{equation*}
\mathbf{V}=\sum_{i=1}^{3} \lambda_{i} \mathbf{v}_{i} \otimes \mathbf{v}_{i}, \quad \mathbf{T}=\sum_{i=1}^{3} t_{i} \mathbf{v}_{i} \otimes \mathbf{v}_{i} \tag{210}
\end{equation*}
$$

Condition (209) imposes the following restrictions on the coefficients in 205):

$$
\begin{array}{ll}
\lambda_{i}^{2} \lambda_{j}^{2} \beta_{1}>\beta_{-1}, & \text { if } \lambda_{i} \neq \lambda_{j}, \\
\lambda_{i}^{4} \beta_{1} \geqslant \beta_{-1}, & \text { if } \lambda_{i}=\lambda_{j} . \tag{212}
\end{array}
$$

For a hyperelastic body under uniaxial tension, the deformation is a simple extension in the direction of the (positive) tensile force. The ratio of the tensile strain to the strain in the perpendicular direction is greater than one if and only if the Baker-Ericksen inequalities hold [103].

- The ordered-forces inequalities. Similar to the Baker-Ericksen inequalities, the ordered-forces inequalities state that the greater stretch occurs in the direction of the greater force. While similar, the two sets of inequalities do not imply each other [146, p. 157]. However, it can be shown that if two of the three principal stresses are nonnegative, then the Baker-Ericksen inequalities follow from the ordered-forces inequalities, and if two of the three principal stresses are non-positive, then the ordered-forces inequalities are implied by the Baker-Ericksen inequalities.
- Empirical inequalities. Based on experimental observations in elastomers, the following empirical inequalities on the coefficients of (205) have been postulated [115]:

$$
\begin{equation*}
\beta_{0} \leqslant 0, \quad \beta_{1}>0, \quad \beta_{-1} \leqslant 0 \tag{213}
\end{equation*}
$$

for the compressible case. For the incompressible case, only the last two inequalities are considered. These inequalities directly imply the Baker-Ericksen inequalities (211) but not conversely.

### 6.3.1 Example: pure shear of an elastic cube

The adscititious inequalities can be used to establish general qualitative trends. For instance, consider a homogeneous isotropic hyperelastic cube subject to a pure shear stress on its top face as shown in Figure 10. In Cartesian coordinates, this stress can be written as $\mathbf{T}=T\left(\mathbf{e}_{1} \otimes \mathbf{e}_{2}+\mathbf{e}_{2} \otimes \mathbf{e}_{1}\right)$, where $T>0$ is constant. Equivalently, in matrix form, it reads

$$
[T]=\left[\begin{array}{ccc}
0 & T & 0  \tag{214}\\
T & 0 & 0 \\
0 & 0 & 0
\end{array}\right]
$$



Figure 10: A cube deformed under pure shear stress $T$ applied to the top face ( $d=\sqrt{b^{2}-a^{2}}$ ).
Since $T$ is constant, in the absence of any body force, the equation of motion is identically satisfied. The corresponding deformation is homogeneous. That is the deformation gradient is independent of the position. For a pure shear stress, it reads

$$
\begin{equation*}
x=a X+\sqrt{b^{2}-a^{2}} Y, \quad y=b Y, \quad z=c Z \tag{215}
\end{equation*}
$$

It consists of a triaxial stretch, a pure strain deformation, combined with a simple shear in the direction of the shear force if and only if the Baker-Ericksen inequalities hold. Therefore, the Baker-Ericksen inequalities guarantee that the shear strain is in the same direction as the shear force.

If the Baker-Ericksen inequalities are not satisfied, the material would shear in the direction opposite to the direction of the shear stress. This behavior would be unrealistic, even though there is no fundamental principle that would rule it out. It is only through our own experience of everyday materials that we infer its physical impossibility.

For the deformation (215), obtained under pure shear, we define the Poynting effect as $0<$ $b \neq 1$ [115]. Specifically, if a cube is deformed under pure shear, the positive Poynting effect occurs when $b>1$ [13], i.e. the sheared faces spread apart, whereas the negative Poynting effect is obtained when $b<1$, i.e. the sheared faces are drawn together. It can be shown that the validity of the empirical inequalities (with $\beta_{-1}<0$ ) is a necessary and sufficient condition for the positive Poynting effect as found in rubber materials [113]. However, experimental observations suggests that semi-flexible polymer gels exhibit a negative Poynting effect [84], which implies $\beta_{-1}>0$. Therefore, it appears that the last of the empirical inequalities may not hold for some biological materials and should be replaced by the generalized empirical inequalities [114] which simply state $\beta_{0} \leqslant 0$ and $\beta_{1}>0$.

### 6.4 Choice of strain-energy functions

The choice of strain-energy functions $W=W(\mathbf{F})$ for particular applications is a controversial and difficult problem. Methods based on a statistical analysis of the microstructure have been proposed [16, 39]. However, typically, phenomenological models are used to capture the essential features of a material such as its behaviour under shear or its strain-hardening or strain-softening properties [76, 79, 134], while respecting basic material properties such as convexity and objectivity [154]. Note that the words model and material are used interchangeably to describe these particular strain-energy functions. For instance, a neo-Hookean material is a material described by the neo-Hookean model, that is a hyperelastic material with the particular form of strain-energy density function given below. These models can be calibrated and fitted to uniaxial or biaxial experiments [72, 73, 92, 96, 135, 136, 150, 148]. Here, we limit our presentation to a few key popular models for incompressible materials that capture specific features and are widely used in applications. A summary is given in Table 1

- Neo-Hookean materials. The simplest model, and the starting point of many theories, is the neo-Hookean model [40]:

$$
\begin{equation*}
W_{\mathrm{nh}}=\frac{C_{1}}{2}\left(I_{1}-3\right) . \tag{216}
\end{equation*}
$$

This strain-energy function can be derived from statistical mechanics as a macroscopic limit of the energy density of an amorphous cross-linked network of polymeric molecules [38, 39, 143, 144]. Each molecule in this network is a freely jointed chain with the same number of monomer units and their end-to-end distances follow a Gaussian distribution.
For small deformations, the macroscopic parameter $C_{1}$ can be identified with the shear modulus $\mu$ and is proportional to the product $k_{\mathrm{B}} T$ of the Boltzmann constant with the absolute temperature. The Young's modulus is then related to $C_{1}$ by

$$
\begin{equation*}
E=3 \mu=3 C_{1} . \tag{217}
\end{equation*}
$$

A simple generalization of neo-Hookean material is obtained by assuming that the strain-energy function is only a function of the first invariant, $W(\mathbf{F})=W\left(I_{1}\right)$. This class of models are know as generalized neo-Hookean materials [4, 155], for which general results can easily be established [100].

- Mooney-Rivlin materials. The neo-Hookean model can be interpreted as the lowest approximation of a strain-energy function with respect to the strain tensor $\mathbf{E}=$ $\left(\mathbf{F}^{\top} \mathbf{F}-\mathbf{1}\right) / 2$, the so-called second-order elasticity approximation. This model is a good descriptor for many elastomers in tension or compression but it often fails to capture quantitatively behaviors associated with shear or torsion. The next order approximation for incompressible isotropic elasticity gives rise to third-order elasticity [27, 32, 58]. Expressed in terms of invariants, it takes the form of the Mooney-Rivlin strain-energy function

$$
\begin{equation*}
W_{\mathrm{mr}}=\frac{C_{1}}{2}\left(I_{1}-3\right)+\frac{C_{2}}{2}\left(I_{2}-3\right) . \tag{218}
\end{equation*}
$$

The combination $C_{1}+C_{2}=\mu$ can be identified again as the shear modulus. Therefore, we can write

$$
\begin{equation*}
C_{1}=\mu\left(\frac{1}{2}+\alpha\right), \quad C_{2}=\mu\left(\frac{1}{2}-\alpha\right) . \tag{219}
\end{equation*}
$$

The Baker-Ericksen inequalities imply that $\alpha \in[-1 / 2,1 / 2]$. NB: This model can also be derived from statistical-mechanics arguments by relaxing some of the assumptions that lead to the neo-Hookean model [45].

- Ogden materials. A general approach for material modeling, originally proposed by Ogden [117, 119, 121], consists in considering a general expansion with $N$ terms of the form

$$
\begin{equation*}
W_{\mathrm{og} N}=\sum_{i=1}^{N} \frac{\mu_{i}}{\alpha_{i}}\left(\lambda_{1}^{\alpha_{i}}+\lambda_{2}^{\alpha_{i}}+\lambda_{3}^{\alpha_{i}}-3\right) . \tag{220}
\end{equation*}
$$

Each parameter $\mu_{i}$ and $\alpha_{i}$ is a material constant to be determined. These constants are related to the shear modulus $\mu$ of small deformations by

$$
\begin{equation*}
\sum_{i=1}^{N} \mu_{i} \alpha_{i}=2 \mu \tag{221}
\end{equation*}
$$

In practice, the number of terms is limited to $N \leqslant 6$. The possibility of having a large number of parameters provides a systematic way to explore many different behaviors and can be used to fit experimental data of both elastomers and biological tissues [82, 112, 152, 153].

- Fung-Demiray materials. Many soft tissues and elastomers exhibit strong strainhardening properties. That is, in simple extension, it becomes increasingly difficult to further extend the material. Examples of generalized neo-Hookean materials that have been used to capture this effect in soft tissues are the Fung and Gent models. The Fung model 49, 50, 94, 142, in its simplest form, reads

$$
\begin{equation*}
W_{\mathrm{fu}}=\frac{\mu}{2 \beta}\left[\exp \beta\left(I_{1}-3\right)-1\right], \tag{222}
\end{equation*}
$$

where $\beta>0$ controls the strain-hardening property. In the limit $\beta \rightarrow 0$ the Fung model reduces to the standard neo-Hookean model. This particular form of the Fung model was first proposed by Demiray in 1972 [29, 30].

- Gent materials. Another popular model is the Gent model that has finite-chain extensibility enforced by a singular limit of the strain-energy function [53, [77, 79 ]

$$
\begin{equation*}
W_{\mathrm{ge}}=-\frac{\mu}{2 \beta} \log \left[1-\beta\left(I_{1}-3\right)\right] . \tag{223}
\end{equation*}
$$

The neo-Hookean model is obtained in the limit $\beta \rightarrow 2$.
For a compressible material, there is an extra dependance on the invariant $I_{3}=J^{2}$. Again, a choice must be made to take into account the energy associated with local changes of the volume. Typically, an additive choice is made for which the strain-energy function is separated into an incompressible part and a compressible part [74, 101] so that

$$
\begin{equation*}
W=W_{\mathrm{inc}}\left(I_{1}, I_{2}\right)+W_{\text {comp }}\left(I_{3}\right) \tag{224}
\end{equation*}
$$

and a model from Table 1 is adopted for $W_{\text {inc }}\left(I_{1}, I_{2}\right)$. Possible choices for $W_{\text {comp }}\left(I_{3}\right)$ include: $\mu_{\mathrm{c}}\left(I_{3}-1\right), \mu_{\mathrm{c}}(J-1)^{2}, \mu_{\mathrm{c}} \ln I_{3}, \mu_{\mathrm{c}} \ln J$, where $\mu_{\mathrm{c}}$ is a material parameter related to the bulk modulus.

| Name | Definition | soft tissues | elastomers |
| :--- | :--- | :---: | :---: |
| neo-Hookean | $W_{\mathrm{nh}}=\frac{C_{1}}{2}\left(I_{1}-3\right)$ |  |  |
| Mooney-Rivlin | $W_{\mathrm{mr}}=\frac{C_{1}}{2}\left(I_{1}-3\right)+\frac{C_{2}}{2}\left(I_{2}-3\right)$ |  |  |
| Ogden 1 | $W_{\mathrm{og} 1}=\frac{2 \mu}{\beta^{2}}\left(\lambda_{1}^{\beta}+\lambda_{2}^{\beta}+\lambda_{3}^{\beta}-3\right)$ | $\beta \geq 9$ | $\beta \approx 3$ |
| Fung | $W_{\mathrm{fu}}=\frac{\mu}{2 \beta}\left[\exp \beta\left(I_{1}-3\right)-1\right]$ | $3<\beta<20$ |  |
| Gent | $W_{\mathrm{ge}}=-\frac{\mu}{2 \beta} \log \left[1-\beta\left(I_{1}-3\right)\right]$ | $0.4<\beta<3$ | $0.005<\beta<0.05$ |

Table 1: A list of phenomenological strain-energy functions for isotropic incompressible materials. Note that the materials have been written so that they share the same infinitesimal shear modulus $\mu$. The limits $\beta \rightarrow 2$ in $W_{\mathrm{og} 1}$ and, $\beta \rightarrow 0$ in $W_{\mathrm{fu}}$ and $W_{\mathrm{ge}}$ all lead to the neo-Hookean strain-energy function. Estimates are taken from: 1-term Ogden is [15, 138], Gent [53, 55, 76, 78, Fung [28, 71].

## 7 Examples of boundary value problems

- Overview For a given strain-energy density function, we can write a full system of equations which can be solved for given boundary conditions. We (finally!) give some simple solutions for homogeneous and semi-inverse problems.


### 7.1 A simple homogeneous deformation

Homogeneous deformations are specified by a constant deformation gradient so that

$$
\begin{equation*}
\mathbf{x}=\mathbf{F} \mathbf{X}+\mathbf{c} \tag{225}
\end{equation*}
$$

where $\mathbf{F}$ and $\mathbf{c}$ are constant.
For a homogenous isotropic compressible material, this choice implies that $\mathbf{T}$ is constant, and in the absence of a body load, the equilibrium equations are therefore trivially satisfied. The solution is then fully specified by the boundary conditions and the constitutive law [133].

Consider for example, the diagonal deformation of a cuboid into another cuboid shown in Figure 11 and described by

$$
\begin{equation*}
x_{i}=\lambda_{i} X_{i}, \quad i=1,2,3(\text { no summation over } i) \tag{226}
\end{equation*}
$$

The corresponding deformation gradient is $[\mathbf{F}]=\operatorname{diag}\left(\lambda_{1}, \lambda_{2}, \lambda_{3}\right)$ and, consequently, the


Figure 11: A simple diagonal homogenous deformation transforming a cuboid into another cuboid. The deformation is characterized by the three constants $\lambda_{i}=h_{i} / H_{i}, i=1,2,3$.

Cauchy stress tensor is also diagonal: $[\mathbf{T}]=\operatorname{diag}\left(t_{1}, t_{2}, t_{3}\right)$. The deformation and stresses are then obtained from the constitutive law

$$
\begin{equation*}
t_{i}=\frac{\lambda_{i}}{J} \frac{\partial W}{\partial \lambda_{i}}, \quad i=1,2,3(\text { no summation over } i) \tag{227}
\end{equation*}
$$

For instance, in a hydrostatic uniaxial extension, the stress is prescribed in one direction, that is $t_{3}=N$ and $t_{1}=t_{2}=0$. By symmetry, we have $\lambda_{1}=\lambda_{2}$ and

$$
\begin{equation*}
t_{2}=\frac{1}{\lambda_{2} \lambda_{3}} W_{2}=0, \quad t_{3}=\frac{1}{\lambda_{2}^{2}} W_{3}=N . \tag{228}
\end{equation*}
$$

These equations constitute a systems of two equations for two unknowns.

We further specialize these equations to a compressible neo-Hookean material with a strain-energy function of the form

$$
\begin{equation*}
W=\frac{\mu_{1}}{2}\left(I_{1}-3\right)-\frac{\mu_{1}}{2}\left(I_{3}-1\right)+\frac{\mu_{2}}{4}\left(I_{3}-1\right)^{2} \tag{229}
\end{equation*}
$$

This particular form is chosen so that all stresses vanish at $\lambda_{1}=\lambda_{2}=\lambda_{3}=1$. Equations 228) then read

$$
\begin{align*}
& 0=\mu_{1}\left(\frac{1}{\lambda_{3}}-\lambda_{2}^{2} \lambda_{3}\right)+\mu_{2} \lambda_{2}^{2} \lambda_{3}\left(\lambda_{2}^{4} \lambda_{3}^{2}-1\right)  \tag{230}\\
& N=\mu_{1}\left(\frac{\lambda_{3}}{\lambda_{2}^{2}}-\lambda_{2}^{2} \lambda_{3}\right)+\mu_{2} \lambda_{2}^{2} \lambda_{3}\left(\lambda_{2}^{4} \lambda_{3}^{2}-1\right) \tag{231}
\end{align*}
$$

The Young's modulus $E$ is obtained for small deformations as the ratio of uniaxial stress to the uniaxial stretch, that is

$$
\begin{align*}
E & =\left.\frac{\partial N\left(\lambda_{2}, \lambda_{3}\right)}{\partial \lambda_{3}}\right|_{\lambda_{2}=\lambda_{3}=1}+\left.\left(\frac{\partial N\left(\lambda_{2}, \lambda_{3}\right)}{\partial \lambda_{2}} \frac{\partial \lambda_{2}}{\partial \lambda_{3}}\right)\right|_{\lambda_{2}=\lambda_{3}=1} \\
& =2 \mu_{1} \frac{2 \mu_{1}-3 \mu_{2}}{\mu_{1}-2 \mu_{2}} \tag{232}
\end{align*}
$$

If we now consider the same deformation but for an incompressible material with a neoHookean strain-energy function $W=\mu\left(I_{1}-3\right) / 2$, we have $\lambda_{1}=\lambda_{2}$ again by symmetry, but $\lambda_{3} \lambda_{2}^{2}=1$ by incompressibility. We replace the constitutive law 227) by

$$
\begin{equation*}
t_{i}=\lambda_{i} \frac{\partial W}{\partial \lambda_{i}}-p \quad i=1,2,3 \text { (no summation over } i \text { ) } \tag{233}
\end{equation*}
$$

The boundary conditions lead to

$$
\begin{equation*}
p=\frac{\mu}{\lambda_{3}}, \quad N\left(\lambda_{3}\right)=\frac{\left(\lambda_{3}^{3}-1\right) \mu}{\lambda_{3}} \tag{234}
\end{equation*}
$$

which defines a Young's modulus

$$
\begin{equation*}
E=\left.\frac{\partial N\left(\lambda_{3}\right)}{\partial \lambda_{3}}\right|_{\lambda_{3}=1}=3 \mu \tag{235}
\end{equation*}
$$

### 7.2 The half-plane in compression

As a second example, we consider another type of homogeneous deformation applied to an incompressible hyperelastic half-space with a free surface, characterized by $W=W\left(\lambda_{1}, \lambda_{2}, \lambda_{3}\right)$, under pure homogeneous static deformation with principal stretch ratios $\lambda_{1}, \lambda_{2}, \lambda_{3}$ [14, 59]. We take $\mathbf{e}_{2}=\mathbf{E}_{2}$ normal to the surface with the half-space located in $X_{2}>0$, so that $\lambda_{2}$ is the stretch ratio in the direction normal to the free surface. We consider homogeneous loadings so that the Cauchy stress tensor, in Cartesian coordinates, can be written $[\mathbf{T}]=\operatorname{diag}\left(t_{1}, t_{2}, t_{3}\right)$ with deformation gradient $[\mathbf{F}]=\operatorname{diag}\left(\lambda_{1}, \lambda_{2}, \lambda_{3}\right)$.

There are three typical types of loading that are of interest as shown in Figure 12 ,

- Equibiaxial strain. An equibiaxial strain is associated with deformations with equal strains in the plane, that is $\lambda_{1}=\lambda_{3}$. In this case, the half-space is compressed with equal force in the 1 - and 3-directions, and expands freely in the 2 -direction, so that

$$
\begin{equation*}
t_{1}=\lambda_{1} W_{1}-\lambda_{2} W_{2}, \quad t_{2}=0, \quad t_{3}=t_{1} \tag{236}
\end{equation*}
$$

where $W_{i}=\partial_{\lambda_{i}} W$.


Figure 12: Three typical deformations of a half space. A. Equibiaxial strain. B. Plane strain. C. Uniaxial strain

- Plane strain. Plane strain corresponds to the condition $\lambda_{3}=1$. It corresponds to a half-space compressed in the 1-direction and prevented from expanding/contracting in the 3 -direction. Thus, it expands in the 2-direction, normal to the free surface. This deformation is maintained by applying the tractions

$$
\begin{equation*}
t_{1}=\lambda_{1} W_{1}-\lambda_{2} W_{2}, \quad t_{2}=0, \quad t_{3}=\lambda_{3} W_{3}-\lambda_{2} W_{2} \neq t_{1} . \tag{237}
\end{equation*}
$$

- Uniaxial strain. A uniaxial strain is defined by $t_{3}=0$. That is, the half-space is free to expand in the 2 - and 3 -directions, and

$$
\begin{equation*}
t_{1}=\lambda_{1} W_{1}-\lambda_{2} W_{2}, \quad t_{2}=0, \quad t_{3}=0 \tag{238}
\end{equation*}
$$

It follows from the incompressibility condition that $\lambda_{1} \lambda_{2} \lambda_{3}=1$ and therefore the three cases can be written in general as

$$
\lambda_{2}=\lambda_{1}^{n} \quad \text { with } \quad \begin{cases}n=-2 & \text { equibiaxial, }  \tag{239}\\ n=-1 & \text { plane strain }, \\ n=-\frac{1}{2} & \text { uniaxial }\end{cases}
$$

Therefore, we can use $\lambda_{1}$ to fully characterize the deformation. For a given strain-energy function, the stresses developed as a function of $\lambda_{1}$ can be computed by direct evaluation of the relations 236 237).

Once the stresses are known, a natural problem is to look for possible bifurcations. That is, we wish to identify a critical value of $\lambda_{1}$ such that the half-space develops surface wrinkles as one would expect when compressing a large rubber block. We will not consider this problem here but it is an active area of research.

### 7.3 Inflation of a spherical shell.

1) Elastic, incompressible, isotropic spherical shell with strain-energy $W\left(I_{1}, I_{2}, I_{3}\right)$.
2) Symmetric inflation

$$
\begin{array}{lc}
A \leqslant R \leqslant R, & \mathbf{F}=\frac{\partial \mathbf{x}}{\partial \mathbf{X}}(\text { see } 82.9) \\
\mathbf{x}=f(R) \mathbf{X}, & r=f(R) R . \tag{241}
\end{array}
$$



$$
\begin{align*}
\mathbf{F}= & {\left[\begin{array}{lll}
\lambda_{r} & & \\
& \lambda_{\theta} & \\
& & \lambda_{\phi}
\end{array}\right]=\left[\begin{array}{lll}
r^{\prime} & & \\
& r / R & \\
& & r / R
\end{array}\right] }  \tag{242}\\
& \lambda_{r}=r^{\prime}(R), \quad \lambda_{\theta}=r / R=\lambda_{\phi}  \tag{243}\\
& \lambda_{a}=a / A, \quad \lambda_{b}=b / B, r=\sqrt[3]{a^{3}-A^{3}+R^{3}} \tag{244}
\end{align*}
$$

where $a$ is the single unknown parameter. Therefore

$$
\begin{equation*}
\lambda_{\theta}=\lambda_{\phi}=\lambda=r / R, \quad \lambda_{r}=\lambda^{-2} \tag{245}
\end{equation*}
$$



$$
\mathbf{T} \cdot \mathbf{n}= \begin{cases}-P & \text { on } r=a  \tag{246}\\ 0 & \text { on } r=b\end{cases}
$$

$\mathbf{S}^{T} \cdot \mathbf{N}=J P \mathbf{F}^{-T} \mathbf{N}$ (mapping of traction vector)

$$
\begin{align*}
& \begin{cases}\mathbf{T n}=-P \mathbf{n} & \text { on } \partial \mathcal{B} \\
\mathbf{S}^{T} \cdot \mathbf{N}=-P J \mathbf{F}^{-T} \mathbf{N}, & \text { on } \partial \mathcal{B}\end{cases}  \tag{247}\\
& \quad \Longrightarrow T_{r r}= \begin{cases}-P & \text { on } r=a \\
0 & \text { on } r=b\end{cases} \tag{248}
\end{align*}
$$

or

$$
S_{r r}= \begin{cases}-P \lambda_{r}^{-1}=-P \lambda^{2} & \text { on } R=A  \tag{249}\\ 0 & \text { on } R=B\end{cases}
$$

Note that the boundary condition depends on the deformation.
3) $\mathbf{b}=0$ and $\operatorname{div} \mathbf{T}=0$,

$$
\begin{equation*}
\Longrightarrow \frac{\mathrm{d} T_{r r}}{\mathrm{~d} r}+\frac{2}{r}\left(T_{r r}-T_{\theta \theta}\right)=0, \tag{250}
\end{equation*}
$$

or

$$
\begin{equation*}
\frac{\mathrm{d} S_{r r}}{\mathrm{~d} R}+\frac{2}{R}\left(S_{r r}-S_{\theta \theta}\right)=0 . \tag{251}
\end{equation*}
$$

Constitutive equations,

$$
\begin{equation*}
\mathbf{S}=\frac{\partial W}{\partial \mathbf{F}}-p \mathbf{F}^{-1} \tag{252}
\end{equation*}
$$

or

$$
\begin{equation*}
\mathbf{T}=\mathbf{F} \frac{\partial W}{\partial \mathbf{F}}-p \mathbb{1} \tag{253}
\end{equation*}
$$

Then

$$
\begin{equation*}
S_{r r}=\frac{\partial W}{\partial \lambda_{r}}-p \lambda_{r}^{-1}, \quad S_{\theta \theta}=\frac{\partial W}{\partial \lambda_{\theta}}-p \lambda_{\theta}^{-1} \tag{254}
\end{equation*}
$$

which are functions of $\lambda(R)$.
4) Solve the equation $\operatorname{div} \mathbf{S}=0$. To do so, we choose $\lambda$ as a variable. Define $h(\lambda)=$ $W\left(\lambda^{-2}, \lambda, \lambda\right)$, then

$$
\begin{gathered}
\frac{\mathrm{d} S_{r r}}{\mathrm{~d} \lambda}=-2 \frac{S_{r r}-S_{\theta \theta}}{\lambda-\lambda^{-2}}=-\frac{h^{\prime}(\lambda)}{\lambda^{3}-1} \\
\quad \Longrightarrow P=\int_{\lambda_{b}}^{\lambda_{a}} \frac{h^{\prime}(\lambda)}{\lambda^{3}-1} \mathrm{~d} \lambda
\end{gathered}
$$

$$
\begin{equation*}
\frac{\partial t_{r}}{\partial r}+\frac{2}{r}\left(t_{r}-t_{\theta}\right)=0 \tag{255}
\end{equation*}
$$

$$
\begin{equation*}
t_{r}=\lambda_{r} W_{r}-p=\lambda^{-2} W_{r}-p, \quad t_{\theta}=\lambda W_{\theta}-p, \quad t_{\phi}=t_{\theta} \tag{256}
\end{equation*}
$$

$$
\begin{equation*}
t_{r}-t_{\theta}=\lambda^{-2} W_{r}-\lambda W_{\theta} \tag{257}
\end{equation*}
$$

$$
\begin{equation*}
\Longrightarrow \frac{\partial t_{r}}{\partial r}+\frac{2}{r}\left(\lambda^{-2} W_{r}-\lambda W_{\theta}\right)=0 \tag{258}
\end{equation*}
$$

Introduce auxiliary function, $h(\lambda)=W\left(\lambda^{-2}, \lambda, \lambda\right)$,

$$
\begin{gather*}
h^{\prime}(\lambda)=\frac{\partial h}{\partial \lambda}=W_{r} \cdot\left(-2 \lambda^{-3}\right)+W_{\theta} \cdot 1+W_{\phi} \cdot 1=-2 \lambda^{-1}\left(\lambda^{-2} W_{r}-\lambda W_{\theta}\right)  \tag{259}\\
\frac{\partial t_{r}}{\partial r}=\frac{\partial t_{r}}{\partial \lambda} \frac{\partial \lambda}{\partial r} \tag{260}
\end{gather*}
$$



$$
\begin{gather*}
\lambda=\frac{r}{R(r)}, \quad \frac{\partial \lambda}{\partial r}=\frac{1}{R}-\frac{r R^{\prime}}{R^{2}} \\
R^{3}=r^{3}-a^{3}+A^{3}, \quad R^{\prime} R^{2}=3 r^{3}, \quad R^{\prime}=\frac{r^{2}}{R^{2}}=\lambda^{2} . \\
\frac{\partial \lambda}{\partial r}=\frac{1}{R}\left(1-\lambda^{3}\right)  \tag{261}\\
\Longrightarrow \frac{\partial t_{r}}{\partial r}=\frac{\partial t_{r}}{\partial \lambda} \frac{1}{R}\left(1-\lambda^{3}\right)=\frac{\lambda h^{\prime}(\lambda)}{r} .  \tag{262}\\
\frac{\partial t_{r}}{\partial \lambda}=\frac{h^{\prime}(\lambda)}{1-\lambda^{3}}, \quad \Longrightarrow t_{r}=\int_{\lambda_{a}}^{\lambda} \frac{h^{\prime}(\lambda)}{1-\lambda^{3}} \mathrm{~d} \lambda \tag{263}
\end{gather*}
$$

At $\lambda=\lambda_{b}, t_{r}=-P$,

$$
\begin{equation*}
-P=-\int_{\lambda_{a}}^{\lambda_{b}} \frac{h^{\prime}(\lambda)}{1-\lambda^{3}} \mathrm{~d} \lambda, \quad \Longrightarrow \quad P=\int_{\lambda_{a}}^{\lambda_{b}} \frac{h^{\prime}(\lambda)}{1-\lambda^{3}} \mathrm{~d} \lambda=f\left(\lambda_{a}\right) \tag{264}
\end{equation*}
$$

Note

$$
\begin{equation*}
\lambda_{a}=a / A, \quad \lambda_{b}=\frac{1}{B} \sqrt[3]{a^{3}-A^{3}+B^{3}}=\frac{1}{B} \sqrt[3]{\left(\lambda_{a}-1\right) A^{3}+B^{3}} \tag{265}
\end{equation*}
$$

For a given $P$, we find $a$, hence the deformation and the value of $t_{r}$ at all points.
Note that $W=\frac{\mu}{2}\left(\lambda_{r}^{2}+\lambda_{\theta}^{2}+\lambda_{\phi}^{2}\right)$,

$$
\begin{equation*}
\Longrightarrow h=\frac{\mu}{2}\left(\frac{1}{\lambda^{4}}+2 \lambda^{2}\right) . \tag{266}
\end{equation*}
$$

Note the nonlinearity in the $1 / \lambda^{4}$ term.

$$
\begin{gather*}
\Longrightarrow \frac{h^{\prime}}{1-\lambda^{3}}=-2 \mu\left(\lambda^{-2}+\lambda^{-5}\right),  \tag{267}\\
P=-\left.2 \mu\left(\frac{1}{\lambda}+\frac{1}{4 \lambda^{4}}\right)\right|_{\lambda_{a}} ^{\lambda_{b}\left(\lambda_{a}\right)} . \tag{268}
\end{gather*}
$$

### 7.4 The inflation-extension of a tube

As an example of non-homogeneous static deformations, we consider the problem of an incompressible hyperelastic cylindrical shell subject to combined extension and inflation [34, 80, 88] in the absence of body loads. We consider a simple thought experiment in which the tube is capped at both ends and subject to an axial extension $\zeta$ due to an internal pressure $P$ and to a total axial load $N$ on the top cap. The tube of initial inner radius $A$ and outer radius $B>A$, and height $H$ is then deformed into a tube with radii $a, b$ and height $h$ as shown in Figure 13 , We consider a finite deformation in which the cylinder is allowed to inflate and extend while remaining cylindrical at all times regardless of possible stability issues [12, [21, 57, 65, 64].


Figure 13: Inflation-extension of a tube. The tube is inflated with an internal pressure $P$ (which is equivalent to an external pressure $-P$ as shown) and an axial load $N$ resulting from an applied load and the pressure acting on the end caps.

For this problem, the deformation $\mathbf{x}=\boldsymbol{\chi}(\mathbf{X}, t)$, in cylindrical coordinates $\{r, \theta, z\}$ and $\{R, \Theta, Z\}$ reads

$$
\begin{equation*}
r=r(R), \quad \theta=\Theta, \quad z=\zeta Z \tag{269}
\end{equation*}
$$

where $\zeta$ is the constant axial stretch of the cylinder such that $h=\zeta H$. The position vectors in the reference and current configurations are

$$
\begin{equation*}
\mathbf{X}=R \mathbf{E}_{R}+Z \mathbf{E}_{Z}, \quad \mathbf{x}=r(R) \mathbf{e}_{r}+\zeta Z \mathbf{e}_{z} . \tag{270}
\end{equation*}
$$

where $\left\{\mathbf{E}_{R}, \mathbf{E}_{\Theta}, \mathbf{E}_{Z}\right\}$ and $\left\{\mathbf{e}_{r}, \mathbf{e}_{\theta}, \mathbf{e}_{z}\right\}$ are the two standard cylindrical bases. Following the identity $(\sqrt{76})$, the deformation gradient $\mathbf{F}=\operatorname{Grad}(\boldsymbol{\chi})$ with respect these coordinates is given by

$$
\begin{equation*}
\mathbf{F}=r^{\prime} \mathbf{e}_{r} \otimes \mathbf{E}_{R}+\frac{r}{R} \mathbf{e}_{\theta} \otimes \mathbf{E}_{\theta}+\zeta \mathbf{e}_{z} \otimes \mathbf{E}_{Z} \tag{271}
\end{equation*}
$$

where the prime denotes differentiation with respect to $R$. Equivalently, we can write

$$
\begin{equation*}
[\mathbf{F}]=\operatorname{diag}\left(r^{\prime}, \frac{r}{R}, \zeta\right) \equiv \operatorname{diag}\left(\lambda_{r}, \lambda_{\theta}, \lambda_{z}\right) \tag{272}
\end{equation*}
$$

which defines the three principal stretches $\left\{\lambda_{r}, \lambda_{\theta}, \lambda_{z}\right\}$.
The incompressibility condition $\operatorname{det}(\mathbf{F})=1=\lambda_{r} \lambda_{\theta} \lambda_{z}$ leads to

$$
\begin{equation*}
r^{\prime} r=\frac{R}{\zeta}, \tag{273}
\end{equation*}
$$

which, together with $r(A)=a$, leads to

$$
\begin{equation*}
r=\sqrt{a^{2}+\frac{R^{2}-A^{2}}{\zeta}} \tag{274}
\end{equation*}
$$

Then, $\lambda=\lambda_{\theta}$ is given by

$$
\begin{equation*}
\lambda=\frac{r}{R}=\frac{1}{R} \sqrt{a^{2}+\frac{R^{2}-A^{2}}{\zeta}} . \tag{275}
\end{equation*}
$$

Therefore, the deformation is fully specified by two parameters: the axial stretch $\zeta$ and the radial stretch of the inner wall $\lambda_{a}=a / A$ so that

$$
\begin{equation*}
\lambda_{b}=\frac{b}{B}=\frac{1}{\zeta} \sqrt{1+\frac{A^{2}}{B^{2}}\left(\zeta \lambda_{a}^{2}-1\right)} . \tag{276}
\end{equation*}
$$

Since the deformation is diagonal in cylindrical coordinates and only depends on $R$, it follows from Equation (199) that the Cauchy stress tensor is also diagonal in these coordinates so that

$$
\begin{equation*}
[\mathbf{T}]=\operatorname{diag}\left(t_{r}, t_{\theta}, t_{z}\right) \Leftrightarrow \mathbf{T}=t_{r} \mathbf{e}_{r} \otimes \mathbf{e}_{r}+t_{\theta} \mathbf{e}_{\theta} \otimes \mathbf{e}_{\theta}+t_{z} \mathbf{e}_{z} \otimes \mathbf{e}_{z} \tag{277}
\end{equation*}
$$

This particular form of the Cauchy stress tensor implies that the Cauchy equation $\operatorname{div} \mathbf{T}=0$ in cylindrical coordinates reduces to a single scalar equation

$$
\begin{equation*}
\frac{\mathrm{d} t_{r}}{\mathrm{~d} r}+\frac{1}{r}\left(t_{r}-t_{\theta}\right)=0 . \tag{278}
\end{equation*}
$$

This equation can be integrated once over $r$ :

$$
\begin{equation*}
t_{r}(r)=t_{r}(a)+\int_{a}^{r} \frac{t_{\theta}-t_{r}}{r} \mathrm{~d} r, \quad r \in[a, b] . \tag{279}
\end{equation*}
$$

We now examine the boundary conditions. First, due to inflation, the jump in pressure between the inner and outer sides of the cylinder is $P=t_{r}(b)-t_{r}(a)$. Without loss of generality, we choose

$$
\begin{equation*}
t_{r}(a)=-P, \quad t_{r}(b)=0, \tag{280}
\end{equation*}
$$

which in 279) implies

$$
\begin{equation*}
P=\int_{a}^{b} \frac{t_{\theta}-t_{r}}{r} \mathrm{~d} r . \tag{281}
\end{equation*}
$$

Second, the boundary conditions on the two caps of the tube, defined as the two rings at $z=0$ and $z=h$, can be written

$$
\begin{equation*}
t_{z}(z=0)=N_{z}, \quad t_{z}(z=h)=N_{z} . \tag{282}
\end{equation*}
$$

However, since a constant axial stretch $\zeta$ cannot be used to fit a constant $N_{z}$, we replace this point-wise condition on the caps of the cylinder by an integral condition for the total axial load applied on the cap [129, 130]

$$
\begin{equation*}
2 \pi \int_{a}^{b} N_{z} r d r=N \equiv F+\chi P \pi a^{2} \tag{283}
\end{equation*}
$$

thereby eliminating the explicit dependence on the variable $r$. The total axial load $N$ is further decomposed into an external applied load $F$, that corresponds to pulling or compressing the
tube, and the load created by the internal pressure acting over the cap. That load is simply the pressure times the projected area of the cap. The coefficient $\chi$ is 1 for a capped cylinder, and 0 for an infinite cylinder [23, 57].

For incompressible materials, this last expression is not the most practical one as the term $T_{z z}$ will contain an arbitrary pressure. An equivalent expression can be obtained by adding and subtracting $T_{r r}$ to obtain

$$
\begin{equation*}
2 \pi \int_{a}^{b} T_{z z} r \mathrm{~d} r=2 \pi \int_{a}^{b}\left(T_{z z}-T_{r r}+T_{r r}\right) r \mathrm{~d} r \tag{284}
\end{equation*}
$$

The last term can be integrated by parts, and use of the balance law 250 gives

$$
\begin{equation*}
2 \pi \int_{a}^{b} T_{z z} r \mathrm{~d} r=\pi \int_{a}^{b}\left(2 T_{z z}-T_{r r}-T_{\theta \theta}\right) r \mathrm{~d} r+P \pi a^{2} \tag{285}
\end{equation*}
$$

which implies

$$
\begin{equation*}
\pi \int_{a}^{b}\left(2 T_{z z}-T_{r r}-T_{\theta \theta}\right) r \mathrm{~d} r=F+(\chi-1) P \pi a^{2} \tag{286}
\end{equation*}
$$

and the last term vanishes for a capped cylinder.
To close the system, we use the constitutive law:

$$
\begin{equation*}
t_{r}=\lambda_{r} \frac{\partial W}{\partial \lambda_{r}}-p, \quad t_{\theta}=\lambda_{\theta} \frac{\partial W}{\partial \lambda_{\theta}}-p, \quad t_{z}=\lambda_{z} \frac{\partial W}{\partial \lambda_{z}}-p \tag{287}
\end{equation*}
$$

and substitute the functions of $\left(\lambda_{r}=1 /(\lambda \zeta), \lambda_{\theta}=\lambda, \lambda_{z}=\zeta\right)$ in 281,283 so that $t_{\theta}-t_{r}=$ $Q\left(r, \lambda_{a}, \zeta\right)$.

The semi-inverse problem consists then in finding the values of $\left(\lambda_{a}, \zeta\right)$ corresponding to the two external loads $(F, P)$ through the analysis of the two equations 281,283$)$. Note that once $\left(\lambda_{a}, \zeta\right)$ is known, the stress $t_{r}(r)$ can be computed as

$$
\begin{equation*}
t_{r}(r)=-P+\int_{a}^{r} Q\left(r, \lambda_{a}, \zeta\right) \mathrm{d} r \tag{288}
\end{equation*}
$$

and the remaining stresses are obtained from 287).

### 7.4.1 A toy model for an artery

As an example, we consider a toy model for an artery subject to pressure and tensile stretch. The artery is modeled as a capped tube $(\chi=1)$ made of a Fung material with values taken from Table 1. The system is subjected to an fixed axial force $F$ and varying pressure $P$ [149]. We solve Equations (281)-283) for $\left(\lambda_{a}, \zeta\right)$ and plot $P$ as a function of $\zeta$, so that if the pressure is controlled, one can determine the amount of axial stretch in the tube.

First, we consider the case of a neo-Hookean material. The curve $P(\zeta)$ shown in Figure 14 is non-monotonic and presents a maximal value of pressure after which unbounded extensional growth follows. This behavior is a drawback of the neo-Hookean model which is not well defined for arbitrarily large deformations and stresses.

Second, we consider the effect of the strain-stiffening parameter $\beta$. In Figure 15, we see that for small values of $\beta$, a non-monotonic behavior is observed in moderate deformations, followed by a rapidly increasing pressure for larger deformations. For larger values of the strain-stiffening parameter, the behavior is monotonic and increasingly large pressures are needed for further small incremental extensions.


Figure 14: Behavior of a tube under pressure and axial force for a Neo-Hookean material ( $A=1, B=1.2, \mu=1, F=0.1, \chi=1$ ). The neo-Hookean model is ill-defined past a critical pressure $P_{1}$.


Figure 15: Behavior of a tube under pressure and axial force for a Fung material $(\beta>0)$. Parameters for all figures: $A=1, B=1.2, \mu=1, F=0.1, \chi=1$.

We conclude that the behavior of the neo-Hookean model is qualitatively different from the behavior of the Fung model even for very small values of the strain-stiffening parameter $\beta$. In particular, typical axial strains in arteries are around 1.3 to 1.6 , in the region where the response of the structure clearly depends on the choice of the material model. This simple computation clearly demonstrates the importance of the choice of the material model for a given problem and the need to use nonlinear rather than linear elasticity to study these problems.


Figure 16: Limit-point instability in of a tube under pressure and axial force for a Fung material $(\beta=0.05)$. The curve $P(\zeta)$ has a minimum and a maximum. If the internal pressure of the tube is raised to $P_{1}$, a sudden extension occurs through a jump from $\zeta_{1}$ to $\zeta_{2}$. When the pressure is then decreased to $P_{2}$, a second jump occurs to $\zeta_{3}$ (lower arrow).

The non-monotonic behavior shown in Figure 16, for intermediate values of $\beta$, is the well-known limit-point instability that already appeared in the experiment by Osborne and Sutherland (compare Figure 1 with Figure 16) for spherical and cylindrical shells under internal pressure [2, 6, 22, 54, 116, 117]. For certain materials, the pressure-stretch curve for spherical shells may present a maximum, followed by a minimum; in that case, once the maximum is reached, and the pressure is increased, the stretch will "jump" to a significantly higher value. In spherical shells, several authors have shown that this limit-point instability disappears as the strain-hardening parameter is increased [11, $15,83,118$.

It is tempting to associate certain pathologies such as aneurysms appearing in arteries to a possible mechanical instability. However, the stabilizing effect due to strain-stiffening leads us to conclude that a simple explanation for the formation of aneurysms in terms of limit-point instability is not plausible [26, 91]. The same general trend is exhibited by more realistic models of arteries, involving multiple layers, fiber anisotropy, and residual stress. Nevertheless, various authors have looked at the interesting possibility that aneurysms could be triggered by a local mechanical instability resulting in a localized, but stable, bulged configuration that would then evolve slowly and remodel [46, 47, 48, 123, 124, 131. Aneurysms are such complex progressive diseases that it is unlikely that their formation could be ex-
plained simply as a mechanical phenomenon. Still, it is now appreciated that mechanics and mechanical feedback play an important role in the proper function of arteries and in the formation of aneurysms process [52, 127].

## 8 Linear Elasticity

Overview We show how to obtain the equations of linear elasticity by linearizing the general nonlinear equations of elasticity for small displacements. We also consider the solution of simple problems.

### 8.1 Infinitesimal strain tensor

The central object is not the mapping $\chi$ but the displacement.


$$
\begin{gather*}
\mathbf{u}=\mathbf{x}-\mathbf{X}=\chi(\mathbf{X}, t)-\mathbf{X}  \tag{289}\\
\Longrightarrow \quad \nabla \mathbf{u}=\operatorname{Grad} \chi-\mathbb{1}=\mathbf{F}-\mathbb{1}:=\mathbf{H} \tag{290}
\end{gather*}
$$

the displacement gradient.
Assumptions:

- Displacement gradient is small.

Now consider the strain tensor,

$$
\begin{equation*}
\mathbf{E}_{\mathrm{nonlin}}=\frac{1}{2}\left(\mathbf{F}^{T} \mathbf{F}-\mathbb{1}\right) \tag{291}
\end{equation*}
$$

Letting

$$
\begin{equation*}
\mathbf{F}=\mathbb{1}+\mathbf{H} \Longrightarrow \mathbf{E}=\frac{1}{2}\left[(\mathbb{1}+\mathbf{H})\left(\mathbb{1}+\mathbf{H}^{T}\right)-\mathbb{1}\right]=\underbrace{\frac{1}{2}\left(\mathbf{H}+\mathbf{H}^{T}\right)}_{\mathbf{E}}+\mathcal{O}\left(\mathbf{H}^{2}\right) \tag{292}
\end{equation*}
$$

where

$$
\begin{equation*}
\mathbf{E}=\frac{1}{2}\left(\mathbf{H}+\mathbf{H}^{T}\right)=\frac{1}{2}\left(\nabla \mathbf{u}+(\nabla \mathbf{u})^{T}\right) \tag{293}
\end{equation*}
$$

This is the strain tensor for linear elasticity.

### 8.2 Constant relationships

$$
\begin{equation*}
\mathbf{S}=\mathcal{S}(\mathbf{F}), \quad \mathbf{T}=\mathcal{T}(\mathbf{F}) \tag{294}
\end{equation*}
$$

We assume $\mathcal{S}(\mathbb{1})=0$ (no residual stress).

$$
\begin{equation*}
\Longrightarrow \mathbf{S}=\mathcal{S}(\mathbb{1}+\mathbf{H})=\underbrace{\mathcal{S}(\mathbb{1})}_{0}+\underbrace{D \mathcal{S}(\mathbb{1})[\mathbf{H}]}_{C[\mathbf{H}]}+\mathcal{O}\left(\mathbf{H}^{2}\right), \tag{295}
\end{equation*}
$$

where $C$ is linear in $\mathbf{H}$. Similarly

$$
\begin{equation*}
\mathbf{T}=\underbrace{\mathcal{T}(\mathbb{1})}_{0}+D \mathcal{T}(\mathbb{1})[\mathbf{H}]+\mathcal{O}\left(\mathbf{H}^{2}\right) \tag{296}
\end{equation*}
$$

Which of $\mathbf{T}$ or $\mathbf{S}$ should we use? Well,

$$
\begin{gather*}
\mathbf{T}=J^{-1} \mathbf{F S}  \tag{297}\\
\Longrightarrow \mathcal{T}=J^{-1} \mathbf{F} \mathcal{S} \tag{298}
\end{gather*}
$$

and

$$
\begin{gather*}
\mathcal{T}=D \mathcal{T}[\mathbf{H}]=J^{-1}(\mathbb{1}+\mathbf{H}) D \mathcal{S}(\mathbb{1})[\mathbf{H}]=\operatorname{det}(\mathbb{1}+\mathbf{H})(\mathbb{1}+\mathbf{H}) D \mathcal{S}(\mathbb{1})[\mathbf{H}]+\mathcal{O}\left(\mathbf{H}^{2}\right)  \tag{299}\\
\Longrightarrow D \mathcal{T}[\mathbf{H}]=D \mathcal{S}[\mathbf{H}]=D \mathcal{S}[\mathbf{H}]=C[\mathbf{H}] \tag{300}
\end{gather*}
$$

Hence, the two measures of stress we use in this course are equivalent in linear elasticity.
Now, C, the elasticity tensor, is such that

$$
\begin{equation*}
T_{i j}=C_{i j k \ell} H_{k \ell} \tag{301}
\end{equation*}
$$

Major symmetries:

$$
\begin{equation*}
C_{i j k \ell}=C_{k \ell i j} \tag{302}
\end{equation*}
$$

Minor symmetries:

$$
\begin{equation*}
C_{i j k \ell}=C_{i j k k}=C_{j i k \ell}=C_{j i \ell k} \tag{303}
\end{equation*}
$$

$\Longrightarrow$ from 81 components to 36 independent components.
Note also

$$
\begin{gather*}
T_{i j}=C_{i j k \ell}[\underbrace{\frac{1}{2}\left(\mathbf{H}+\mathbf{H}^{T}\right)}_{\mathbf{E}}+\frac{1}{2}\left(\mathbf{H}-\mathbf{H}^{T}\right)]_{k \ell}  \tag{304}\\
T_{i j}=C_{i j k \ell} \mathbf{E}_{k \ell} \tag{305}
\end{gather*}
$$

constant relationship for linear elasticity.

### 8.3 Isotropic linear elasticity

If the material is isotropic:

$$
\begin{equation*}
S_{i j}=T_{i j}=2 \mu e_{i j}+\lambda(\operatorname{tr} \mathbf{E}) \delta_{i j} \tag{306}
\end{equation*}
$$

where

$$
\begin{equation*}
C_{i j k \ell}=\lambda \delta_{i j} \delta_{k \ell}+2 \mu \delta_{i k} \delta_{j \ell} \tag{307}
\end{equation*}
$$

for $\mu$ and $\lambda$ the Lamé coefficients. From the symmetry of $C$ and positive definiteness, we have

$$
\begin{equation*}
\mu>0, \quad 2 \mu+3 \lambda>0 \tag{308}
\end{equation*}
$$

Note: C is positive definite means

$$
\begin{equation*}
\text { E.C }(\mathbf{E})>0, \quad \forall \mathbf{E} \in \operatorname{Sym} . \tag{309}
\end{equation*}
$$

Material hyperelasticity $\Longleftrightarrow \mathrm{C}$ is positive definite
$\Longrightarrow C$ is symmetric.
If the body is homogeneous, then $\rho_{0}, \lambda, \mu$ are constant.

### 8.3.1 Summary of equations

With $\mathbf{u}=(\boldsymbol{\chi})(\mathbf{X})-\mathbf{X}$, we have that:

$$
\begin{align*}
\mathbf{S}=\mathrm{C}[\mathbf{E}], \quad \mathbf{E} & =\frac{1}{2}\left(\nabla \mathbf{u}+\nabla \mathbf{u}^{T}\right)  \tag{310}\\
& \operatorname{Div} \mathbf{S}+\mathbf{b}_{0} \tag{311}
\end{align*}=\rho_{0} \ddot{\mathbf{u}}=\rho_{0} \mathbf{a} .
$$

Assuming homogeneity and isotropy,

$$
\begin{align*}
& \mathbf{S}=2 \mu \mathbf{E}+\lambda(\operatorname{tr} \mathbf{E}) \mathbb{1}  \tag{312}\\
& \operatorname{Div} \mathbf{S}=\not 2 \mu \operatorname{Div}\left(\frac{1}{\not 2}\left(\nabla \mathbf{u}+\nabla \mathbf{u}^{T}\right)\right)+\lambda \operatorname{Div}\left(\operatorname{tr} \frac{1}{2}\left(\nabla \mathbf{u}+\nabla \mathbf{u}^{T}\right) \mathbb{1}\right)  \tag{313}\\
&= \mu \nabla^{2} \mathbf{u}+\mu \operatorname{Grad} \operatorname{Div} \mathbf{u}+\lambda \operatorname{Grad} \operatorname{Div} \mathbf{u}  \tag{314}\\
&= \mu \nabla^{2} \mathbf{u}+(\mu+\lambda) \operatorname{Grad} \operatorname{Div} \mathbf{u} \tag{315}
\end{align*}
$$

Therefore we have the Navier equation,

$$
\begin{equation*}
\mu \nabla^{2} \mathbf{u}+(\mu+\lambda) \text { Grad Div } \mathbf{u}+\mathbf{b}_{0}=\rho_{0} \ddot{\mathbf{u}} \tag{316}
\end{equation*}
$$

Note that $\mathbf{u}=\mathbf{u}(\mathbf{X})$ implies that $\mathbf{x}$ does not appear any more (we can replace $\mathbf{X}$ by $\mathbf{x}$ if we want - this is a matter of taste).

In components,

$$
\begin{equation*}
\mathbf{u}=\mathbf{u}(\mathbf{X}, t)=u_{i} \mathbf{E}_{i} \tag{317}
\end{equation*}
$$

(with $\mathbf{E}_{i}$ the usual Cartesian basis vectors) implies

$$
\begin{equation*}
\rho_{0} \frac{\partial^{2} u_{i}}{\partial t^{2}}=b_{i}+\mu \sum_{j=1}^{3} \frac{\partial^{2} u_{i}}{\partial X_{j}^{2}}+(\lambda+\mu) \frac{\partial^{2} u_{j}}{\partial X_{i} \partial X_{j}} \tag{318}
\end{equation*}
$$

### 8.4 Examples

To understand the meaning of the elastic moduli, we consider simple deformations.

1) Pure shear, $\mathbf{u}=\left(\gamma X_{2}, 0,0\right)$

$$
[\mathbf{E}]=\frac{1}{2}\left[\begin{array}{ccc}
0 & \gamma & 0  \tag{319}\\
\gamma & 0 & 0 \\
0 & 0 & 0
\end{array}\right], \quad[\sigma]=\left[\begin{array}{ccc}
0 & \tau & 0 \\
\tau & 0 & 0 \\
0 & 0 & 0
\end{array}\right]
$$

$\Longrightarrow \tau=\mu \gamma \Longrightarrow \mu$ is the shear modulus.
2) Uniform compression, $\mathbf{u}=\delta \mathbf{X}$ and $\mathbf{u}=\mathbf{x}-\mathbf{X}=(\delta+1) \mathbf{X}-\mathbf{X}$


$$
\begin{equation*}
\mathbf{E}=\delta \mathbb{1}, \quad \sigma=-p \mathbb{1} \tag{320}
\end{equation*}
$$

We use

$$
\begin{align*}
\mathbf{E}= & \frac{1}{2 \mu}\left[\sigma-\frac{\lambda}{2 \mu+3 \lambda}(\operatorname{tr} \sigma) \mathbb{1}\right]  \tag{321}\\
\delta \mathbb{1} & =\frac{1}{2 \mu}\left[-p \mathbb{1}+\frac{\lambda}{2 \mu+3 \lambda} 3 p \mathbb{1}\right]  \tag{322}\\
& =\frac{1}{2 \mu} p\left[\frac{-(2 \mu+3 \lambda)+3 \lambda}{2 \mu+3 \lambda}\right] \mathbb{1}  \tag{323}\\
& =-\frac{p}{2 \mu+3 \lambda}  \tag{324}\\
\Longrightarrow p & =-(2 \mu+3 \lambda) \delta=-3(\underbrace{\frac{2 \mu+3 \lambda}{3}}_{\kappa}) \delta, \tag{325}
\end{align*}
$$

where $\kappa$ is the modulus of compression. Remember the condition $2 \mu+3 \lambda>0$ !
3) Uniaxial tension, $\sigma=t \mathbf{E}_{1} \otimes \mathbf{E}_{1}$

$$
\begin{equation*}
[\mathbf{E}]=\operatorname{diag}(\alpha, \beta, \beta), \quad \alpha=\frac{t}{E}, \quad \beta=-\nu \alpha . \tag{326}
\end{equation*}
$$



Here $E$ is equated to the infinitesimal Young's modulus and $\nu$ is equated to Poisson's ratio.

$$
\begin{equation*}
\mathbf{E}=\frac{1}{E}[(1+\nu) \sigma-\nu(\operatorname{tr} \quad \sigma) \mathbb{1}] \tag{328}
\end{equation*}
$$

an alternative form for $\mathbf{E}$.
Expect $\nu>0$ (NB: Materials with $\nu<0$ do exist, and are called auxetic materials.) Now

$$
\begin{equation*}
\kappa=\frac{2 \mu+3 \lambda}{3}=\frac{E}{3(1-2 \nu)}, \tag{329}
\end{equation*}
$$

so that as $\nu \rightarrow 1 / 2, \kappa \rightarrow \infty$, and we would need an infinite force to change the volume. Therefore incompressible materials have $\nu=1 / 2$.

### 8.5 Incompressible linear elasticity

Recall: Incompressibility:

$$
\begin{equation*}
\operatorname{det} \mathbf{F}=1, \quad \Longrightarrow \operatorname{det}(\mathbb{1}+\mathbf{H})=1+\operatorname{tr} \quad \mathbf{H}+\mathcal{O}\left(\mathbf{H}^{2}\right)=1 \tag{330}
\end{equation*}
$$

Therefore $\operatorname{tr} \mathbf{H}=0=\operatorname{Div} \mathbf{u}$, and

$$
\begin{equation*}
\operatorname{Div} \mathbf{u}=0 \Longleftrightarrow \operatorname{tr} \quad \mathbf{E}=0 \tag{331}
\end{equation*}
$$

Also

$$
\begin{equation*}
\mathbf{T}=-p \mathbb{1}+J^{-1} \mathbf{F} \frac{\partial \mathbf{W}}{\partial \mathbf{F}}, \quad \sigma=-p \mathbb{1}+C_{i j k \ell} e_{k \ell} \tag{332}
\end{equation*}
$$

For an isotropic material,

$$
\begin{equation*}
\sigma=2 \mu \mathbf{E}+\lambda(\operatorname{tr} \mathbf{E}) \mathbb{1}-p \mathbb{1} \tag{333}
\end{equation*}
$$

but

$$
\begin{equation*}
\mu=\frac{E}{2(1+\nu)}=\frac{E}{3} . \tag{334}
\end{equation*}
$$

Therefore

$$
\begin{equation*}
\rho \ddot{\mathbf{u}}=-\operatorname{Grad} p+\mu \nabla^{2} \mathbf{u} \tag{335}
\end{equation*}
$$

and

$$
\begin{equation*}
\mu=\frac{E}{3} \tag{336}
\end{equation*}
$$

N.B. Boundary conditions

$$
\begin{align*}
& \mathbf{u}=\mathbf{u}^{*}(t),  \tag{337}\\
& \tau \mathbf{n}=\mathbf{T}^{*}(t),  \tag{338}\\
& \text { on } \partial_{1} \mathcal{B} \text { displacements } \\
& \partial_{2} \mathcal{B} \text { traction }
\end{align*}
$$

### 8.5.1 General principles

1) Linear superposition
2) Stresses, strains and displacements are proportional to the loads (or displacements) applied to the solid.
3) If $\partial_{2} \mathcal{B}=\emptyset$ then there exists one unique solution, only displacements.
4) If only traction and tractions are in equilibrium, then stresses and strains are unique. For initial conditions, there exists one unique $u(t)$.

Some nomenclature about loading

1) Plane strain


$$
\mathbf{u}=(u(X, Y), v(X, Y), 0) \Longrightarrow e_{13}=e_{23}=e_{33}=0, \quad \tau_{13}=\tau_{23}=\tau_{31}=\tau_{32}=0 .(339)
$$

2) Plane stress

$$
\tau_{13}=\tau_{23}=\tau_{33}=0, \quad \tau=\left[\begin{array}{lll}
* & * & 0  \tag{340}\\
* & * & 0 \\
0 & 0 & 0
\end{array}\right]
$$

3) Antiplane strain

$$
\begin{equation*}
\mathbf{u}=(0,0, w(X, Y)) \tag{341}
\end{equation*}
$$

4) Pure torsion

$$
\begin{equation*}
\mathbf{u}=[-\Omega Y Z, \Omega X Z, \Omega \varphi(X, Y)] \tag{342}
\end{equation*}
$$

Each of these deformations are covered in detail in C5.2 Elasticity \& Plasticity.

### 8.6 Plane/Strain/Stress Solutions

### 8.6.1 Plane solutions

(stress or strains)
In cartesian coordinates,

$$
\begin{gather*}
e_{i j}=\frac{1}{2}\left(u_{i, j}+u_{j, i}\right)=\frac{1+\nu}{E} \tau_{i j}-\frac{\nu}{E} \tau_{k k} \delta_{i j}  \tag{343}\\
\frac{\partial \tau_{i j}}{\partial X_{i}}+b_{j}=0 \tag{344}
\end{gather*}
$$

Assume that $b$ derives from a potential,

$$
\begin{equation*}
b_{i}=\frac{\partial V}{\partial X_{i}}, \quad i=1,2, \quad b_{3}=0 \tag{345}
\end{equation*}
$$

Plane stresses or strain $\tau_{13}=\tau_{23}=0$.

### 8.6.2 Idea

We would like to ensure that (344) is automatically satisfied identically (just as the streamfunction $\psi$ ensures that incompressibility is automatically satisfied in fluid mechanics). To do this, we let

$$
\begin{equation*}
\tau_{11}=\frac{\partial \phi}{\partial X_{2}}-V, \quad \tau_{22}=\frac{\partial \phi}{\partial X_{1}}-V, \quad \tau_{12}=-\frac{\partial^{2} \phi}{\partial X_{1} \partial X_{2}}, \quad \tau_{33}=\beta \nu\left(\tau_{11}+\tau_{22}\right), \tag{346}
\end{equation*}
$$

$\beta=0$ is plane stress and $\beta=1$ is plane strain.

### 8.6.3 Equations

Now, (344) gives

$$
\begin{equation*}
\frac{\partial \tau_{11}}{\partial X_{1}}+\frac{\partial \tau_{12}}{\partial X_{2}}+b_{1}=0, \quad \frac{\partial \tau_{12}}{\partial X_{1}}+\frac{\partial \tau_{22}}{\partial X_{2}}+b_{2}=0 \tag{347}
\end{equation*}
$$

so substituting in (346) gives

$$
\begin{align*}
& \frac{\partial}{\partial X_{1}}\left(\frac{\partial^{2} \phi}{\partial X_{2}^{2}}-V\right)+\frac{\partial}{\partial X_{2}}\left(-\frac{\partial^{2} \phi}{\partial X_{1} \partial X_{2}}\right)+b_{1}=0,  \tag{348}\\
& \frac{\partial}{\partial X_{1}}\left(-\frac{\partial^{2} \phi}{\partial X_{1} \partial X_{2}}\right)+\frac{\partial}{\partial X_{2}}\left(\frac{\partial^{2} \phi}{\partial X_{2}^{2}}-V\right)+b_{2}=0, \tag{349}
\end{align*}
$$

and the equations of motion are satisfied identically. But we do not have an equation for $\phi$. We have equations for $\tau_{i j}$ or $e_{i j}$, that is, 6 fields but $u_{i}$ is 3 components.

### 8.6.4 Compatibility conditions

Recall: conditions for $\mathbf{F}$ : $\operatorname{Curl} \mathbf{F}=0$. For

$$
\begin{equation*}
e_{i j}=\frac{1}{2}\left(\frac{\partial u_{i}}{\partial x_{j}}+\frac{\partial u_{j}}{\partial x_{i}}\right) \tag{350}
\end{equation*}
$$

Compatibility conditions:

$$
\begin{gather*}
\text { Curl Curl } \mathbf{E}=0  \tag{351}\\
\Longleftrightarrow \epsilon_{i p m} \epsilon_{j q n} \frac{\partial^{2} e_{m n}}{\partial X_{p} \partial X_{q}}=0  \tag{352}\\
\Longleftrightarrow \frac{\partial^{2} e_{i j}}{\partial X_{k} \partial X_{\ell}}+\frac{\partial^{2} e_{k \ell}}{\partial X_{i} \partial X_{j}}-\frac{\partial^{2} e_{i \ell}}{\partial X_{j} \partial X_{k}}-\frac{\partial^{2} e_{j k}}{\partial X_{i} \partial X_{\ell}}=0 \tag{353}
\end{gather*}
$$

These are $\underline{6}$ relations (but only 3 are independent). For planar problems: $e_{13}=e_{23}=0$, $\partial e_{i j} / \partial X_{3}=0$,

$$
\begin{equation*}
\Longrightarrow \frac{\partial^{2} e_{11}}{\partial X_{2}^{2}}+\frac{\partial^{2} e_{22}}{\partial X_{1}^{2}}-2 \frac{\partial^{2} e_{12}}{\partial X_{1} \partial X_{2}}=0 . \tag{354}
\end{equation*}
$$

Now for plane stress we have $\tau_{33}=0$ and from plane strain we have $\tau_{33}=\nu\left(\tau_{11}+\tau_{22}\right)$,

$$
\begin{equation*}
\Longleftrightarrow \tau_{33}=\beta \nu\left(\tau_{11}+\tau_{22}\right) \tag{355}
\end{equation*}
$$

which implies

$$
\begin{align*}
e_{11} & =\frac{1+\nu}{E} \tau_{11}-\frac{\nu}{E}(1+\beta \nu)\left(\tau_{11}+\tau_{22}\right)  \tag{356}\\
e_{22} & =\frac{1+\nu}{E} \tau_{22}-\frac{\nu}{E}(1+\beta \nu)\left(\tau_{11}+\tau_{22}\right)  \tag{357}\\
e_{12} & =\frac{1+\nu}{E} \tau_{12} \tag{358}
\end{align*}
$$

Insert these into $(*)$ and use $\tau_{11}=\frac{\partial^{2} \phi}{\partial X_{1}^{2}}-V$,

$$
\begin{gather*}
\Longrightarrow \frac{\partial^{4} \phi}{\partial x_{1}^{4}}+2 \frac{\partial^{4} \phi}{\partial x_{1}^{2} \partial_{2}^{2}}+\frac{\partial^{4} \phi}{\partial x_{2}^{4}}=\frac{1-\beta \nu^{2}}{1-\nu-2 \beta \nu^{2}}\left(\frac{\partial^{2} V}{\partial x_{1}^{2}}+\frac{\partial^{2} V}{\partial x_{2}^{2}}\right)  \tag{359}\\
\Longleftrightarrow \nabla^{4} \phi=C_{\nu} \Delta V, \quad C_{\nu}=\frac{1-\beta \nu^{2}}{1-\nu-2 \beta \nu^{2}} . \tag{360}
\end{gather*}
$$

Here $\nabla^{4}$ is the biharmonic operator and $\phi$ is the Airy potential. If $\beta=0$, we have plane stress and $\beta=1$ is plane strain.

### 8.7 Elasto-dynamics

$$
\begin{equation*}
\mu \Delta \mathbf{u}+(\lambda+\mu) \operatorname{Grad} \operatorname{Div} \mathbf{u}=\rho \ddot{\mathbf{u}} \tag{*}
\end{equation*}
$$

### 8.7.1 Planar waves

$$
\begin{equation*}
\mathbf{u}(\mathbf{x}, t)=\mathbf{a} \sin (\mathbf{k} \cdot \mathbf{x}-c t) \tag{361}
\end{equation*}
$$

Here $\mathbf{a}$ is the amplitude, $\mathbf{k}$ is the direction and $c$ is the velocity. We normalize such that $|\mathbf{k}|=1$.
2 interesting cases:
$\mathbf{a} \| \mathbf{k} \quad$ longitudinal - primary, pressure, P-waves.
$\mathbf{a} \perp \mathbf{k}$ transverse - shear, secondary, S-waves.


Let $\varphi(\mathbf{x}, t)=\mathbf{k} \cdot \mathbf{x}-c t$.

$$
\begin{align*}
\text { Note that Div } \mathbf{u} & =\mathbf{a} \cdot \mathbf{k} \cos \varphi  \tag{362}\\
\operatorname{Curl} \mathbf{u} & =-\mathbf{a} \times \mathbf{k} \cos \varphi \tag{363}
\end{align*}
$$

Div $\mathbf{u}=0$ is transverse, Curl $\mathbf{u}=0$ is longitudinal.
Substitute $\mathbf{u}=\mathbf{a} \sin \varphi$ in (*). Then

$$
\begin{align*}
\Delta \mathbf{u} & =-\mathbf{a} \sin \varphi  \tag{364}\\
\operatorname{Grad} \operatorname{Div} \mathbf{u} & =\operatorname{Grad}(\mathbf{a} \cdot \mathbf{k} \cos \varphi)=(\mathbf{a} \cdot \mathbf{k}) \mathbf{k}(-\sin \varphi) \tag{365}
\end{align*}
$$

Therefore $\ddot{\mathbf{u}}=-c^{2} \mathbf{a} \sin \varphi$ and

$$
\begin{equation*}
\mu \mathbf{a}+(\lambda+\mu)(\mathbf{a} \cdot \mathbf{k}) \mathbf{k}=\rho c^{2} \mathbf{a} \tag{366}
\end{equation*}
$$

This is a linear operator on a. Define A the acoustic tensor,

$$
\begin{equation*}
\mathbf{A}=\frac{1}{\rho}(\mu \mathbb{1}+(\lambda+\mu) \mathbf{k} \otimes \mathbf{k})[\mathrm{A}]_{i j}=\frac{1}{\rho}\left(\mu \delta_{i j}+(\lambda+\mu) k_{i} k_{j}\right) \tag{367}
\end{equation*}
$$

so that we have the eigenvalue problem

$$
\begin{equation*}
\mathrm{A} \mathbf{a}=c^{2} \mathbf{a} \tag{368}
\end{equation*}
$$

1) $\mathbf{a}=\alpha \mathbf{k}$

$$
\begin{gather*}
\alpha A_{i j} k_{j}=\frac{1}{\rho}(\mu k_{i}+(\lambda+\mu) \underbrace{k_{j} k_{j}}_{1} k_{i})=c^{2} \alpha k_{i}  \tag{369}\\
\Longrightarrow \frac{\lambda+2 \mu}{\rho}=c^{2}, \quad c_{L}=\sqrt{\frac{\lambda+2 \mu}{\rho}} \tag{370}
\end{gather*}
$$

2) $\mathbf{a} \perp \mathbf{k}, a_{i} k_{i}=0$.

$$
\begin{align*}
& A_{i j} a_{j}=\frac{1}{\rho}\left(\mu a_{i}+(\lambda+\mu) k_{i} k_{j} a_{j}\right)=c^{2} a_{i}  \tag{371}\\
& \Longrightarrow c^{2}=\frac{\mu}{\rho}, \quad c_{T}=\sqrt{\frac{\mu}{\rho}}<\sqrt{\frac{\lambda+2 \mu}{\rho}} \tag{372}
\end{align*}
$$

i.e. slower than $c_{L}$.

Note also

$$
\begin{equation*}
c_{L}=\sqrt{\frac{E(1-\nu)}{(1+\nu)(1-2 \nu) \rho}}, \tag{373}
\end{equation*}
$$

where $1-2 \nu=0$ for an incompressible material. Therefore $c_{L} \rightarrow \infty$ as $\nu \rightarrow 1 / 2$.
Also note

$$
\begin{gather*}
c_{T}^{2}=\mu / \rho \quad \Longrightarrow \quad \mu=c_{T}^{2} \rho  \tag{374}\\
c_{L}^{2}=\frac{\lambda}{\rho}+2 c_{T}^{2}, \quad \Longrightarrow \quad \rho c_{L}^{2}-2 \rho c_{T}^{2}  \tag{375}\\
\Longrightarrow  \tag{376}\\
\\
\ddot{\mathbf{u}}=c_{T}^{2} \Delta \mathbf{u}+\left(c_{L}^{2}-c_{T}^{2}\right) \operatorname{Grad} \operatorname{Div} \mathbf{u}
\end{gather*}
$$

## References

[1] Adams, D.S., Keller, R., Koehl, M.A.: The mechanics of notochord elongation, straightening and stiffening in the embryo of Xenopus laevis. Development 110(1), 115-130 (1990)
[2] Adkins, J.E., Rivlin, R.S.: Large elastic deformations of isotropic materials. IX. The deformation of thin shells. Philos. Trans. Roy. Soc. A 244, 505-531 (1952)
[3] Adkins, J.E., Rivlin, R.S.: Large elastic deformations of isotropic materials X. Reinforcement by inextensible cords. Philos. Trans. Roy. Soc. A 248(944), 201-223 (1955)
[4] Agoras, M., Lopez-Pamies, O., Ponte Castañeda, P.: A general hyperelastic model for incompressible fiber-reinforced elastomers. J. Mech. Phys. Solids 57(2), 268-286 (2009)
[5] Alberts, B., Johnson, A., Lewis, J., Raff, M., Roberts, K., Walter, P.: Molecular Biology of the Cell. Taylor \& Francis Group (2008)
[6] Alexander, H.: Tensile instability of initially spherical balloons. Int. J. Eng. Sci 9, 151-160 (1971)
[7] Antman, S.S.: Nonlinear problems of elasticity. Springer New York (2005)
[8] Arruda, E.M., Boyce, M.C.C.: A three-dimensional constitutive model for the large stretch behavior of rubber elastic materials. J. Mech. Phys. Solids 41(2), 389-412 (1993)
[9] Baker, M., Ericksen, J.L.: Inequalities restricting the form of the stress-deformation relations for isotropic elastic solids and Reiner-Rivlin fluids. J. Wash. Acad. Sci 44(3), 33-35 (1954)
[10] Beatty, M.F.: A class of universal relations in isotropic elasticity theory. J. Elasticity 17(2), 113-121 (1987)
[11] Beatty, M.F.: Introduction to nonlinear elasticity. In: Nonlinear effects in fluids and solids, pp. 13-112. Springer (1996)
[12] Bigoni, D., Gei, M.: Bifurcations of a coated, elastic cylinder. Int. J. Solids Struct. 38(30-31), 5117-5148 (2001)
[13] Billington, E.W.: The Poynting effect. Acta Mech. 58(1), 19-31 (1986)
[14] Biot, M.A.: Mechanics of incremental deformation. Wiley, New York (1965)
[15] Bogen, D.K., McMahon, T.A.: Do cardiac aneurysms blow out? Biophys. J. 27 (1979)
[16] Boyce, M.C., Arruda, E.M.: Constitutive models for rubber elasticity: a review. Rubber Chem. Technol. 73, 504-523 (2000)
[17] Bruck, H., Evans, J., Peterson, M.: The role of mechanics in biological and biologically inspired materials. Exp. Mech. 42(4), 361-371 (2002)
[18] Buganza, T.A., Gosain, A.K., Kuhl, E.: Stretching skin: The physiological limit and beyond. Int. J. Non-Linear Mech. 47(8), 938-949 (2012)
[19] Burgert, I.: Exploring the micromechanical design of plant cell walls. Am. J. Bot. 93(10), 1391-1401 (2006)
[20] Castle, E.S.: Spiral growth and reversal of spiraling in Phycomyces, and their bearing on primary wall structure. Amer. J. Bot. 29(8), 664-672 (1942)
[21] Chen, Y.C., Haughton, D.: Stability and bifurcation of inflation of elastic cylinders. Proc. Roy. Soc. Lond. A Mat. 459 (2029), 137-156 (2003)
[22] Chen, Y.C., Healey, T.J.: Bifurcation to pear-shaped equilibria of pressurized spherical membranes. Int. J. Non-Linear Mech. 26, 279-291 (1991)
[23] Chuong, C., Fung, Y.: Compressibility and constitutive equation of arterial wall in radial compression experiments. J. Biomech. 17(1), 35-40 (1984)
[24] Clark, R.B., Cowey, J.B.: Factors controlling the change of shape of certain nemertean and turbellarian worms. J. Exp. Biol. 35(4), 731-748 (1958)
[25] Daerden, F., Lefeber, D.: Pneumatic artificial muscles: actuators for robotics and automation. Euro. J. Mech. Environ. Eng. 47(1), 11-21 (2002)
[26] David, G., Humphrey, J.D.: Further evidence for the dynamic stability of intracranial saccular aneurysms. J. Biomech. 36, 1143-1150 (2003)
[27] De Pascalis, R., Destrade, M., Goriely, A.: Nonlinear correction to the euler buckling formula for compressed cylinders with guided-guided end conditions. J. Elasticity 102(2), 191-200 (2011)
[28] Delfino, A., Stergiopulos, N., Moore, J.E., Meister, J.J.: Residual strain effects on the stress field in a thick wall finite element model of the human carotid bifurcation. J. Biomech. 30(8), 777-786 (1997)
[29] Demiray, H.: A note on the elasticity of soft biological tissues. J. Biomech. 5(3), 309-311 (1972)
[30] Demiray, H., Weizsäcker, H.W., Pascale, K., Erbay, H.A.: A stress-strain relation for a rat abdominal aorta. J. Biomech. 21(5), 369-374 (1988)
[31] Demirkoparan, H., Pence, T.J.: Torsional swelling of a hyperelastic tube with helically wound reinforcement. J. Elasticity 92(1), 61-90 (2008)
[32] Destrade, M., Ogden, R.W.: On the third-and fourth-order constants of incompressible isotropic elasticity. J. Acoust. Soc. Am. 128, 3334-3343 (2010)
[33] Driessen, N.J.B., Cox, M.A.J., Bouten, C.V.C., Baaijens, F.P.T.: Remodelling of the angular collagen fiber distribution in cardiovascular tissues. Biomech. Model. Mechanobiol. 7(2), 93-103 (2008)
[34] Duka, E.D., England, A.H., Spencer, A.J.M.: Bifurcation of a solid circular elastic cylinder under finite extension and torsion. Acta Mech. 98(1), 107-121 (1993)
[35] Dyson, R.J., Jensen, O.E.: A fibre-reinforced fluid model of anisotropic plant cell growth. J. Fluid Mech. 655, 472-503 (2010)
[36] Ericksen, J.L.: Deformations possible in every isotropic, incompressible, perfectly elastic body. ZAMP 5(6), 466-489 (1954)
[37] Ericksen, J.L.: Deformations possible in every compressible, isotropic, perfectly elastic material. J. Math. Phys 34, 126-128 (1955)
[38] Flory, P.J.: Network structure and the elastic properties of vulcanized rubber. Chem. Rev. 35(1), 51-75 (1944)
[39] Flory, P.J.: Statistical thermodynamics of semi-flexible chain molecules. Proc. Roy. Soc. Lond. A 234(1196), 60-73 (1956)
[40] Flory, P.J.: Network topology and the theory of rubber elasticity. Brit. Polym. J. 17(2), 96-102 (1985)
[41] Fosdick, R.L., Schuler, K.W.: On Ericksen's problem for plane deformations with uniform transverse stretch. International Journal of Engineering Science 7(2), 217-233 (1969)
[42] Fratzl, P.: Collagen: structure and mechanics, an introduction. In: P. Fratzl (ed.) Collagen: structure and mechanics, pp. 1-13. Springer Verlag (2008)
[43] Fratzl, P., Burgert, I., Gupta, H.S.: On the role of interface polymers for the mechanics of natural polymeric composites. Phys. Chem Ch. Ph. 6(24), 5575-5579 (2004)
[44] Frei, E., Preston, R.D.: Cell wall organization and wall growth in the filamentous green algae Cladophora and Chaetomorpha. I. The basic structure and its formation. Proc. Roy. Soc. Lond. B pp. 70-94 (1961)
[45] Fried, E.: An elementary molecular-statistical basis for the Mooney and RivlinSaunders theories of rubber elasticity. J. Mech. Phys. Solids 50(3), 571-582 (2002)
[46] Fu, Y., Pearce, S., Liu, K.K.: Post-bifurcation analysis of a thin-walled hyperelastic tube under inflation. Int. J. Nonlinear Mech. 43(8), 697-706 (2008)
[47] Fu, Y., Rogerson, G.A., Zhang, Y.: Initiation of aneurysms as a mechanical bifurcation phenomenon. Int. J. Nonlinear Mech. 47(2), 179-184 (2012)
[48] Fu, Y., Xie, Y.: Stability of localized bulging in inflated membrane tubes under volume control. Int. J. Eng. Sci. 48(11), 1242-1252 (2010)
[49] Fung, Y.C.: Elasticity of soft tissues in simple elongation. Am. J. Physiol. 213(6), 1532-1544 (1967)
[50] Fung, Y.C.: Biorheology of soft tissues. Biorheology 10(2), 139-155 (1973)
[51] Fung, Y.C.: Biomechanics: mechanical properties of living tissues. Springer, New York (1993)
[52] Gasser, T.C., Auer, M., Labruto, F., Swedenborg, J., Roy, J.: Biomechanical rupture risk assessment of abdominal aortic aneurysms: model complexity versus predictability of finite element simulations. Europ. J. Vasc. and Endovasc. Surg. 40(2), 176-185 (2010)
[53] Gent, A.: A new constitutive relation for rubber. Rubber Chem. and Technol. 69 (1996)
[54] Gent, A.: Elastic instabilities of inflated rubber shells. Rubber Chem. Technol. 72, 263-268 (1999)
[55] Gent, A.N.: Elastic instabilities in rubber. Int. J. Non-Linear Mech. 40, 165-175 (1995)
[56] Goriely, A., Tabor, M.: Spontaneous rotational inversion in Phycomyces. Phys. Rev. Lett. 106(13), 138,103 (2011)
[57] Goriely, A., Tabor, M.: Rotation, inversion and perversion in anisotropic elastic cylindrical tubes and membranes. Proc. Roy. Soc. Lond. A 469(2153) (2013)
[58] Goriely, A., Vandiver, R., Destrade, M.: Nonlinear Euler buckling. Proc. Roy. Soc. Lond. A 464(2099), 3003-3019 (2008)
[59] Green, A.E., Zerna, W.: Theoretical Elasticity. Dover, New York (1992)
[60] Gurtin, M.E.: An introduction to continuum mechanics. Academic Press (1981)
[61] Gurtin, M.E., Fried, E., Anand, L.: The mechanics and thermodynamics of continua. Cambridge University Press (2010)
[62] Hariton, I., DeBotton, G., Gasser, T.C., Holzapfel, G.A.: Stress-driven collagen fiber remodeling in arterial walls. Biomech. Model. Mechanobiol. 6(3), 163-175 (2007)
[63] Harris, J.E., Crofton, H.D.: Structure and function in the nematodes: internal pressure and cuticular structure in ascaris. J. Exp. Biol. 34(1), 116-130 (1957)
[64] Haughton, D.M., Ogden, R.W.: Bifurcation of inflated circular cylinders of elastic material under axial loading-II. exact theory for thick-walled tubes. J. Mech. Phys. Solids 27, 489-512 (1979)
[65] Haughton, D.M., Ogden, R.W.: Bifurcation of inflated circular cylinders of elastic material under axial loading-I. Membrane theory for thin-walled tubes. J. Mech. Phys. Solids 27, 179-212 (1979)
[66] Hennel, J.W., Klinowski, J.: Magic-angle spinning: a historical perspective. In: New techniques in solid-state NMR, pp. 1-14. Springer (2005)
[67] Hofhuis, H., Moulton, D., Lessinnes, T., Routier-Kierzkowska, A.L., Bomphrey, R.J., Mosca, G., Reinhardt, H., Sarchet, P., Gan, X., Tsiantis, M., Ventikos, Y., Walker, S., A., G., R., S., Hay, A.: Morphomechanical innovation drives explosive seed dispersal. Cell 166, 222-233 (2016)
[68] Holzapfel, G.A.: Biomechanics of soft tissue. The handbook of materials behavior models 3, 1049-1063 (2001)
[69] Holzapfel, G.A.: Collagen in arterial walls: biomechanical aspects. In: P. Fratzl (ed.) Collagen: structure and mechanics, pp. 285-324. Springer Verlag (2008)
[70] Holzapfel, G.A., Gasser, T.C.: A viscoelastic model for fiber-reinforced composites at finite strains: Continuum basis, computational aspects and applications. Comput. Methods Appl. Mech. Eng 190(34), 4379-4403 (2001)
[71] Holzapfel, G.A., Gasser, T.C., Ogden, R.W.: A new constitutive framework for arterial wall mechanics and a comparative study of material models. J. Elasticity 61, 1-48 (2000)
[72] Holzapfel, G.A., Ogden, R.W.: Constitutive modelling of passive myocardium: A structurally based framework for material characterization. Philos. Trans. Roy. Soc. A 367(1902), 3445-3475 (2009)
[73] Holzapfel, G.A., Ogden, R.W.: Constitutive modelling of arteries. Proc. Roy. Soc. Lond. A 466(2118), 1551-1597 (2010)
[74] Horgan, C.O., Murphy, J.G.: Constitutive modeling for moderate deformations of slightly compressible rubber. J. Rheol. 53, 153-168 (2009)
[75] Horgan, C.O., Murphy, J.G.: Torsion of incompressible fiber-reinforced nonlinearly elastic circular cylinders. J. Elasticity 103(2), 235-246 (2011)
[76] Horgan, C.O., Saccomandi, G.: Constitutive modeling of rubber-like and biological materials with limited chain extensibility. Math. Mech. Solids 7, 353-371 (2002)
[77] Horgan, C.O., Saccomandi, G.: A molecular-statistical basis for the Gent constitutive model of rubber elasticity. J. Elasticity 68, 167-176 (2002)
[78] Horgan, C.O., Saccomandi, G.: A description of arterial wall mechanics using limiting chain extensibility constitutive models. Biomech. Model. Mechanobiol. 1 (2003)
[79] Horgan, C.O., Saccomandi, G.: Constitutive models for compressible nonlinearly elastic materials with limiting chain extensibility. J. Elasticity 77, 123-138 (2004)
[80] Horny, L., Kronek, J., Chlup, H., Gultova, E., Heller, L., Zitny, R., Vokoun, D.: Inflation-extension test of silicon rubber-nitinol composite tube. In: 5th European Conference of the International Federation for Medical and Biological Engineering, pp. 1027-1030. Springer (2012)
[81] Howard, R.J., Valent, B.: Breaking and entering: host penetration by the fungal rice blast pathogen, Magnaporthe grisea. Annu. Rev. Microbiol. 50, 491-512 (1996)
[82] Hu, T., Desai, J.P.: Characterization of soft-tissue material properties: large deformation analysis. In: Medical Simulation, pp. 28-37. Springer (2004)
[83] Humphrey, J.D.: Cardiovascular solid mechanics. Cells, tissues, and organs. Springer Verlag, New York (2002)
[84] Janmey, P.A., McCormick, M.E., Rammensee, S., Leight, J.L., Georges, P.C., MacKintosh, F.C.: Negative normal stress in semiflexible biopolymer gels. Nature Mat. 6(1), 48-51 (2006)
[85] Ker, R.F.: Damage and fatigue. In: P. Fratzl (ed.) Collagen: structure and mechanics, pp. 111-131. Springer Verlag (2008)
[86] Kier, W.M.: The diversity of hydrostatic skeletons. J. Exp. Biol. 215(8), 1247-1257 (2012)
[87] Kier, W.M., Smith, K.K.: Tongues, tentacles and trunks: the biomechanics of movement in muscular-hydrostats. Zool. J. Linn. Soc. 83(4), 307-324 (1985)
[88] Kirkinis, E., Ogden, R.W.: On extension and torsion of a compressible elastic circular cylinder. Math. Mech. Solids 7(4), 373-392 (2002)
[89] Koehl, M.A.R.: Physical modelling in biomechanics. Philos. Trans. Roy. Soc. Lond. B 358(1437), 1589-1596 (2003)
[90] Koehl, M.A.R., Quillin, K.J., Pell, C.A.: Mechanical design of fiber-wound hydraulic skeletons: the stiffening and straightening of embryonic notochords. Amer. Zool. 40(1), 28-41 (2000)
[91] Kyriacou, S., Humphrey, J.D.: Influence of size, shape and properties on the mechanics of axisymmetric saccular aneurysms. J. Biomech. 29(8), 1015-1022 (1996)
[92] Lally, C., Reid, A., Prendergast, P.: Elastic behavior of porcine coronary artery tissue under uniaxial and equibiaxial tension. Ann. Biomed. Eng. 32(10), 1355-1364 (2004)
[93] Landau, L.D., Lifshitz, E.M.: Theory of Elasticity. Pergamon Press, Oxford (1959)
[94] Langewouters, G.J., Wesseling, K.H., Goedhard, W.J.A.: The static elastic properties of 45 human thoracic and 20 abdominal aortas in vitro and the parameters of a new model. J. biomechanics 17(6), 425-435 (1984)
[95] Lanir, Y.: A structural theory for the homogeneous biaxial stress-strain relationships in flat collagenous tissues. J. Biomech. 12(6), 423-436 (1979)
[96] Lanir, Y.: Constitutive equations for fibrous connective tissues. J. Biomech. 16(1), 1-12 (1983)
[97] Lanir, Y., Fung, Y.C.: Two-dimensional mechanical properties of rabbit skin-II. Experimental results. J. Biomech. 7(2), 171-182 (1974)
[98] Liu, W., Rahn, C.R.: Fiber-reinforced membrane models of mckibben actuators. J. Appl. Mech. 70(6), 853-859 (2003)
[99] Lloyd, C., Chan, J.: Helical microtubule arrays and spiral growth. Plant Cell Online 14(10), 2319-2324 (2002)
[100] Lopez-Pamies, O.: Onset of cavitation in compressible, isotropic, hyperelastic solids. J. Elasticity 94, 115-145 (2009)
[101] Lopez-Pamies, O., Ponte Castañed, P.: Homogenization-based constitutive models for porous elastomers and implications for macroscopic instabilities: I-analysis. J. Mech. Phys. Solids 55(8), 1677-1701 (2007)
[102] Mallock, A.: Note on the instability of india-rubber tubes and balloons when distended by fluid pressure. Proc. Roy. Soc. Lond. 49(296-301), 458-463 (1890)
[103] Marzano, S.: An interpretation of Baker-Ericksen inequalities in uniaxial deformation and stress. Meccanica 18(4), 233-235 (1983)
[104] Melnik, A.V., Da Rocha, H.B., Goriely, A.: On the modeling of fiber dispersion in fiber-reinforced elastic materials. Int. J. Non Linear Mech. 75, 92-106 (2015)
[105] Melnik, A.V., Goriely, A.: Dynamic fiber reorientation in a fiber-reinforced hyperelastic material. Math. Mech. Solids 18(6), 634-648 (2013)
[106] Menzel, A.: Modelling of anisotropic growth in biological tissues. Biomech. Model. Mechanobiol. 3(3), 147-171 (2005)
[107] Menzel, A.: Anisotropic remodelling of biological tissues. Mechanics of Biological Tissue pp. 91-104 (2006)
[108] Merodio, J., Ogden, R.W.: Instabilities and loss of ellipticity in fiber-reinforced compressible non-linearly elastic solids under plane deformation. Int. J. Solids and Struct. 40(18), 4707-4727 (2003)
[109] Merodio, J., Ogden, R.W.: Mechanical response of fiber-reinforced incompressible nonlinearly elastic solids. Int. J. Nonlinear Mech. 40(2), 213-227 (2005)
[110] Merodio, J., Ogden, R.W.: The influence of the invariant I8 on the stress-deformation and ellipticity characteristics of doubly fiber-reinforced non-linearly elastic solids. Int. J. Nonlinear Mech. 41(4), 556-563 (2006)
[111] Middlebrook, M.J., Preston, R.D.: Spiral growth and spiral structure: III. wall structure in the growth zone of Phycomyces. Biochim. Biophys. Acta. 9, 32-37 (1952)
[112] Mihai, L.A., Chin, L., Janmey, P.A., Goriely, A.: A comparison of hyperelastic constitutive models applicable to brain and fat tissues. J. R. Soc. Interface $\mathbf{1 2 ( 1 1 0 ) , ~ 2 0 1 5 0 , 4 8 6 ~}$ (2015)
[113] Mihai, L.A., Goriely, A.: Positive or negative Poynting effect? the role of adscititious inequalities in hyperelastic materials. Proc. Roy. Soc. Lond. A 467(2136), 3633-3646 (2011)
[114] Mihai, L.A., Goriely, A.: Numerical simulation of shear and the Poynting effects by the finite element method: An application of the generalised empirical inequalities in non-linear elasticity. Int. J. Nonlinear Mech. 49, 1-14 (2012)
[115] Moon, H., Truesdell, C.: Interpretation of adscititious inequalities through the effects pure shear stress produces upon an isotropic elastic solid. Arch. Rat. Mech. Anal. 55(1), 1-17 (1974)
[116] Müller, I., H., S.: Inflating a rubber balloon. Math. Mech. Solids 7, 569-577 (2002)
[117] Ogden, R.W.: Large deformation isotropic elasticity - On the correlation of theory and experiment for incompressible rubberlike solids. Proc. Roy. Soc. Lond. A 326 (1972)
[118] Ogden, R.W.: Non-linear Elastic Deformations. Dover, New york (1984)
[119] Ogden, R.W.: Recent advances in the phenomenological theory of rubber elasticity. Rubber Chem. Technol. 59(3), 361-383 (1986)
[120] Ogden, R.W.: Nonlinear elasticity with application to material modeling. Polish Academy of Sciences (2003)
[121] Ogden, R.W., Saccomandi, G., Sgura, I.: Fitting hyperelastic models to experimental data. Comp. Mech. 34(484-502) (2004)
[122] Osborne, W.A., Sutherland, W.: The elasticity of rubber balloons and hollow viscera. Proc. Roy. Soc. Lond. B 81(551), 485-499 (1909)
[123] Pearce, S.: Effect of strain-energy function and axial prestretch on the bulges, necks and kinks forming in elastic membrane tubes. Math. Mech. Solids 17(8), 860-875 (2012)
[124] Pearce, S., Fu, Y.: Characterization and stability of localized bulging/necking in inflated membrane tubes. IMA J. Appl. Math. 75(4), 581-602 (2010)
[125] Pucci, E., Saccomandi, G.: On universal relations in continuum mechanics. Continuum Mech. Therm. 9(2), 61-72 (1997)
[126] Qiu, G.Y., Pence, T.J.: Remarks on the behavior of simple directionally reinforced incompressible nonlinearly elastic solids. J. Elasticity 49(1), 1-30 (1997)
[127] Riveros, F., Martufi, G., Gasser, T.C., Rodriguez-Matas, J.F.: On the impact of intraluminal thrombus mechanical behavior in AAA passive mechanics. Ann. Biomed. Eng. pp. 1-12 (2015)
[128] Rivlin, R.S.: Large elastic deformations of isotropic materials. I. fundamental concepts. Philos. Trans. Roy. Soc. A 240(822), 459-490 (1948)
[129] Rivlin, R.S.: Large elastic deformations of isotropic materials. III. some simple problems in cylindrical polar co-ordinates. Philos. Trans. Roy. Soc. A 240(823), 509-525 (1948)
[130] Rivlin, R.S.: Large elastic deformations of isotropic materials. IV. further developments of the general theory. Philos. Trans. Roy. Soc. A 241(835), 379-397 (1948)
[131] Rodriguez, J., Merodio, J.: A new derivation of the bifurcation conditions of inflated cylindrical membranes of elastic material under axial loading. application to aneurysm formation. Mech. Res. Commun. 38(3), 203-210 (2011)
[132] S., M.R., Kier, W.M.: The functional morphology of starfish tube feet: the role of a crossed-fiber helical array in movement. Biol. B. 188(2), 197-209 (1995)
[133] Saccomandi, G.: Universal results in finite elasticity. Nonlinear Elasticity: Theory and Applications 283, 97 (2001)
[134] Saccomandi, G.: Nonlinear elasticity for soft fibrous materials. In: Nonlinear Mechanics of Soft Fibrous Materials, pp. 121-173. Springer (2015)
[135] Sacks, M.S.: Biaxial mechanical evaluation of planar biological materials. J. Elasticity 61, 199-246 (2000)
[136] Sacks, M.S., Sun, W.: Multiaxial mechanical behavior of biological materials. Annu. Rev. Biomed. Eng. 5(1), 251-284 (2003)
[137] Santulli, C., Patel, S.I., Jeronimidis, G., Davis, F.J., Mitchell, G.R.: Development of smart variable stiffness actuators using polymer hydrogels. Smart Mater. Struct. 14, 434-440 (2005)
[138] Shergold, O.A., Fleck, N.A., Radford, D.: The uniaxial stress versus strain response of pig skin and silicone rubber at low and high strain rates. Int. J. Impact Eng. 32, 1384-1402 (2006)
[139] Spencer, A.J.M.: Deformations of Fibre-Reinforced Materials. Oxford (1972)
[140] Spencer, A.J.M.: Continuum theory of the mechanics of fibre-reinforced composites, vol. 282. Springer New York: (1984)
[141] Steigmann, D.J.: Effects of fiber bending and twisting resistance on the mechanics of fiber-reinforced elastomers. In: Nonlinear Mechanics of Soft Fibrous Materials, pp. 269-305. Springer (2015)
[142] Sun, W., Sacks, M.S.: Finite element implementation of a generalized fung-elastic constitutive model for planar soft tissues. Biomech. Model. Mechanobiol. 4(2-3), 190199 (2005)
[143] Treloar, L.R.G.: The elasticity of a network of long-chain molecules-II. Trans. Faraday Soc. 39, 241-246 (1943)
[144] Treloar, L.R.G.: The elasticity of a network of long-chain molecules. I. Rubber Chem. Technol. 16(4), 746-751 (1943)
[145] Triantafyllidis, N., Abeyaratne, R.: Instabilities of a finitely deformed fiber-reinforced elastic material. J. Appl. Mech. 50, 149-156 (1983)
[146] Truesdell, C., Noll, W.: The Non-Linear Field Theories of Mechanics. Springer (2004)
[147] Truesdell, C.A.: A program of physical research in classical mechanics. ZAMP 3(2), 79-95 (1952)
[148] Vande Geest, J.P., Sacks, M.S., Vorp, D.A.: The effects of aneurysm on the biaxial mechanical behavior of human abdominal aorta. J. Biomech. 39(7), 1324-1334 (2006)
[149] Vandiver, R., Goriely, A.: Differential growth and residual stress in cylindrical elastic structures. Philos. Trans. Roy. Soc. Lond. A 367(1902), 3607-3630 (2009)
[150] Vito, R.P., Dixon, S.A.: Blood vessels constitutive models-1995-2002. Annu. Rev. Biomed. Eng. 5 (2003)
[151] Wang, C.C., Truesdell, C.: Introduction to Rational Elasticity. Springer Science \& Business Media (1973)
[152] Weickenmeier, J., Butler, C., Young, P.G., A., G., Kuhl, E.: The mechanics of decompressive craniectomy: Personalized simulations. Comput. Methods Appl. Mech. Eng. (2016)
[153] Weickenmeier, J., Saez, P., Butler, C., Young, P., Goriely, A., Kuhl, E.: Bulging brains. Journal of Elasticity 129(1-2), 197-212 (2017)
[154] Wilber, J.P., Walton, J.R.: The convexity properties of a class of constitutive models for biological soft issues. Math. Mech. Solids 7(3), 217-235 (2002)
[155] Wineman, A.: Some results for generalized neo-Hookean elastic materials. Int. J. Non Linear Mech. 40(2), 271-279 (2005)
[156] Zou, Y., Zhang, Y.: An experimental and theoretical study on the anisotropy of elastin network. Ann. Biomed. Eng. 37(8), 1572-1583 (2009)

